

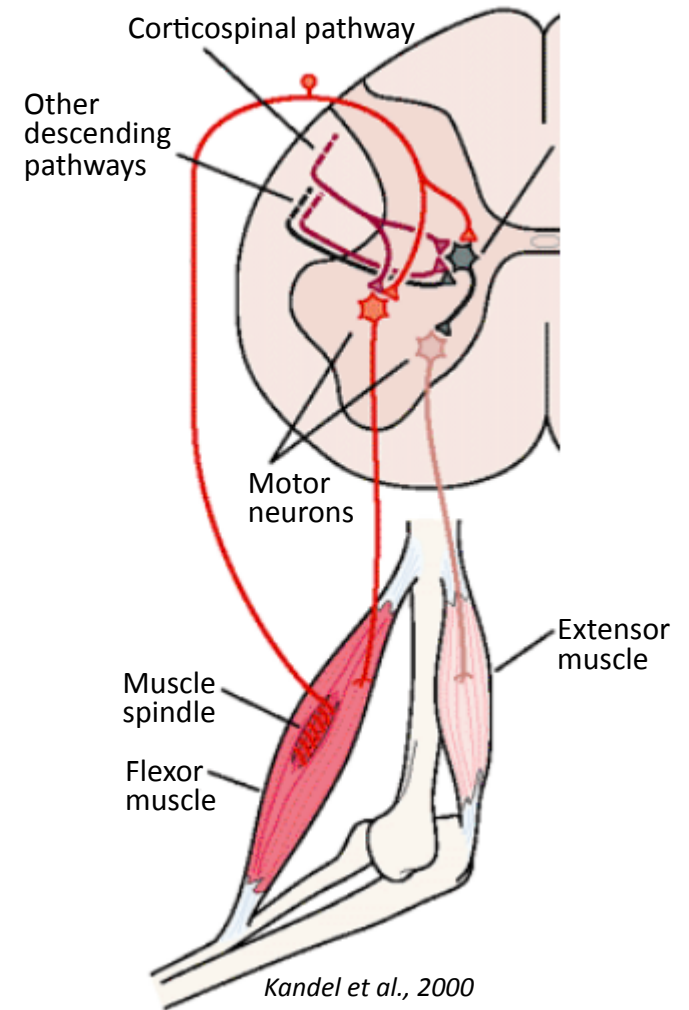
# *What Roboticians Need to Know About NeuroMusculoSkeletal Systems*

Gerald E. Loeb, M.D.  
Professor of Biomedical Engineering  
Director of the Medical Device Development Facility  
University of Southern California

# Gerald E. Loeb

- Background
  - 1965-1973 B.A., M.D. Johns Hopkins University, internship in surgery
  - 1973-1988 Lab. Of Neural Control, National Institutes of Health
  - 1988-1999 Professor of Physiology, Queen's Univ., Canada
  - 1994-1999 Chief Scientist, Advanced Bionics Corp., Los Angeles
  - 1999-present Professor of Biomedical Engineering, Director of the Medical Device Development Facility, Univ. Southern California
  - 2008-present CEO, SynTouch LLC, Los Angeles
- Research Interests
  - Sensorimotor neurophysiology and control
  - Biomimetic prosthetic and robotic systems
- Issues in Impedance Control
  - Biological components (actuators, sensors, feedback loops) are much more nonlinear, noisy and slow than their mechatronic counterparts, yet they perform much better on unpredictable tasks and a baby can learn to use them.
  - We need to understand why if we are going to repair or replace them.

# Investigating the role of muscle physiology and spinal circuitry in movement



## Current and recent collaborators:

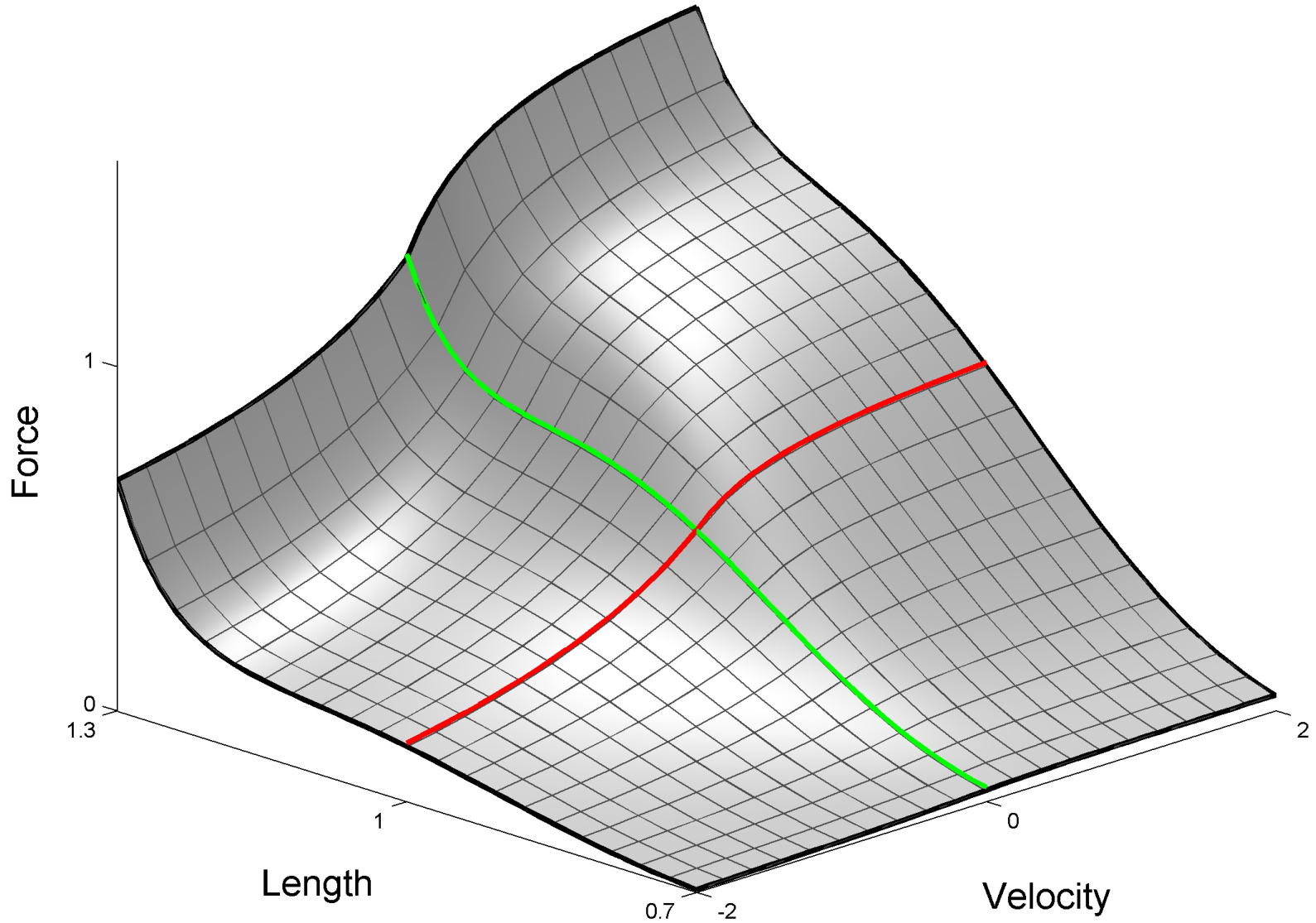
*Research Asst. Professor:* Dr. Rahman Davoodi

*Post-doctoral fellows:* Giby Raphael, Yao Li

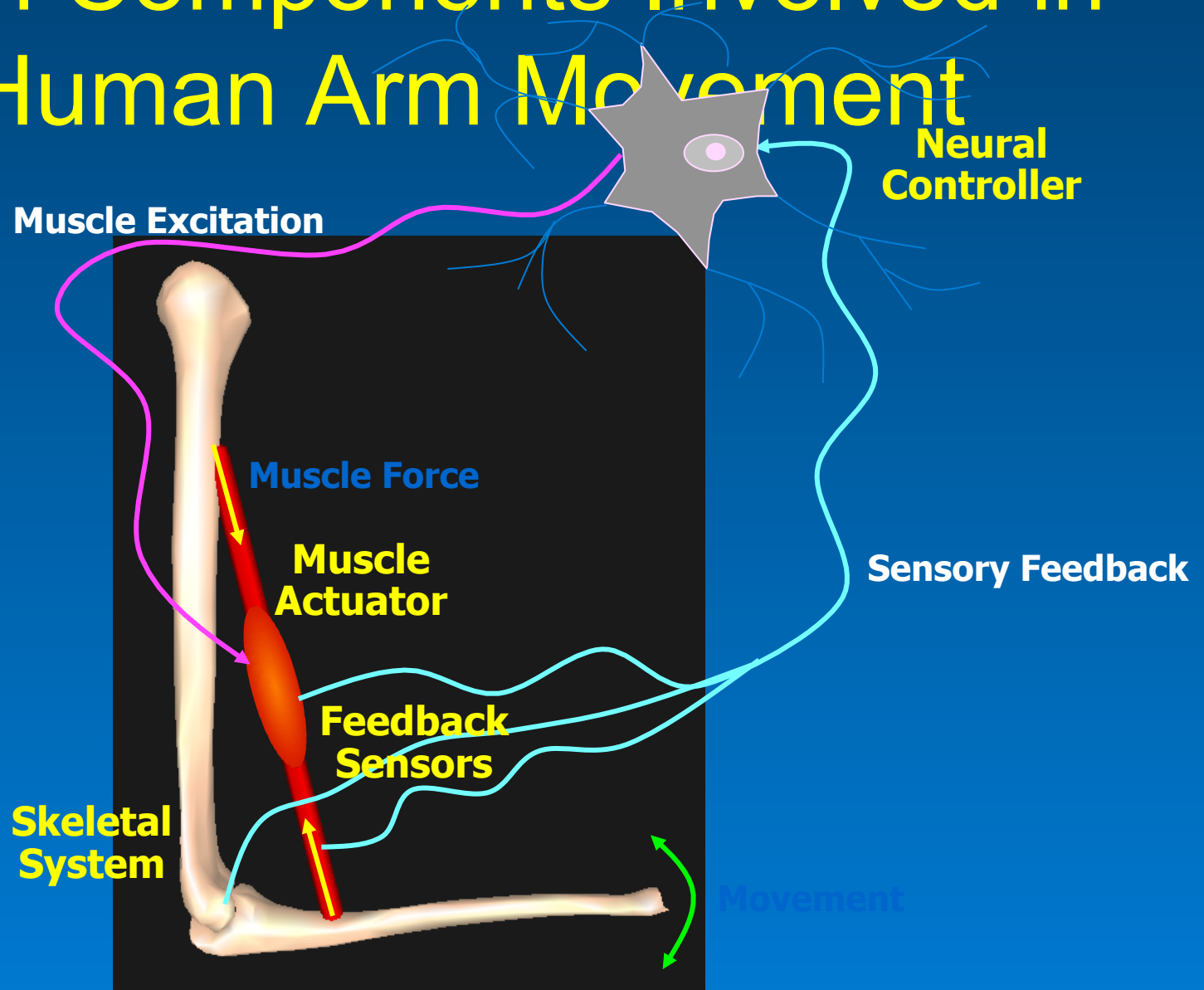
*Graduate students:* George Tsianos, Cedric Rustin, Jared Goodner, Katherine Quigley

*Undergraduates:* Norman Li, Travis Marziani, Adam Baybutt, Enrique Morales, Michelle Fung

# Muscle $\neq$ Torque Motor



# Main Components Involved in Human Arm Movement

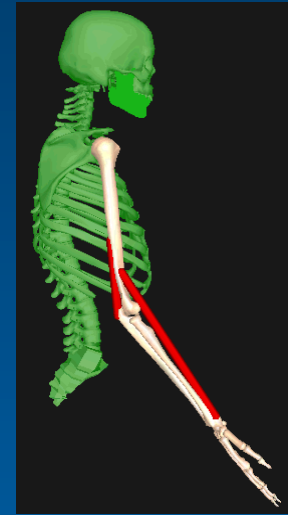


# Actuator Properties: Underlying Mechanisms

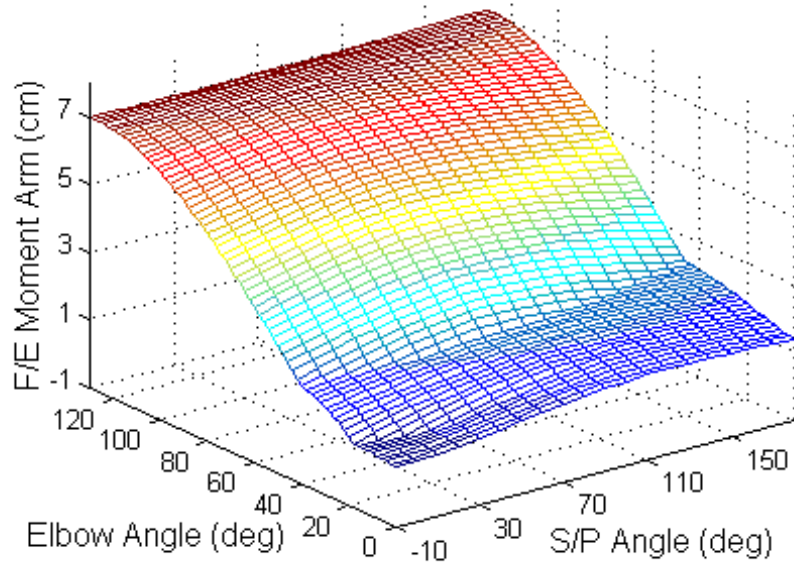
- Force – Length: Myofilament overlap
- Force – Velocity: Cross-bridge dynamics
- Force – Frequency: Calcium kinetics
- **Moment – Angle: Tendon path**
- **Elastic Storage: Collagen ultrastructure**
- Energy Transfer: Multiarticular muscles
- Impedance Control: Cocontraction

*Muscle accounts for the majority of animal mass and energy consumption. The evolutionary pressures to find and exploit any advantage are huge.*

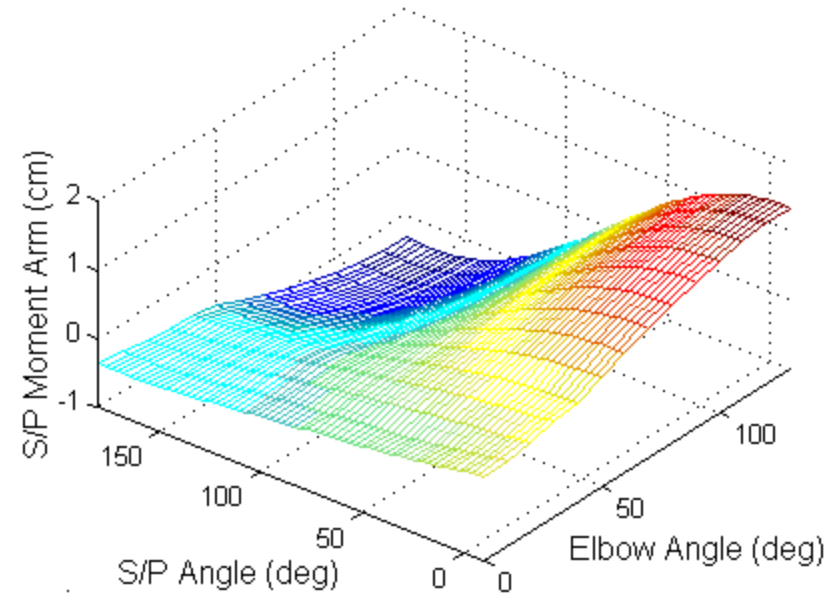
# Complex Moment Arms at the Human Elbow

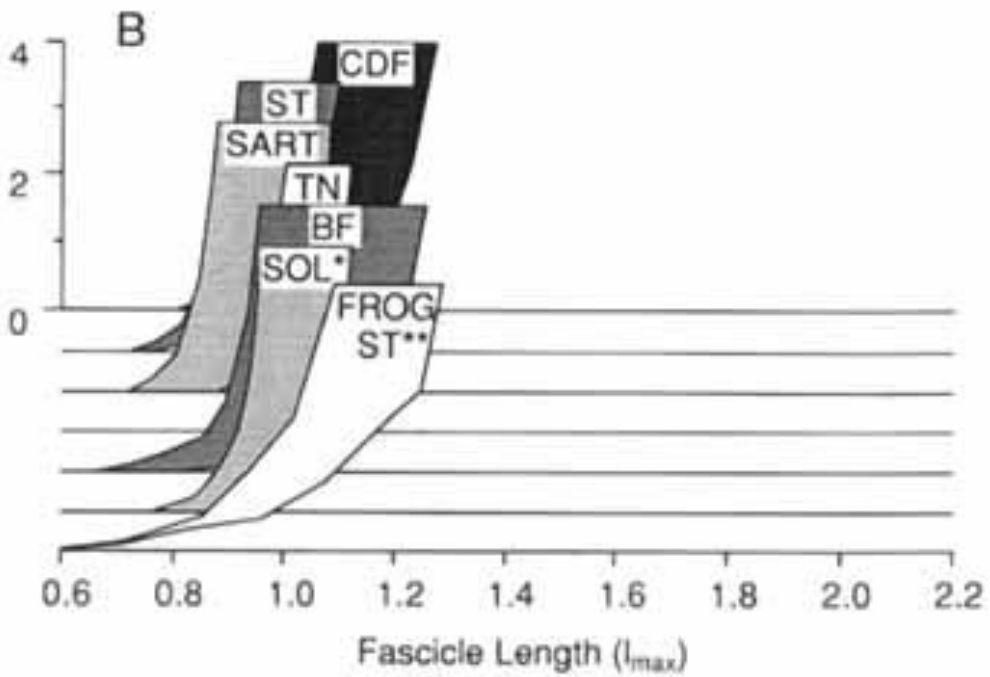
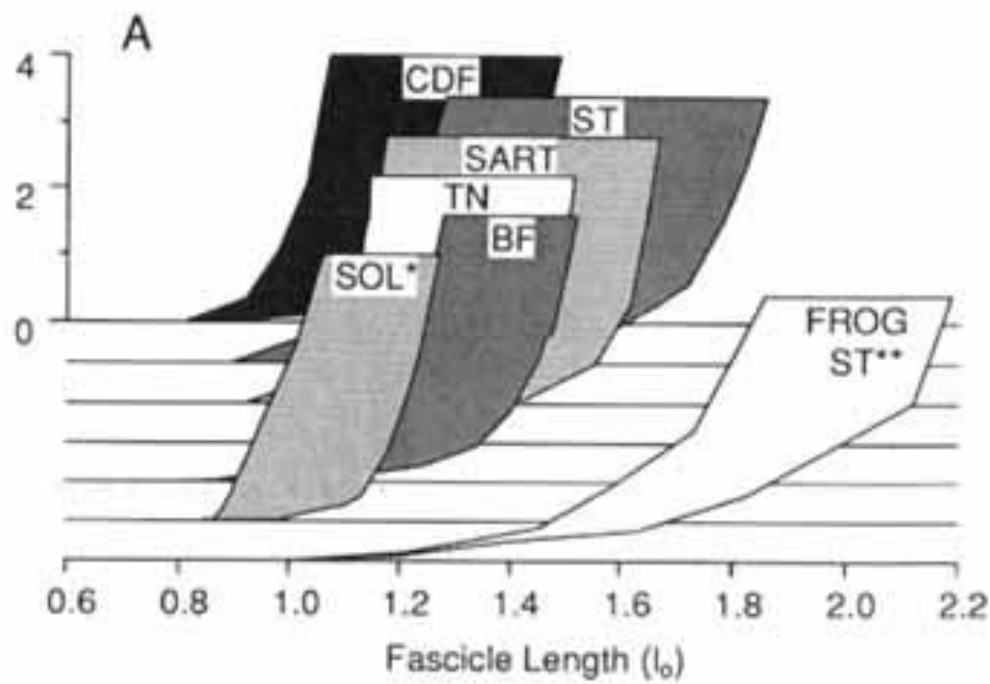
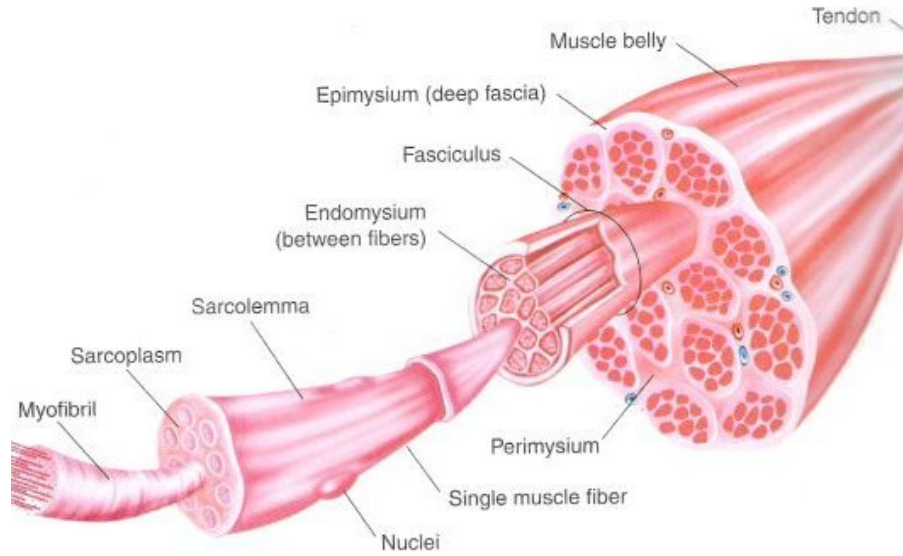


F/E Moment Arm of Brachioradialis



S/P Moment Arm of Brachioradialis

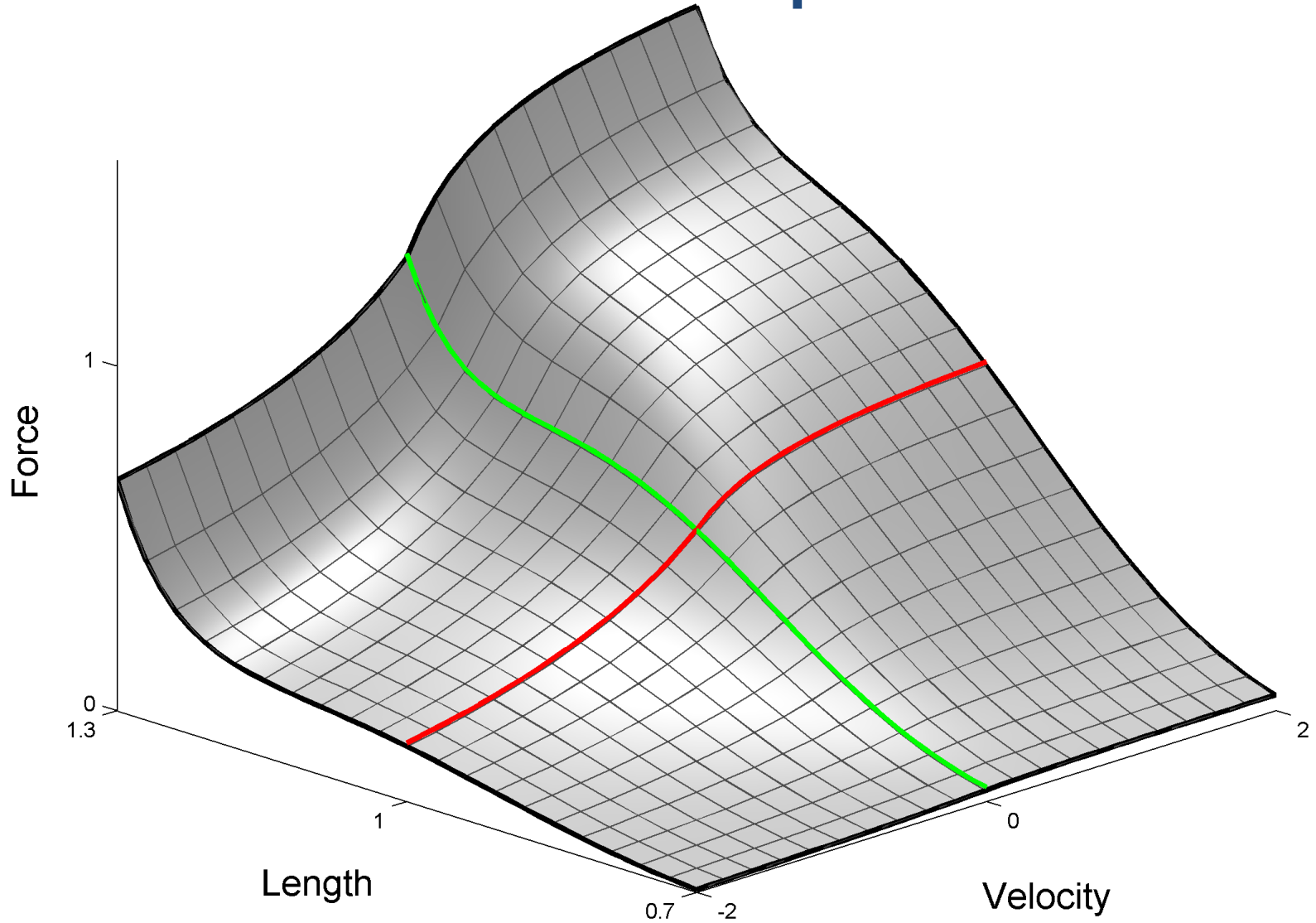




**Biological  
Elasticity:  
*Nonlinear  
Adaptive***



# Muscle $\neq$ Torque Motor



Virtual Muscle, based on ~20 experimental and modeling papers with Steve Scott, Ian Brown, Milana Mileusnic, George Tsianos, et al.

Available from <http://bme.usc.edu/gloeb>

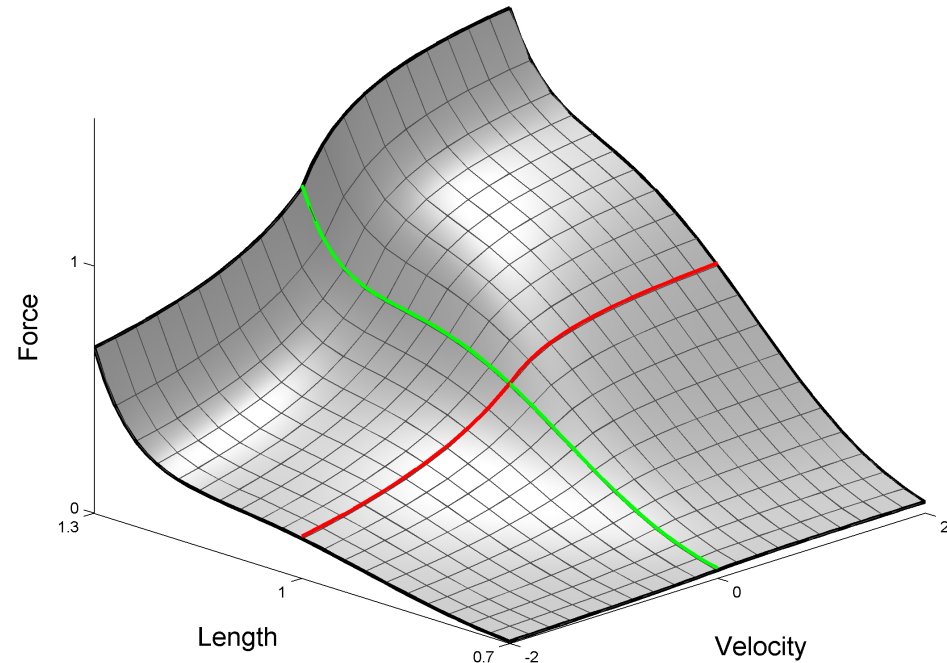
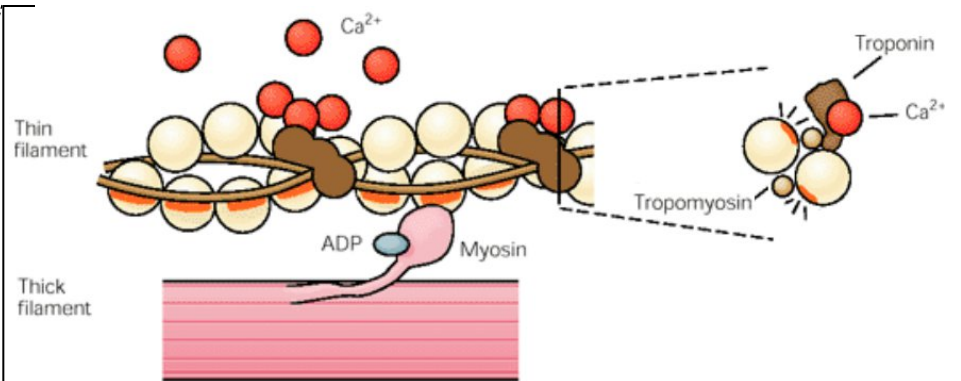
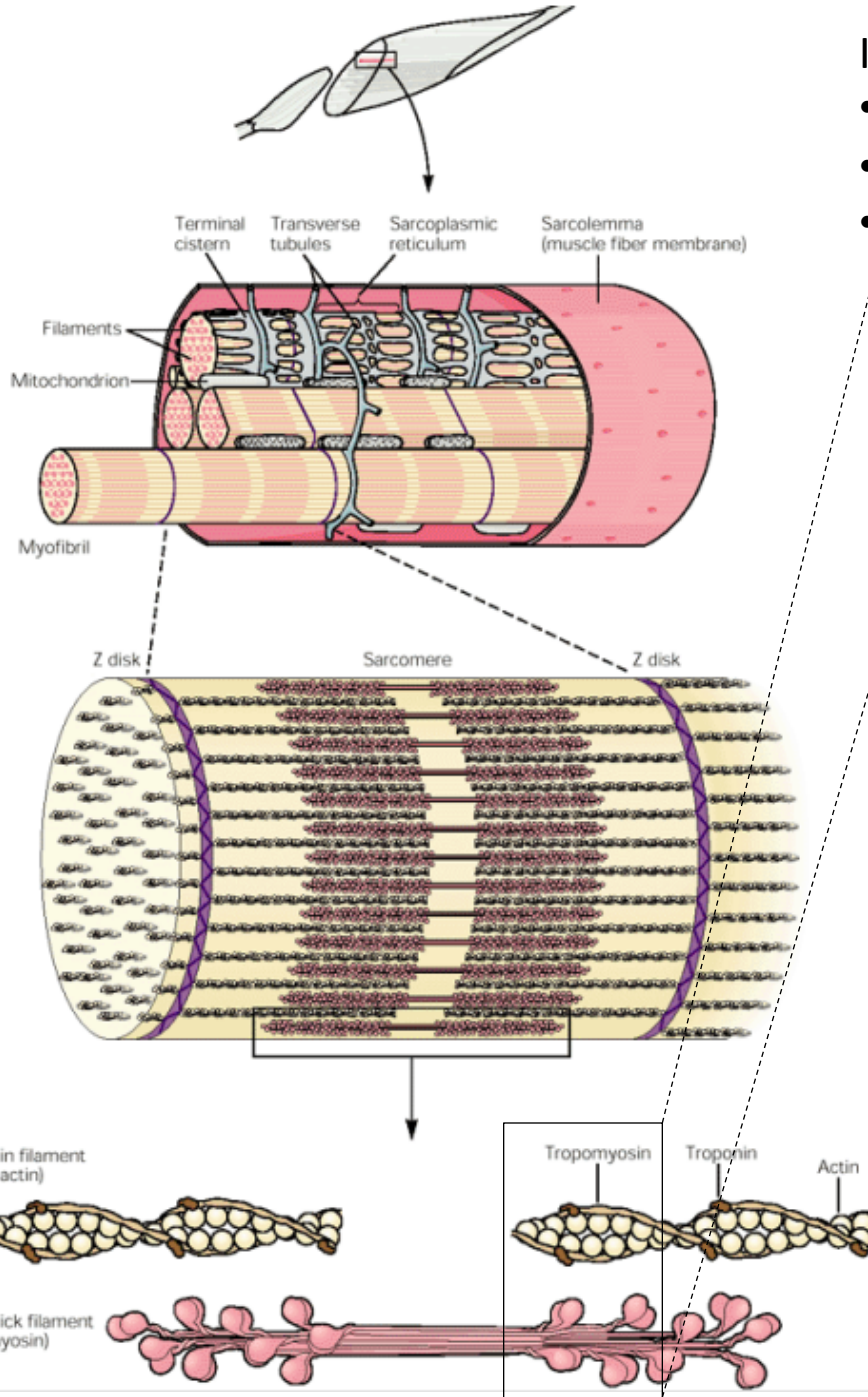
# Actuator Properties: Underlying Mechanisms

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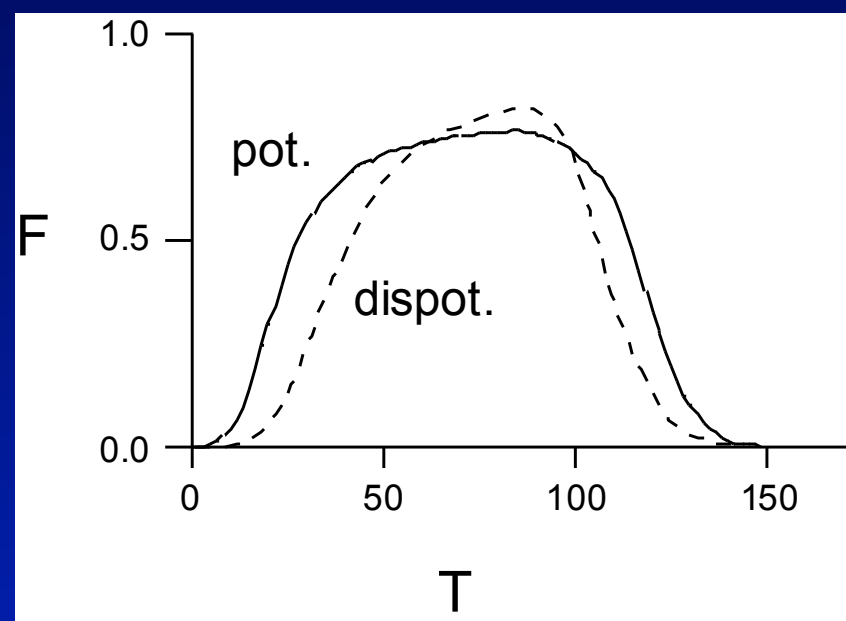
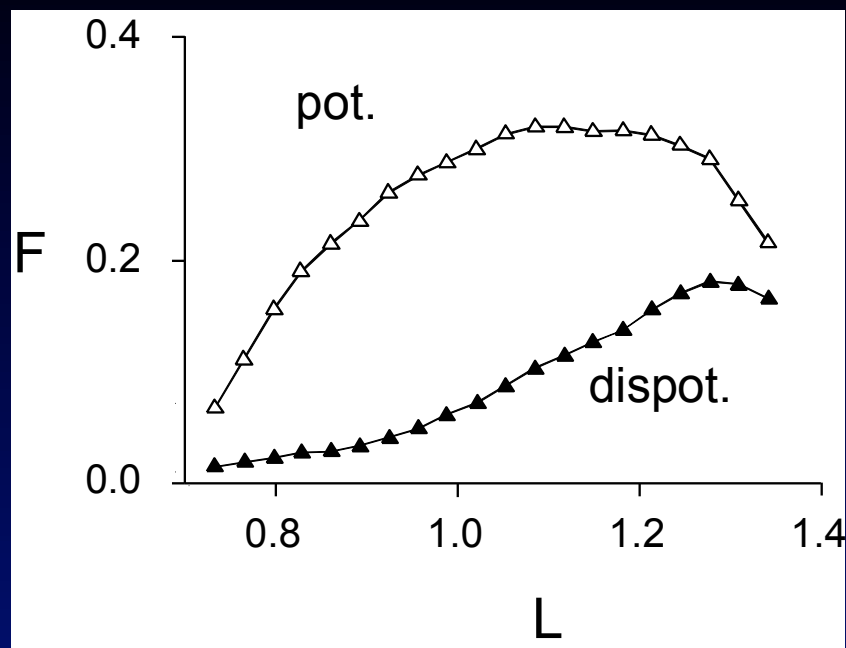
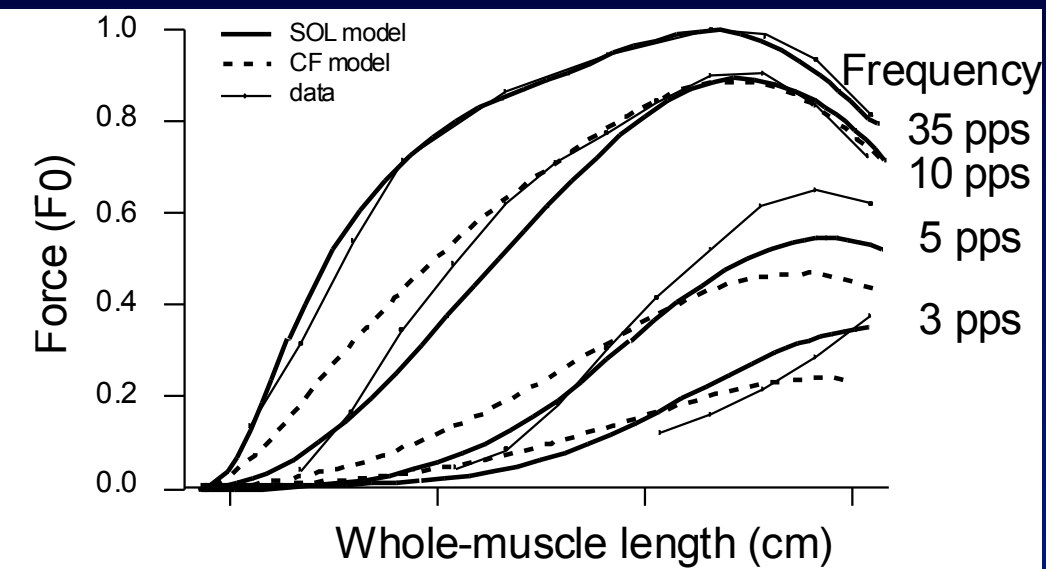
*Muscle accounts for the majority of animal mass and energy consumption. The evolutionary pressures to find and exploit any advantage are huge.*

In order to produce active force:

- Myofilaments overlap
- Myosin heads cocked
- Binding sites exposed

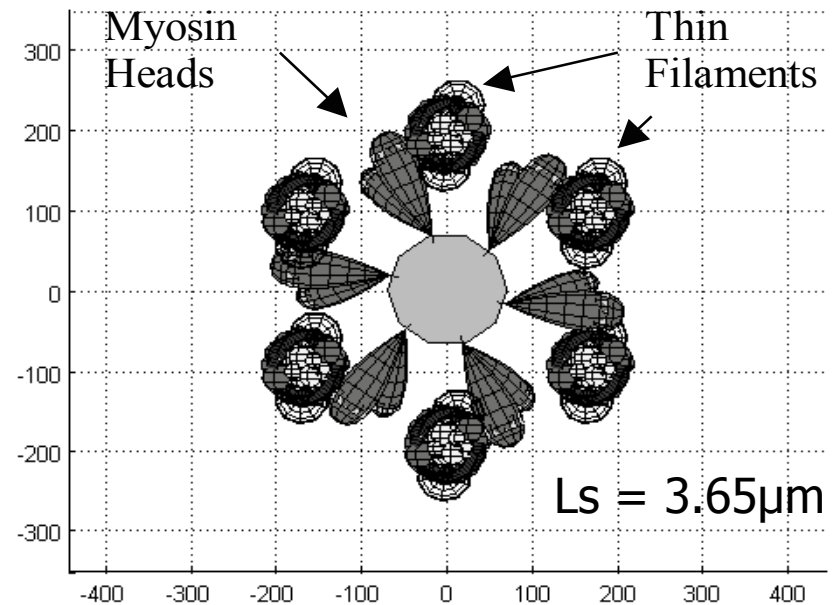
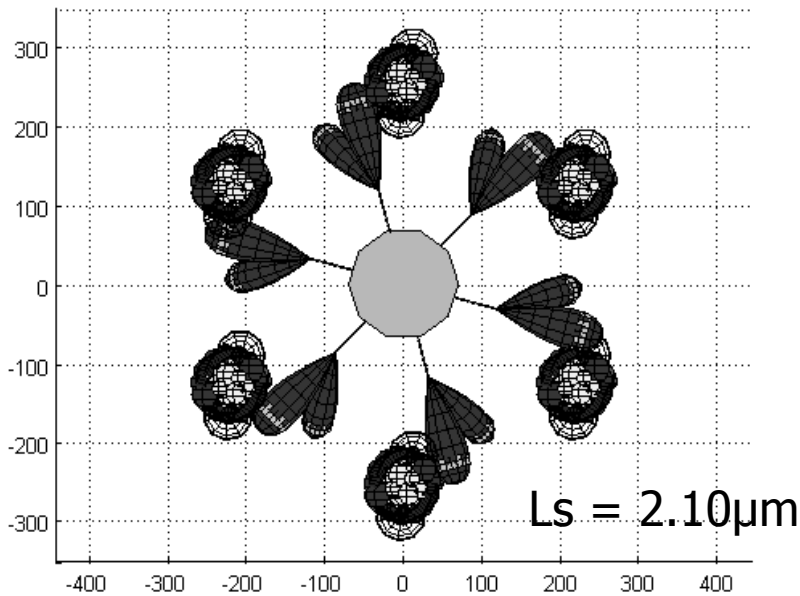
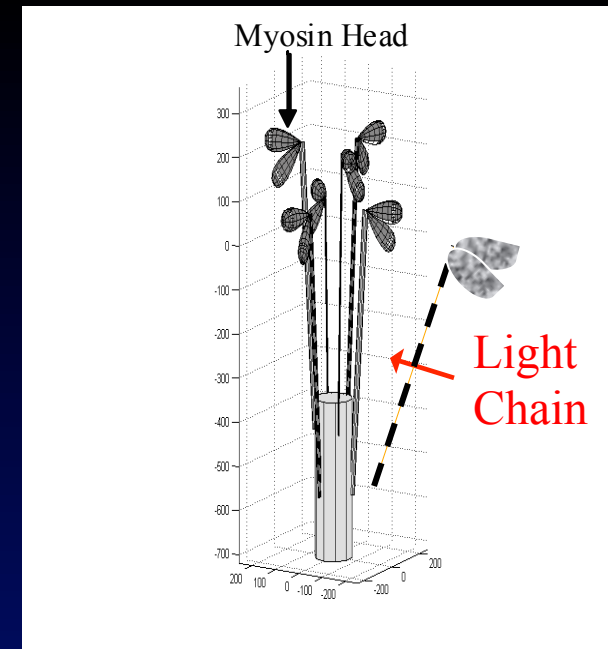


# ...and other nonlinear properties of muscle actuators



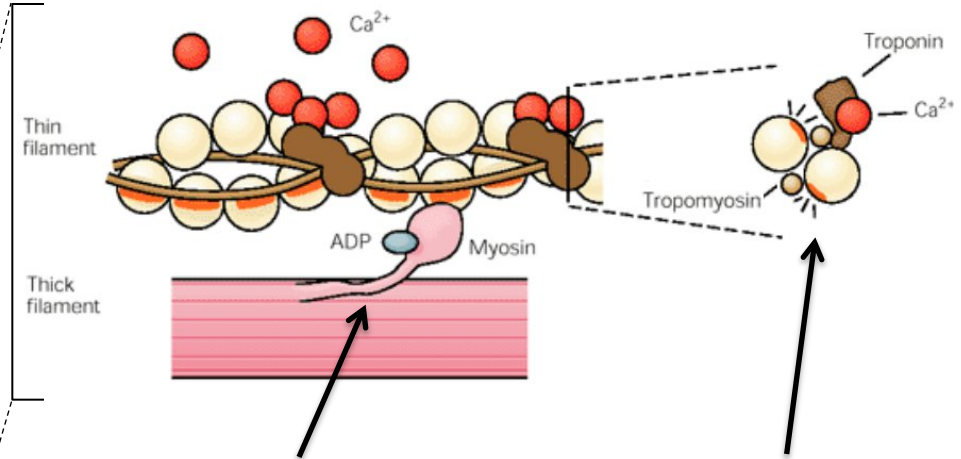
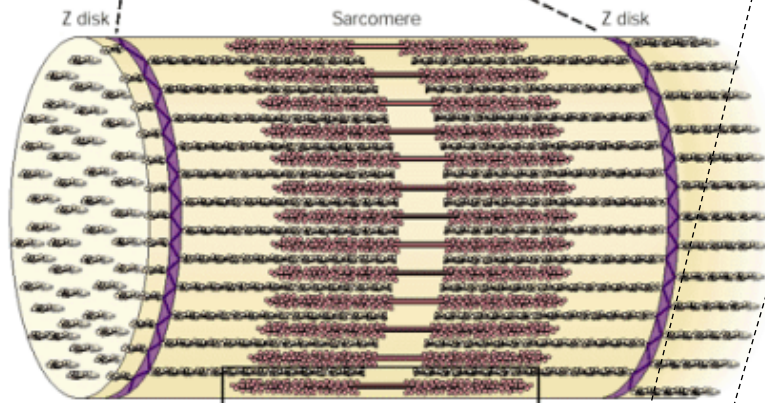
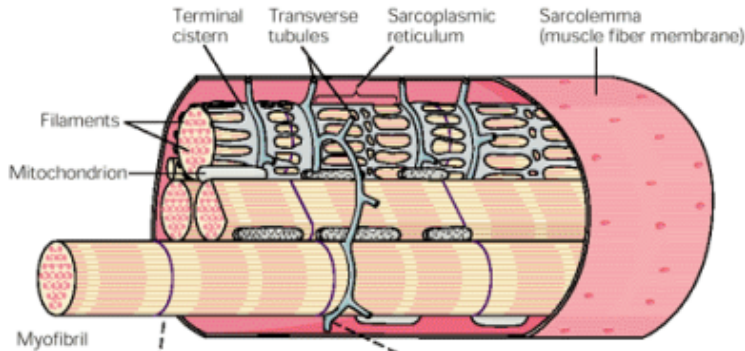
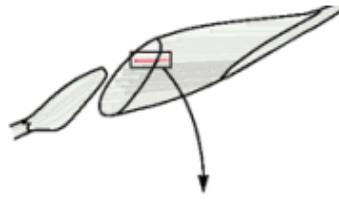
# Potential

Myosin light-chain phosphorylation shifts resting position of myosin heads



In order to produce active force:

- Myofilaments overlap
- Myosin heads cocked
- Binding sites exposed



**Cocked myosin head**

ATP required to release myosin head and move it to the cocked state

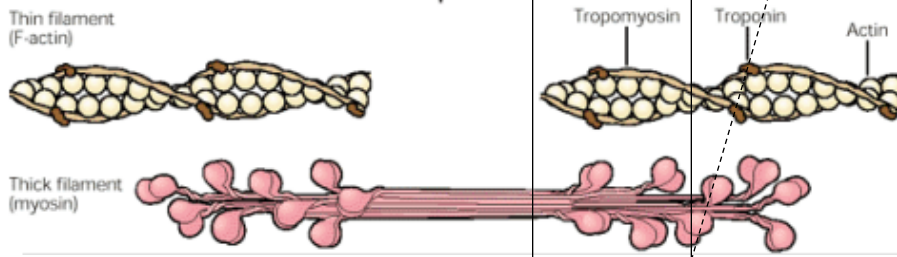
**Exposed actin site**

Activation requires action potentials and calcium release; ATP used to pump ions back.

➤ **E<sub>xb</sub>** depends on the number of cross-bridges and shortening velocity

➤ **E<sub>a</sub>** depends on calcium flux in the sarcoplasm

➤ **E<sub>rec</sub>** ATP and PCr replenishment results in delayed recovery heat



# Virtual Muscle™

Cheng et. al. 2000

Song et. al. 2008

Tsianos et al. in press IEEE-TNSRE

## Neural Drive – U

Stimulation frequency

$$f_{env}(U)$$

$$\dot{f}_{eff}(t, L, Af, f_{env})$$

Rise and fall time

Sag

$$\dot{S}(t, f_{eff})$$

Yield

$$\dot{Y}(t, V)$$

Weighting function

Force-Length Force-Velocity

$$W(t, U)$$

$$Af(L, f_{eff}, S, Y, W)$$

$$FL(L)$$

$$FV(V, L)$$

Activation-force relationship

$$F_{CE} = FL * FV * Af$$

Active contractile force

Parallel elastic element

$$F_{PE1}(L, V)$$

Thick filament compression

$$F_{PE2}(L)$$

$$F_{PE} = F_{PE1} + Af * F_{PE2}$$

Total parallel elastic force

Energy-Velocity

$$EV(V)$$

$$F_{Total} = F_{CE} + F_{PE}$$

Total contractile element force

mass

Series elastic element

Total muscle force

$$\dot{E}_{xb}(Af, FL, EV)$$

Energy rate related to cross-bridge cycling

$$\dot{E}_{initial} = \dot{E}_{xb} + \dot{E}_a$$

Initial energy consumption rate

$$\dot{E}_{rec} = R * \dot{E}_{initial}$$

Recovery energy rate

= Total energy rate

$$\dot{E}_a(f_{env})$$

Energy related to excitation

# Virtual Muscle

(analogous to Biceps Long)

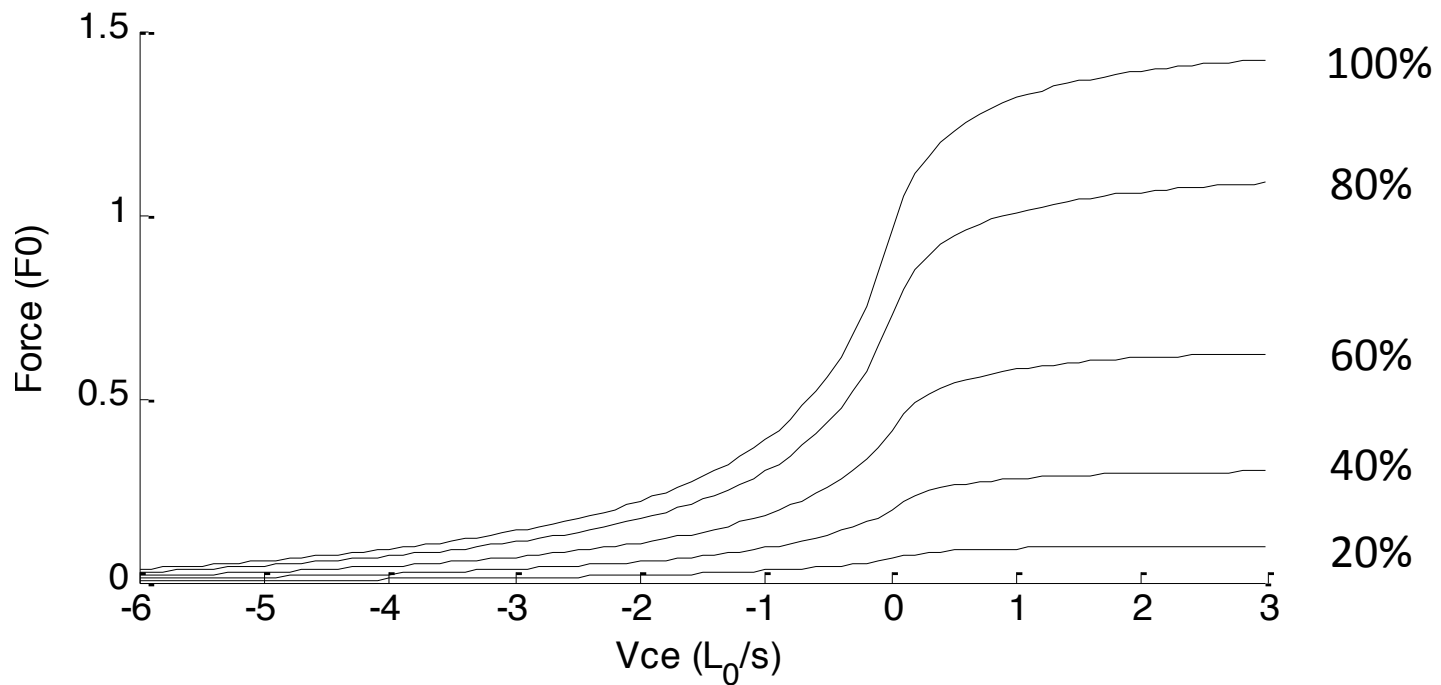
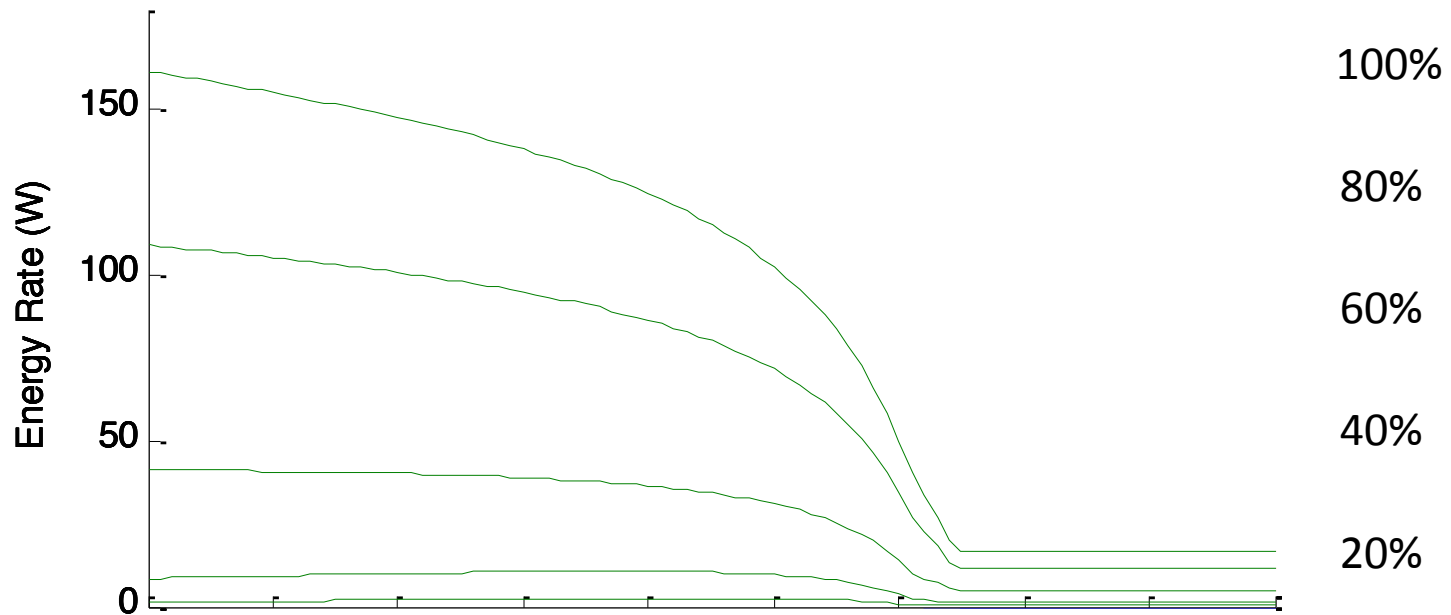
40% Slow twitch

60% Fast twitch

Mass = 300g

F0 = 600N

L0 = 16cm



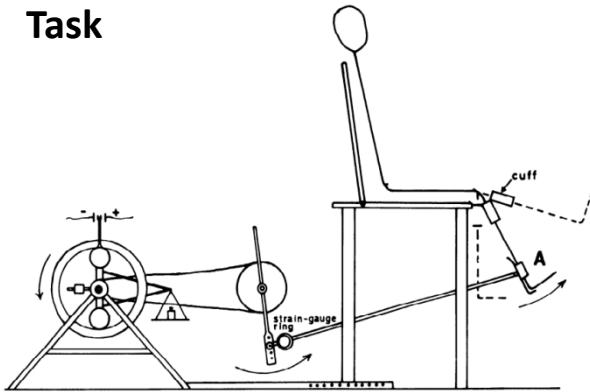


# Validation of Energetics Model

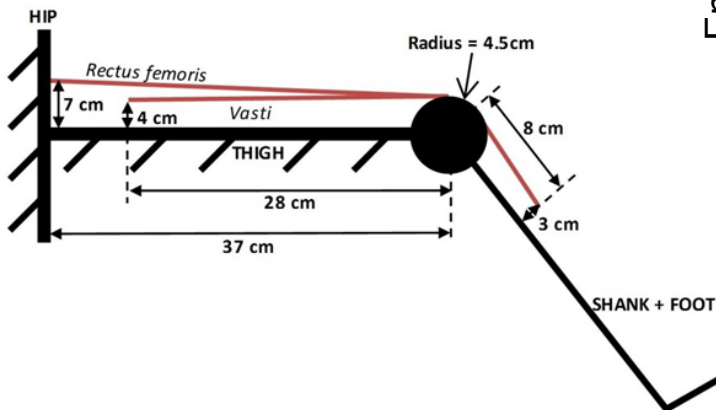
## Dynamic knee extension

(Andersen et al., 1985; Gonzalez-Alonso et al., 2000)

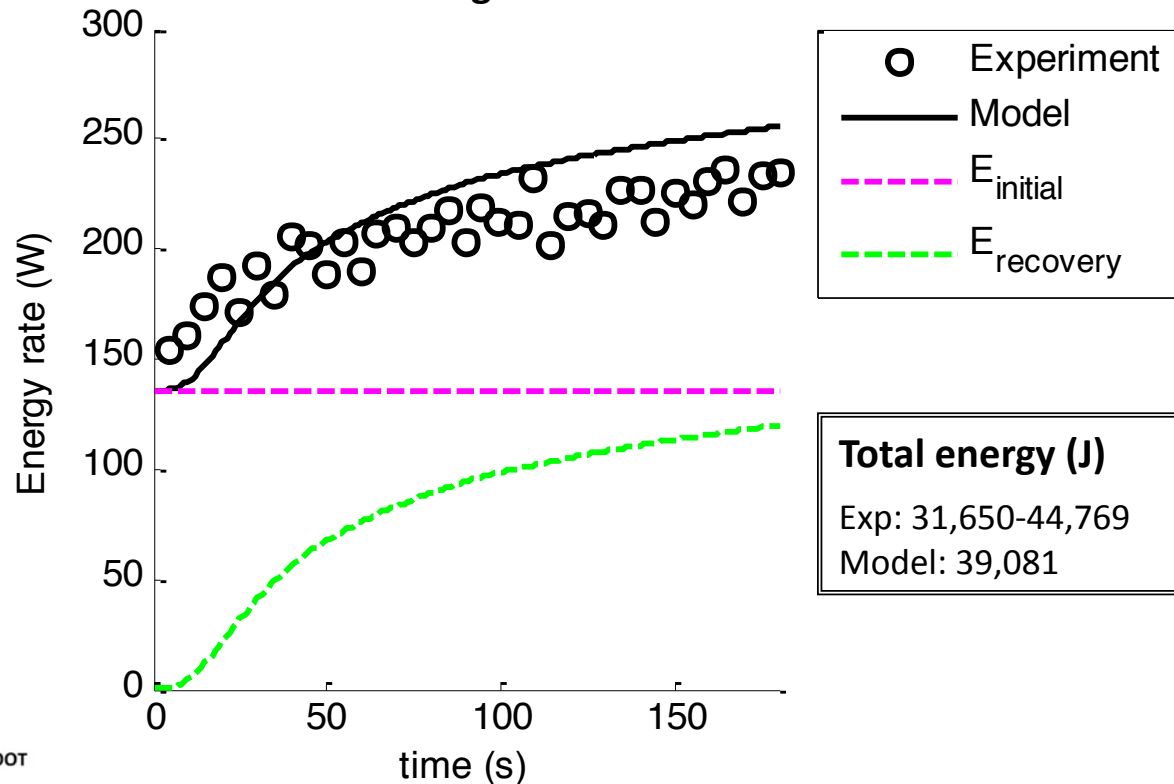
### Task



### Model

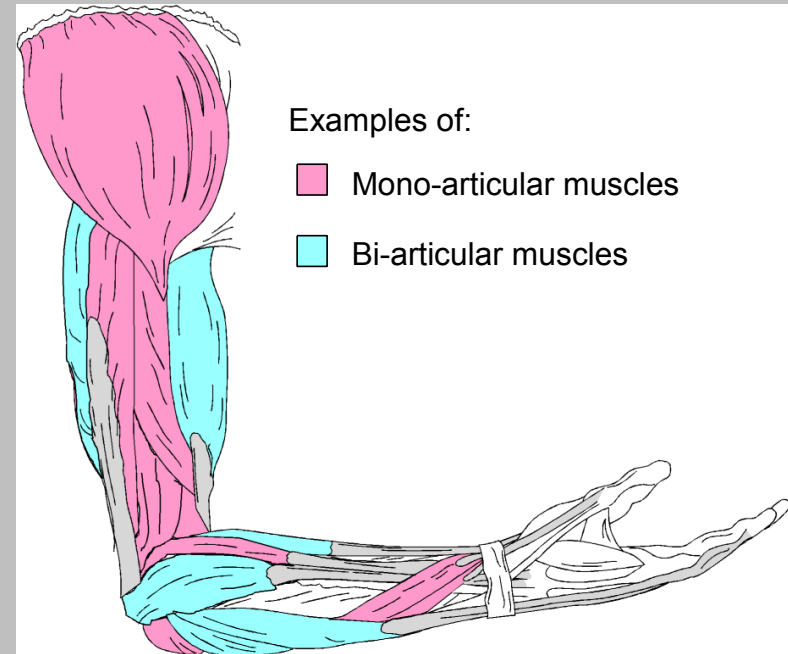
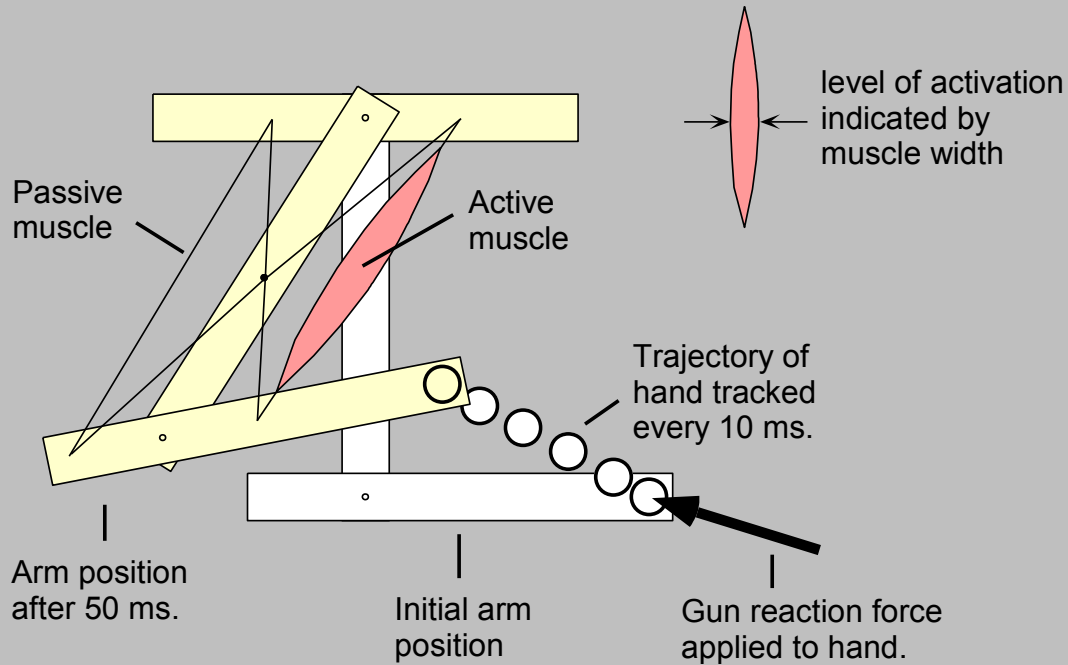


### Energetics



# Model System to Study Preflexes

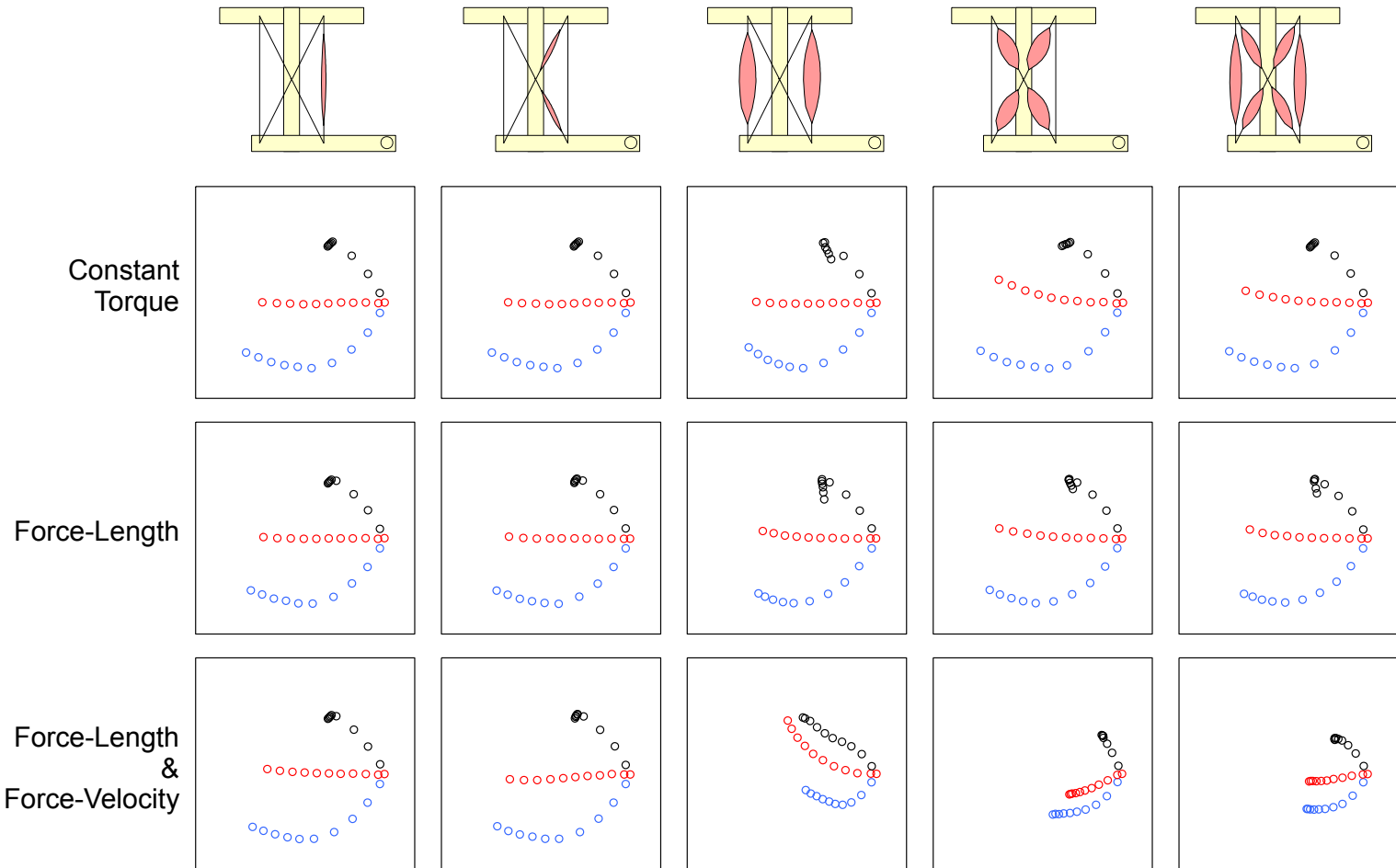
Sample Simulation (50 ms):



# The Effectiveness of Preflexes

## MUSCLE ACTIVATION PATTERNS

INTRINSIC PROPERTIES OF MUSCLE



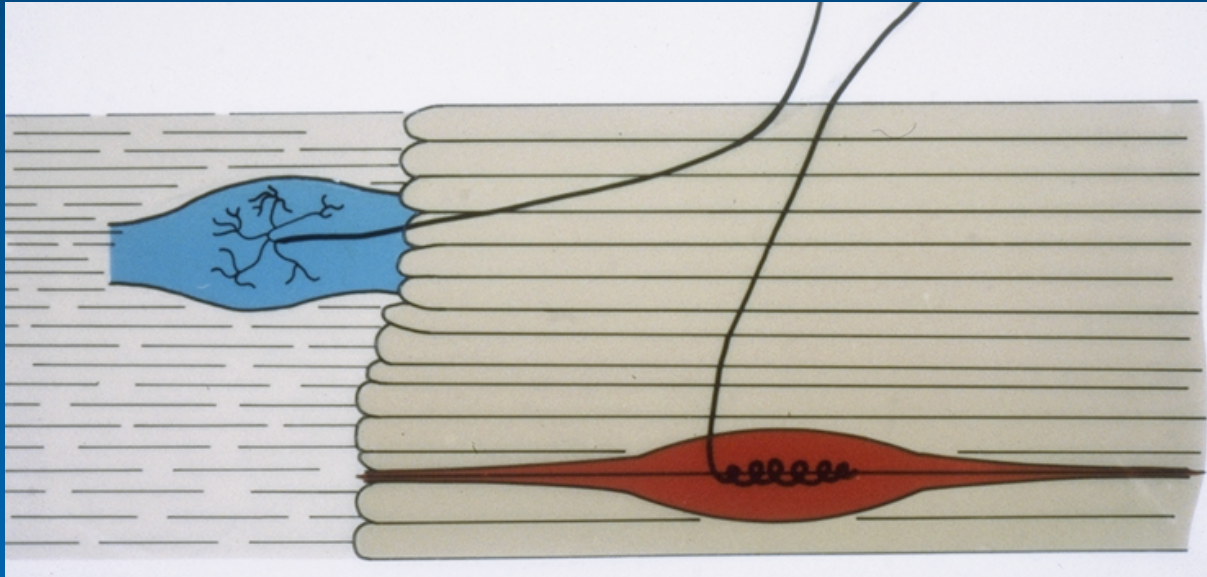
# Sensing & Control: Underlying Mechanisms

- Resolution: Populations of receptors
- Dynamic Range: Predictive gain control
- Signal Processing: Integrative
- Feedback: Multimodal convergent/divergent
- Control: Programmable regulator (MIMO)

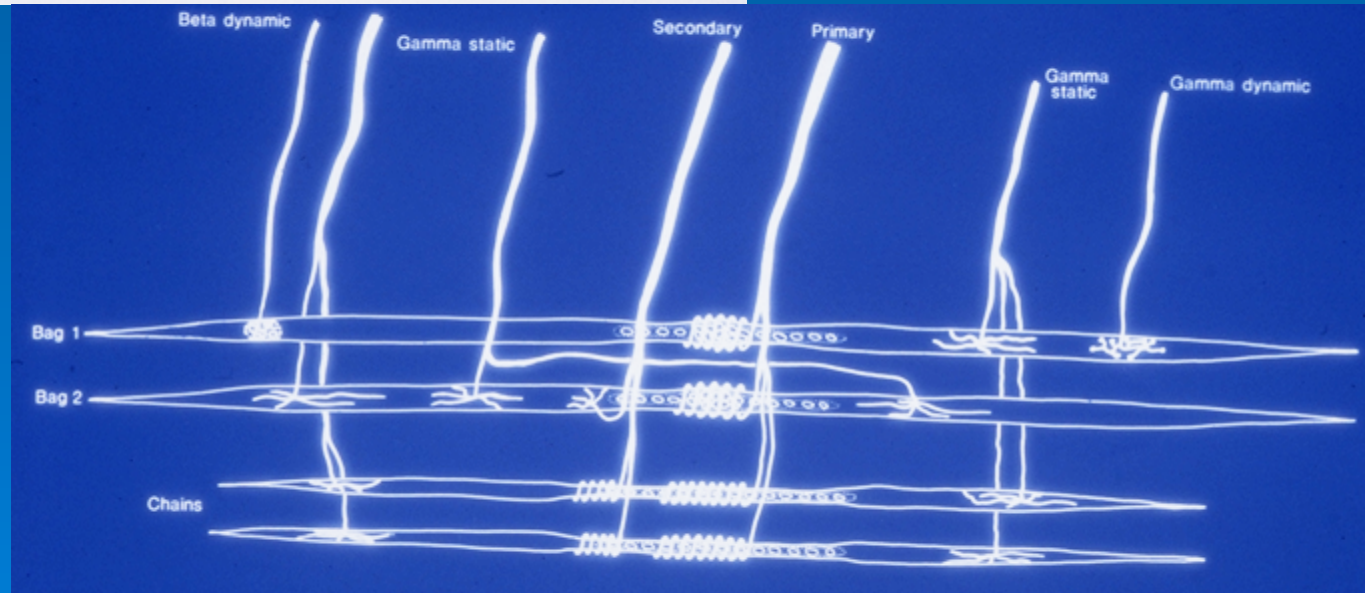
*Fast & accurate movement is what distinguishes even primitive animals from plants. Servocontrol is too limited for multiarticular organisms and inverse models and optimal control are not feasible analytically.*

*Animals use hierarchical and “good enough” controls.*

# Muscles have hundreds of proprioceptive sense organs

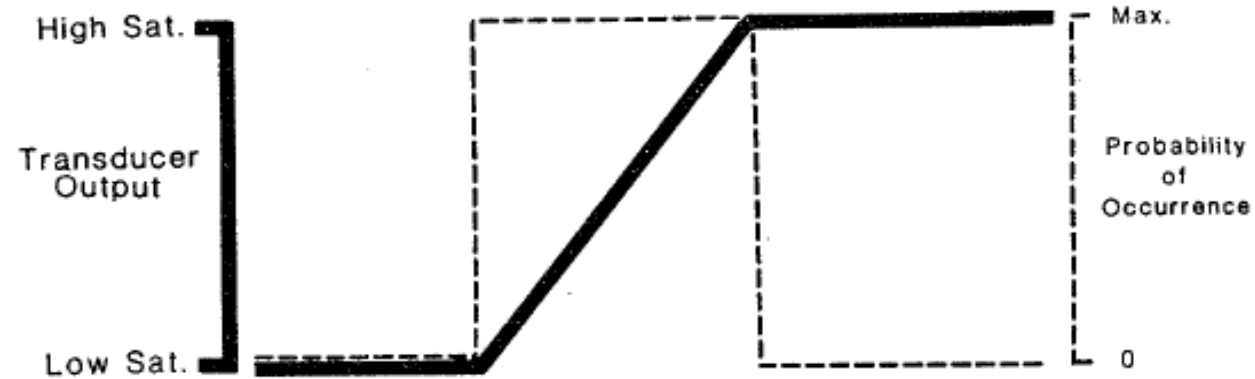


Spindles are very complex and provide most sense of posture and movement



# Fusimotor System as Optimal Sensor Control

A. LINEAR:



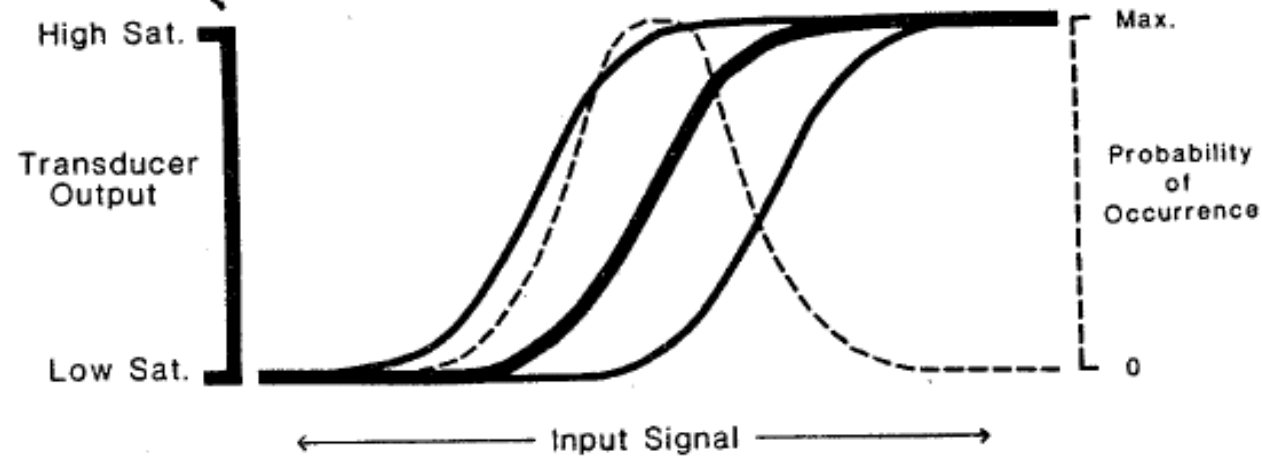
$$E = n + T(S),$$

$$\Delta E = \frac{dT}{dS} \Delta S = \frac{dT}{dS} \frac{1}{P(S)} = \text{const.}$$

$$\frac{dT}{dS} \sim P(S)$$

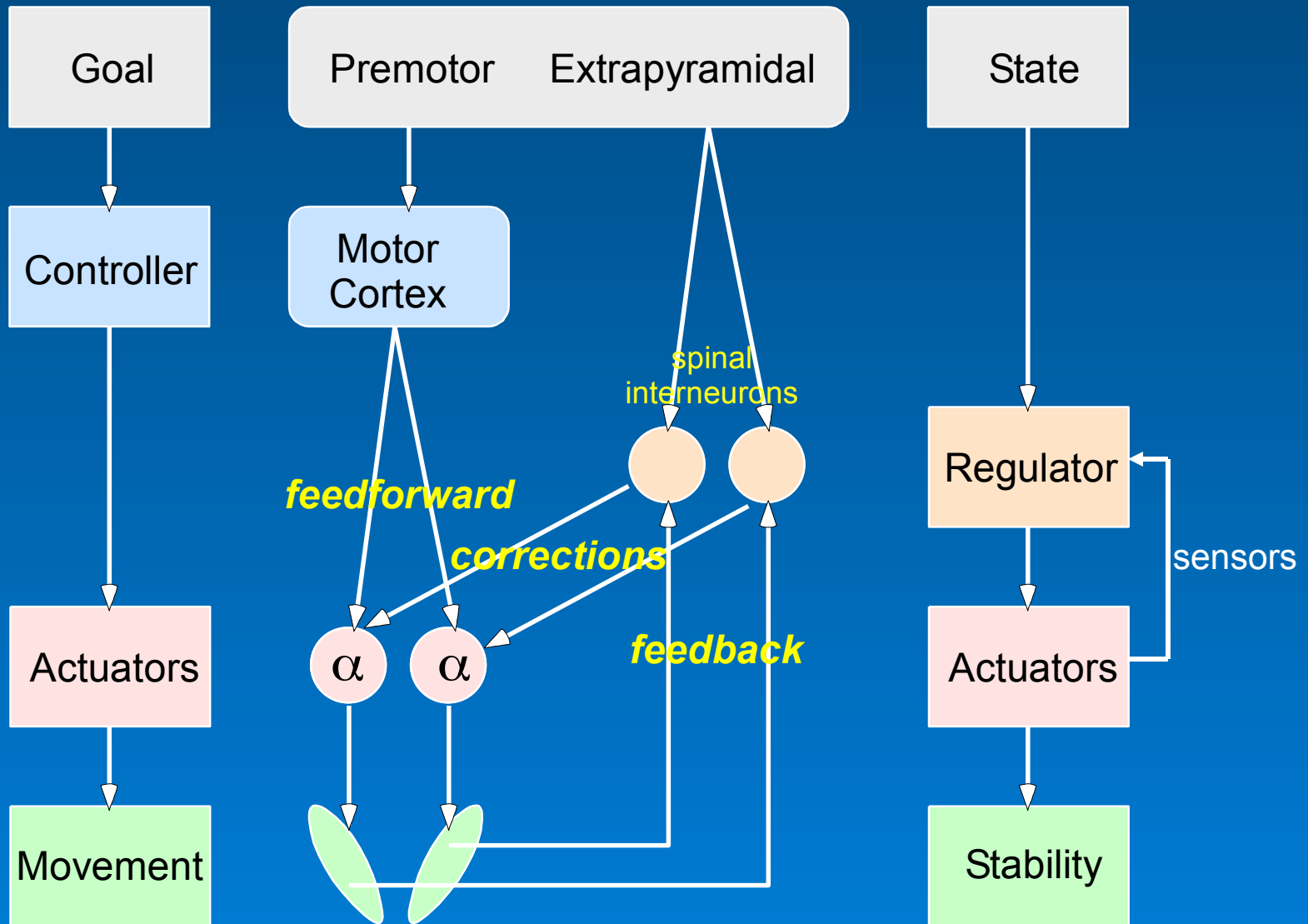
$$T(S) \sim \int_{-\infty}^S P(S) ds.$$

B. SIGMOIDAL:

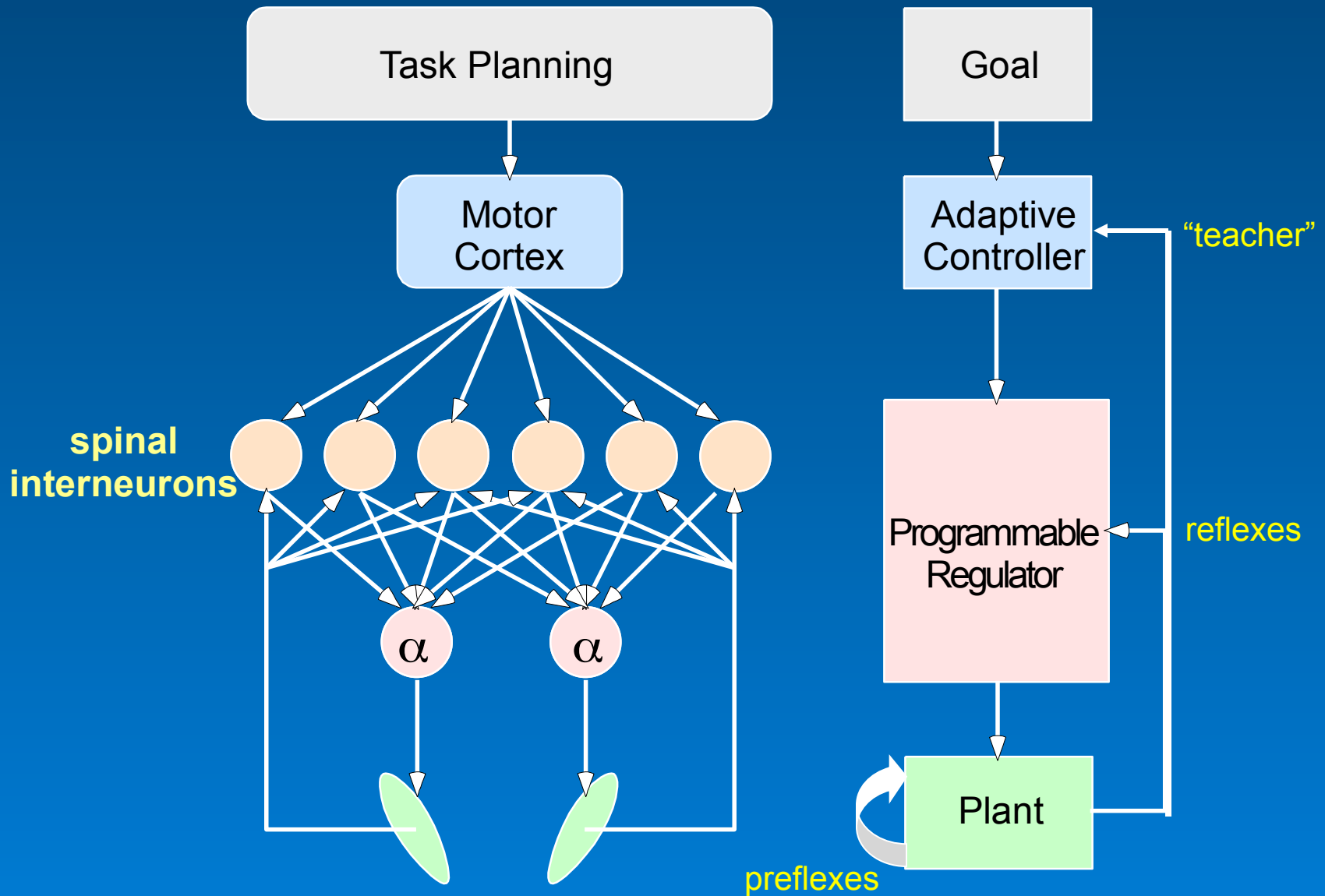


WB Marks, Appendix: Spindle Transduction Properties  
 in GE Loeb (1984) The Control and Responses of Mammalian Muscle Spindles During  
 Normally Executed Motor Tasks, Exer. & Sport Sci. Revs. 12:157-204.

# Textbook Robotics & Biology



# Biomimetic Hierarchical Control

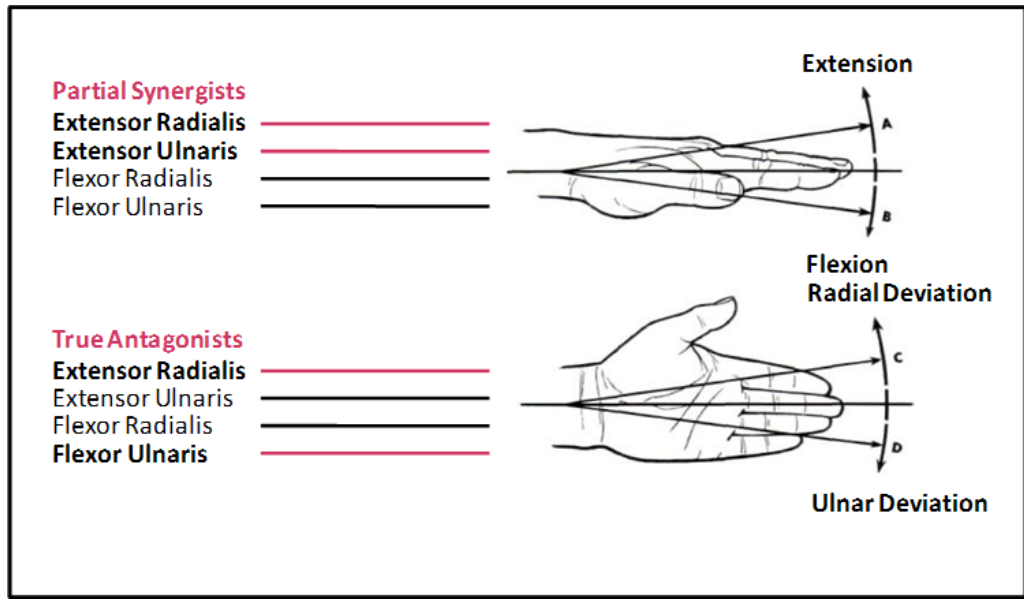
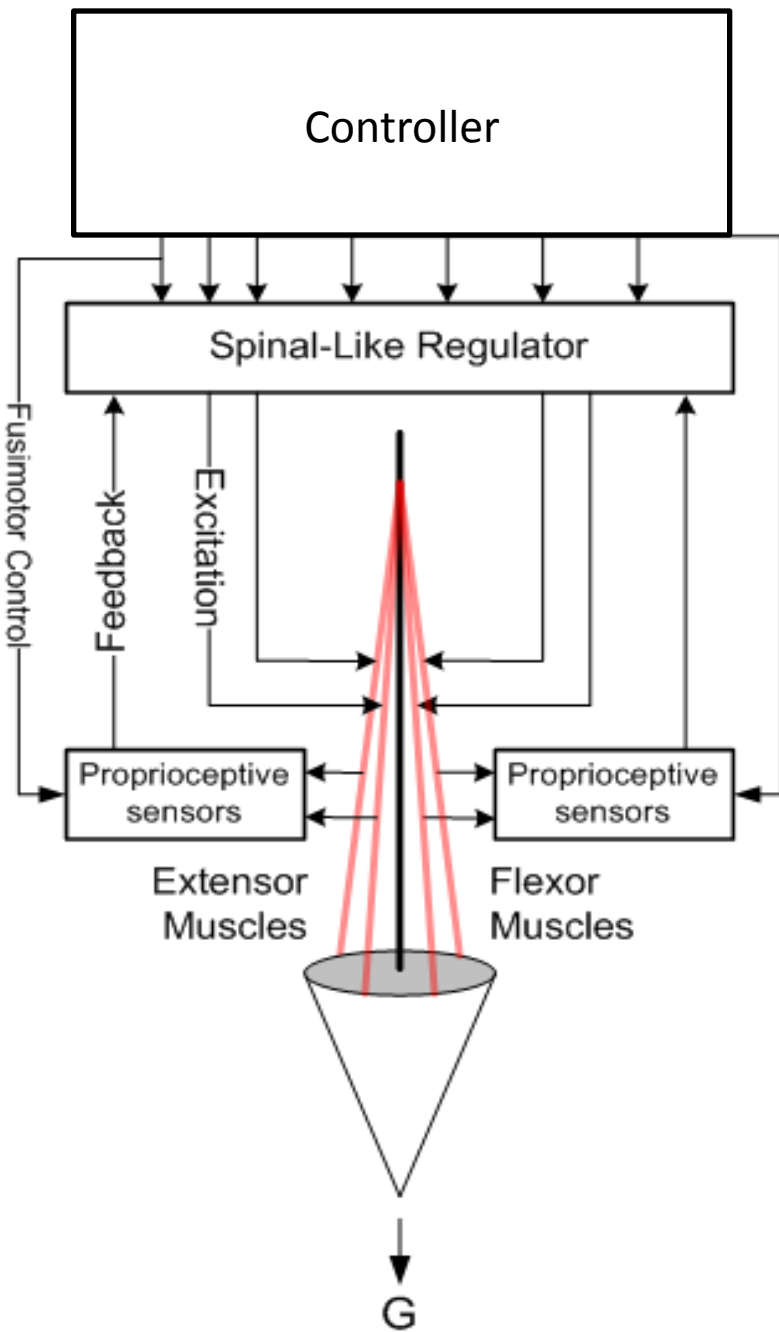




# Biomechanical Model

## Simplified 2-axis, 4-muscle, Wrist Joint

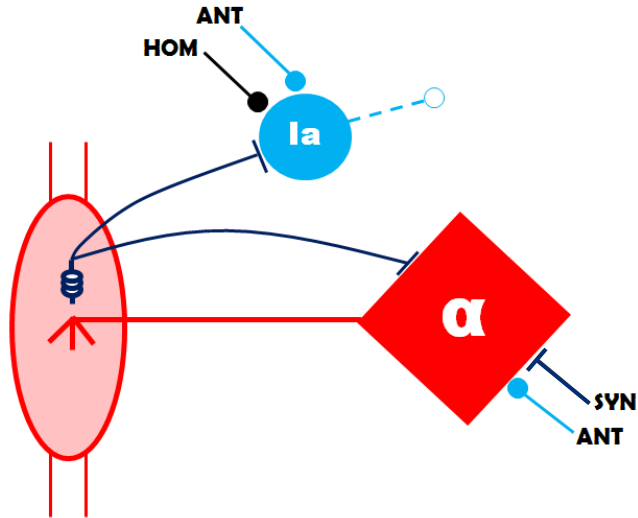
Components of the Simulation Environment
Skeletal Model <i>SimMechanics Toolbox, SimuLink</i>
Muscle Model <i>Virtual Muscle [Cheng, Brown, Loeb, 2000]</i>
Muscle Spindle Model <i>[Mileusnic, Brown, Lan &amp; Loeb, 2006]</i>
Ensemble GTO Model <i>[Crago, Houk &amp; Rymer, 1982]</i>
MSMS <i>[Davoodi et al, 2003]</i>



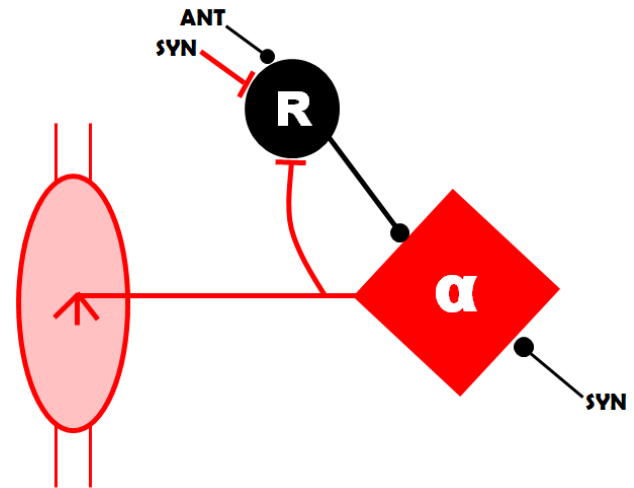
Raphael, G., Tsianos, G.A. and Loeb, G.E. Spinal-like regulator facilitates control of a two degree-of-freedom wrist. *J. Neuroscience* 30:9431-9444. July. 2010.

# Classical spinal circuits

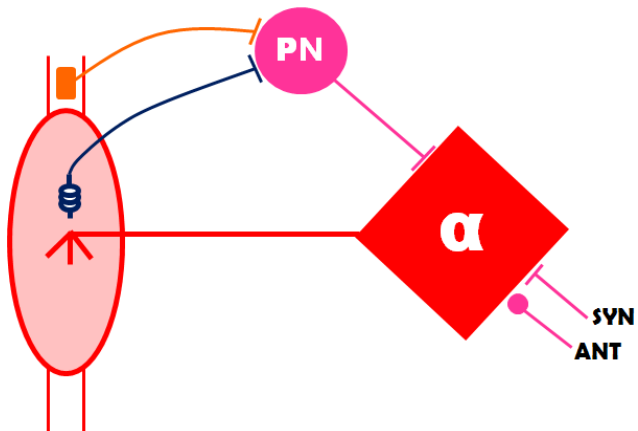
## Stretch reflex and Ia inhibitory



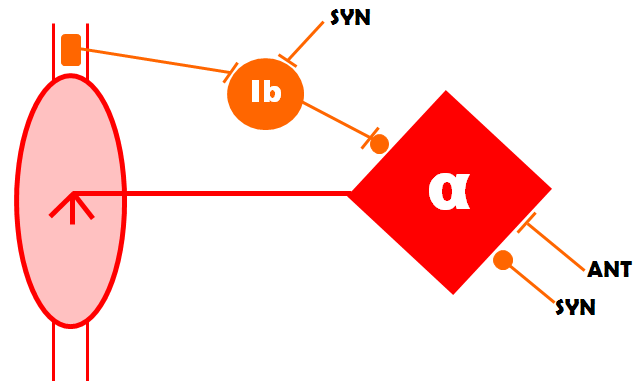
## Renshaw



## Propriospinal

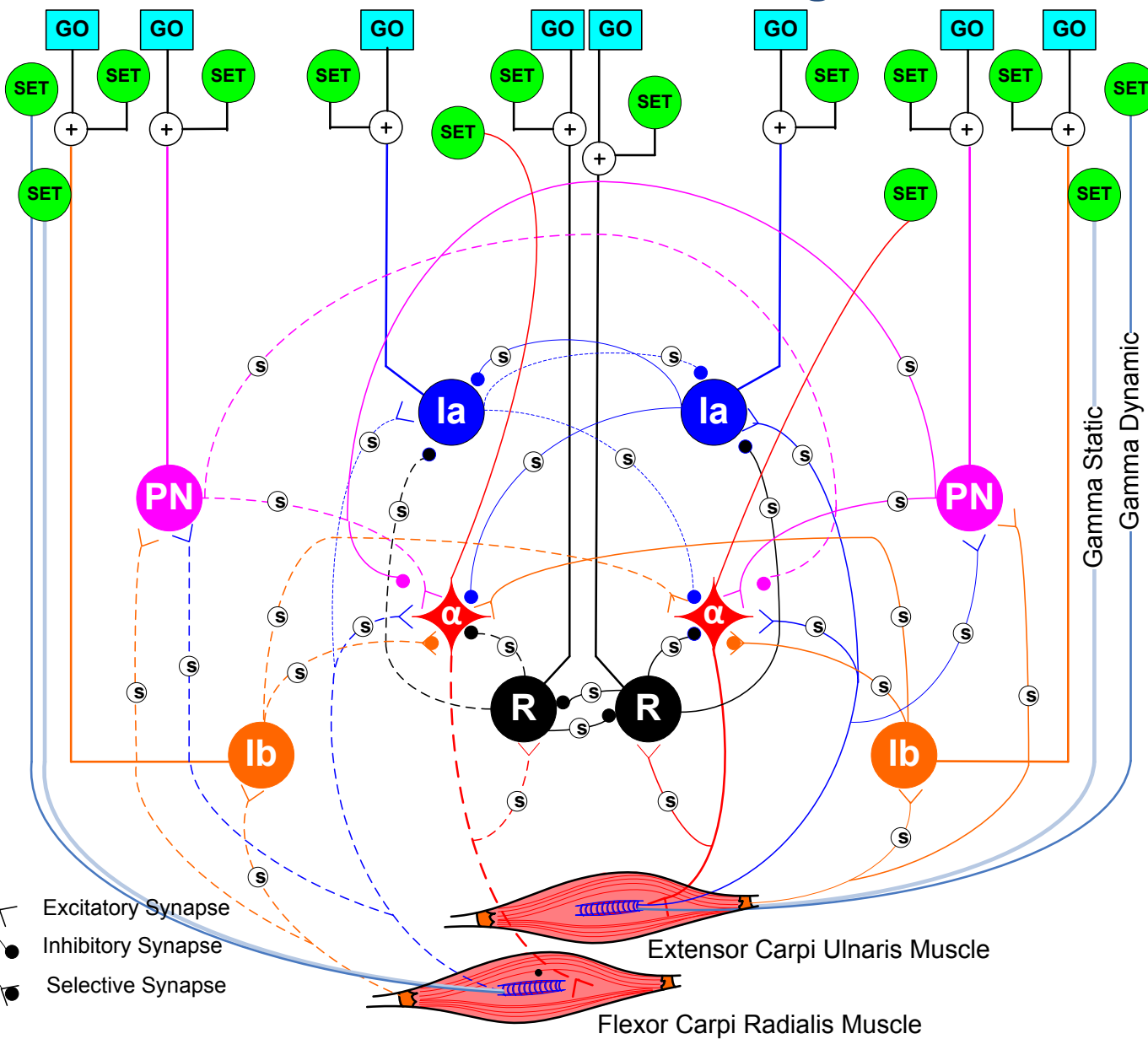


## Ib



# Partial view of the Integrated Spinal Cord Model

## “True-Antagonists”

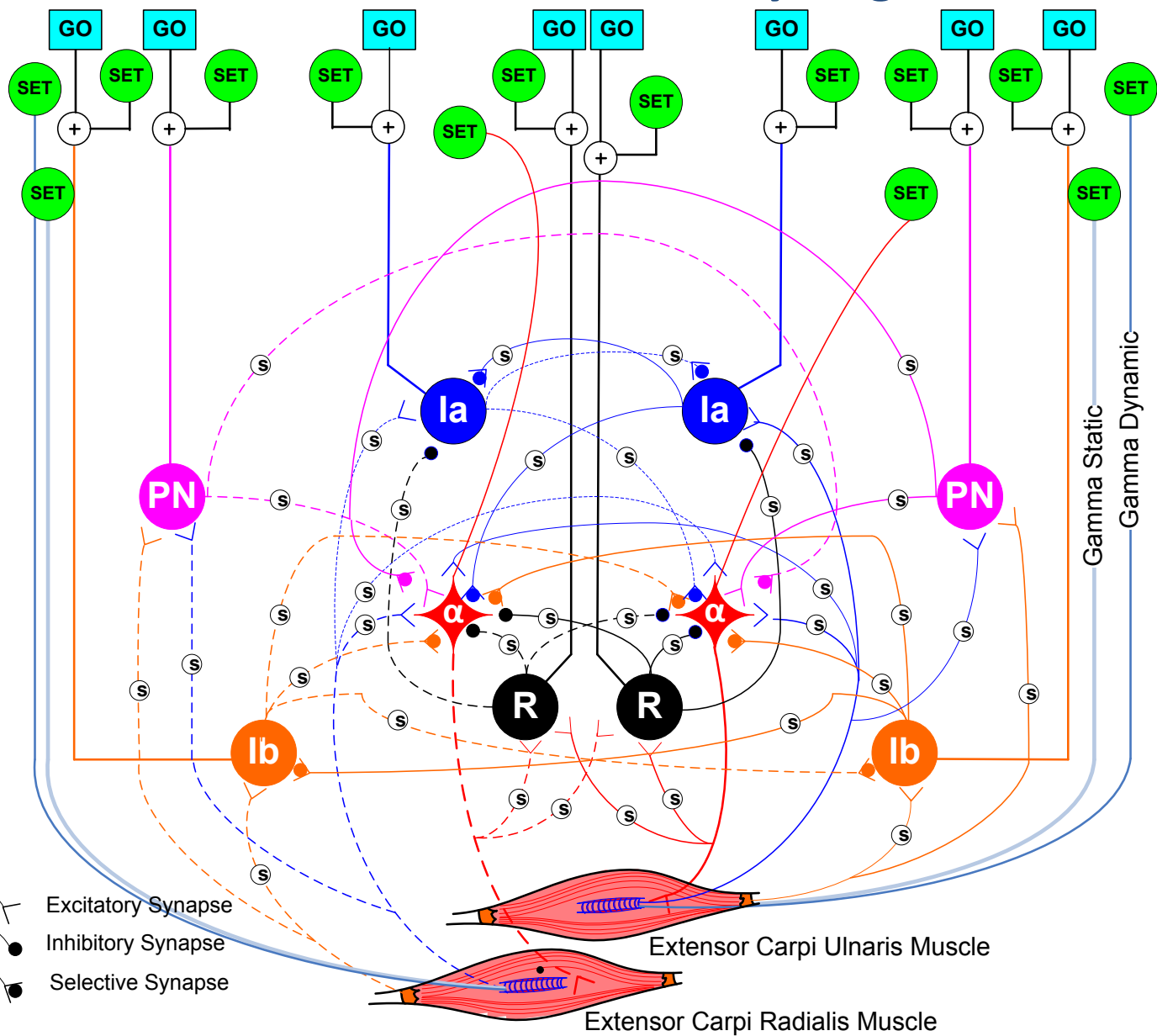


### Modeled Pathways

1. Propriospinal
2. Monosynaptic Ia
3. Reciprocal Ia
4. Renshaw
5. Ib inhibitory

# Partial view of the Integrated Spinal Cord Model

## “Partial-Synergists”

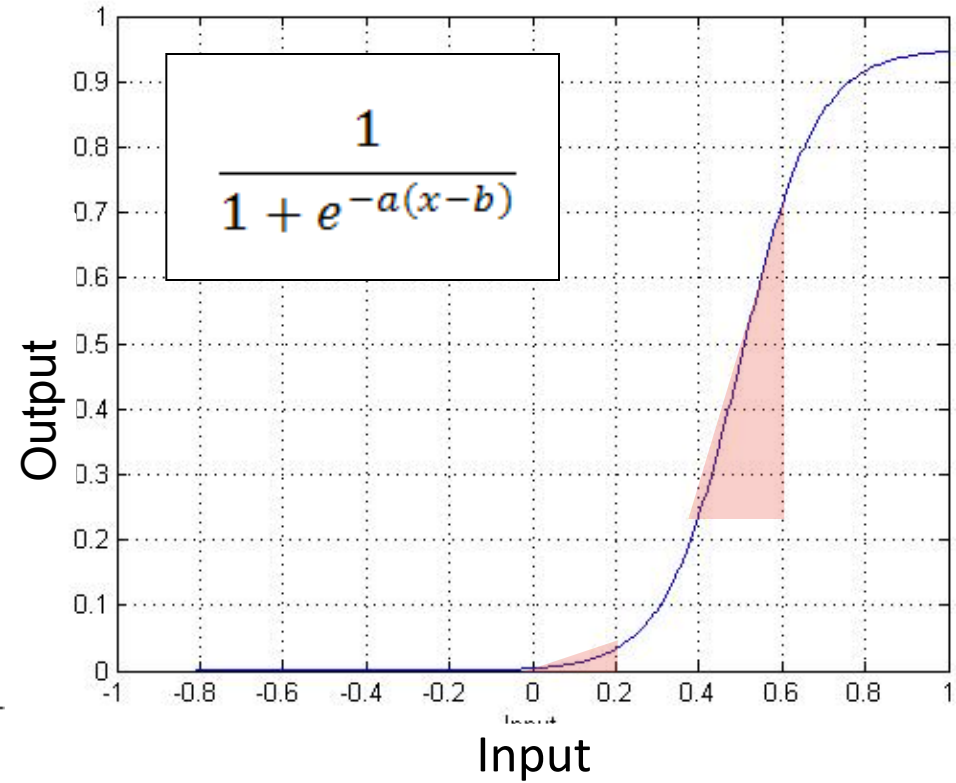
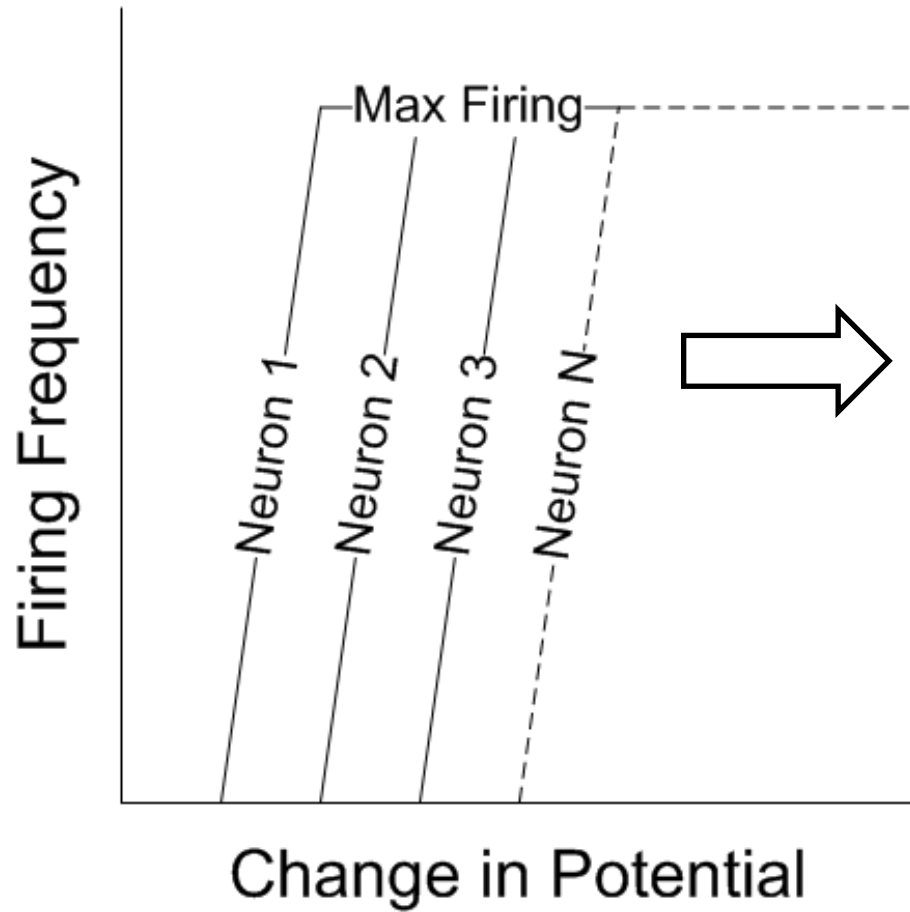


### Modeled Pathways

1. Proprioceptive
2. Monosynaptic Ia
3. Reciprocal Ia
4. Renshaw
5. Ib inhibitory

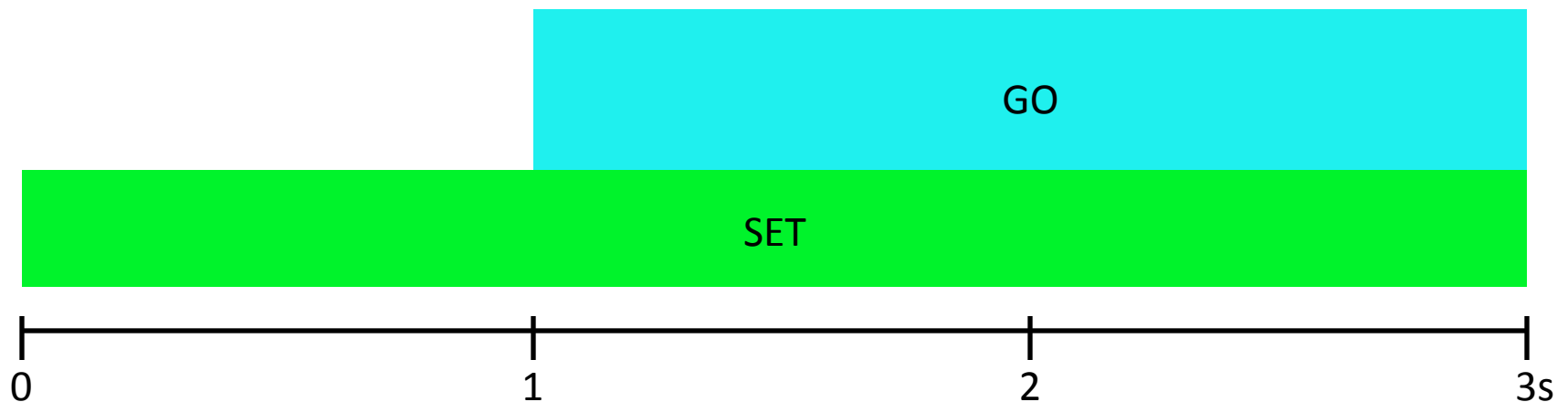
Excitatory Synapse  
 Inhibitory Synapse  
 Selective Synapse

# Computational Model of the Interneuron

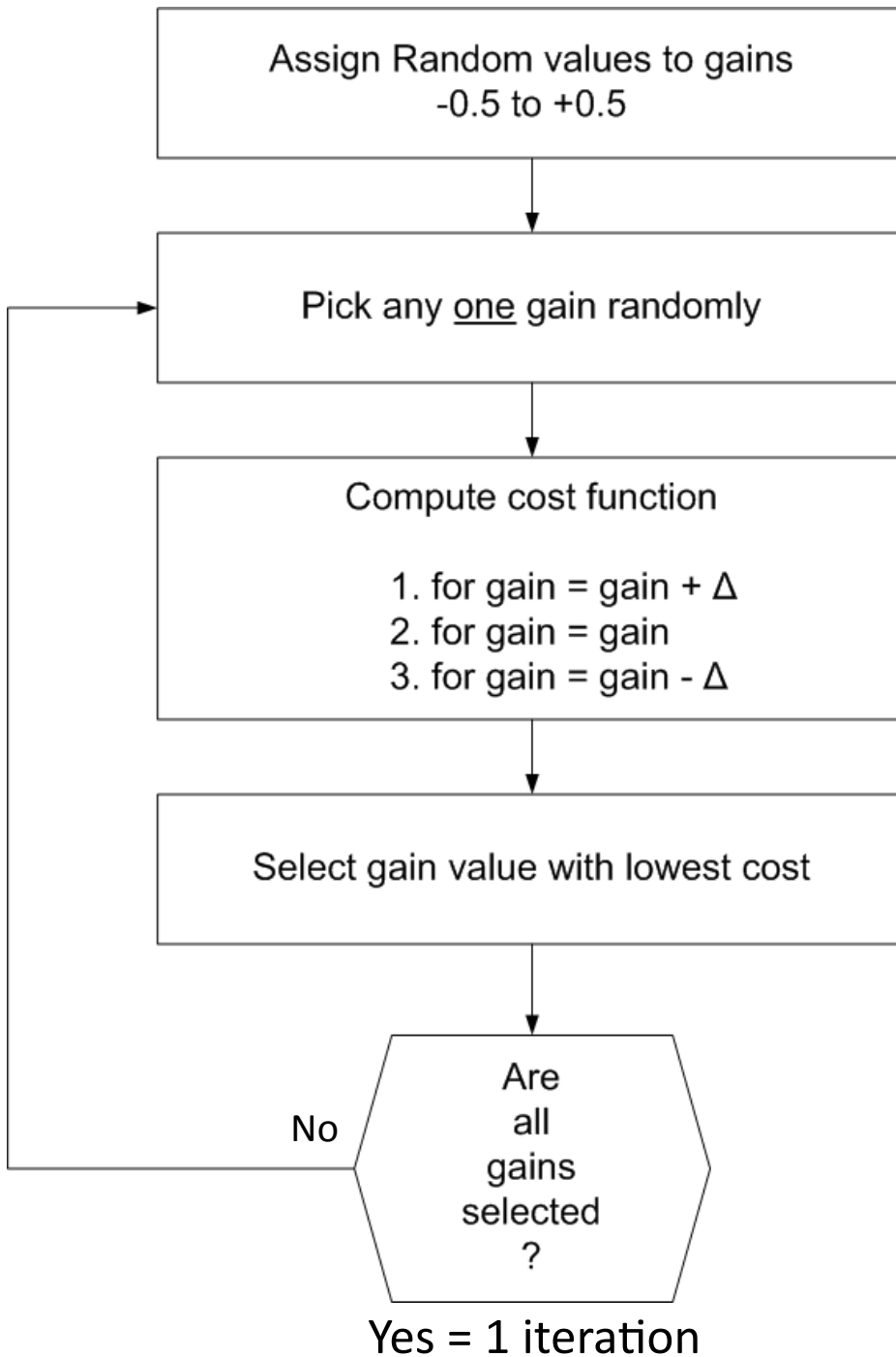


# Command Space = 184 dimensions

Constant Inputs	SET Inputs	GO Inputs
<ul style="list-style-type: none"><li>• Presynaptic Inhibition</li></ul>	<ul style="list-style-type: none"><li>• 140 Neural pathway gains</li><li>• 8 Fusimotor inputs</li><li>• Bias to 16 Interneurons &amp; 4 Motoneurons</li></ul>	<ul style="list-style-type: none"><li>• Step input to 16 Interneurons</li></ul>



# Random Gradient Descent Optimization

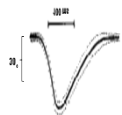
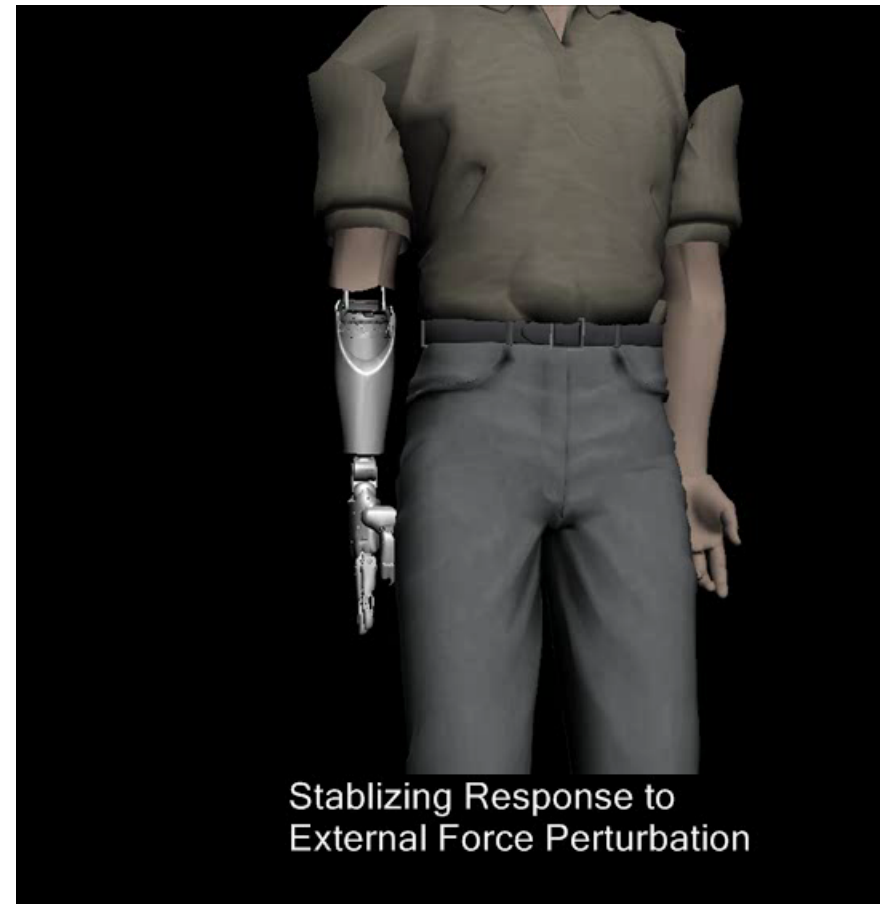
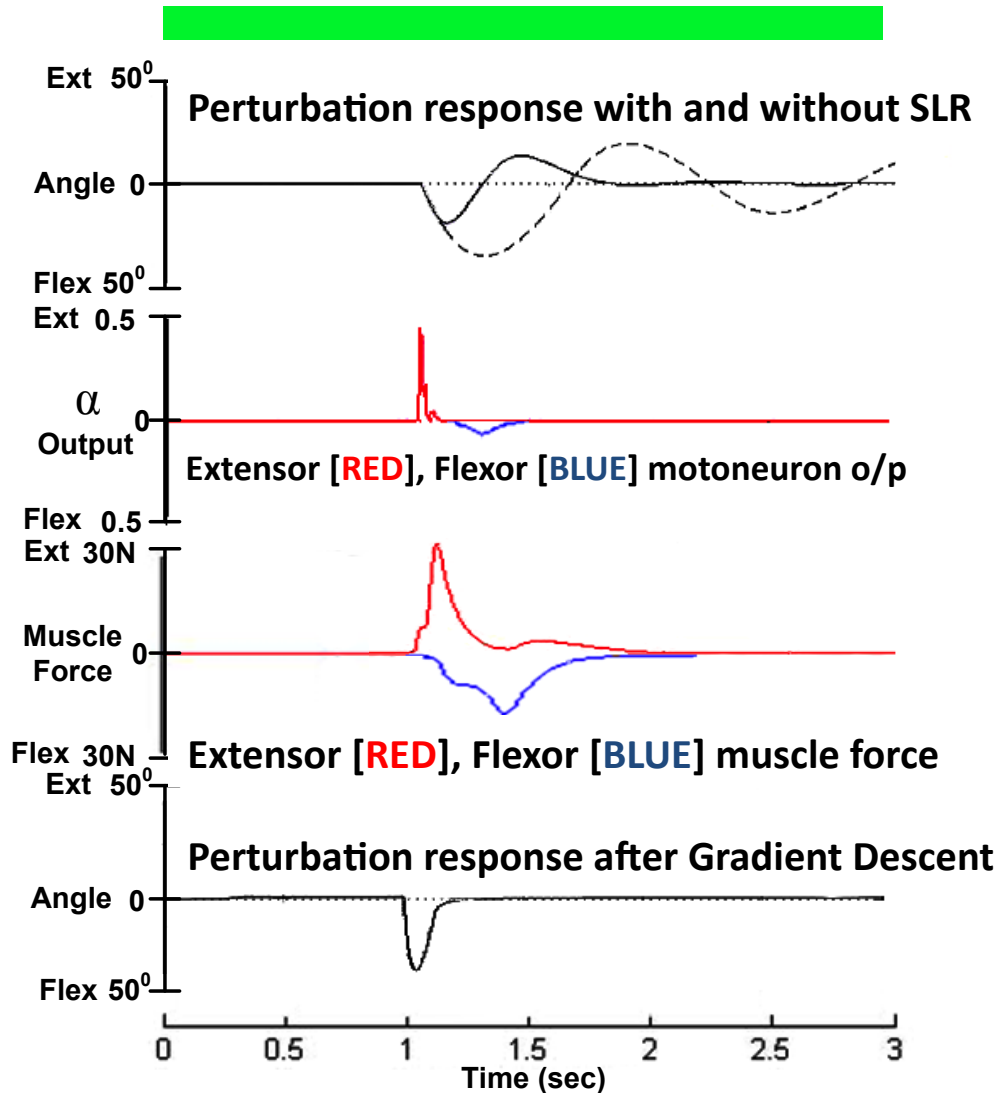


Method-1	Intuitive optimization !
Method-2	Random Gradient Descent
Method-3	Stochastic Hill Climbing

**Cost Function :**

$$\int (\text{Desired state} - \text{Actual state})^2$$

# Task 1: Stabilizing response to external force perturbation

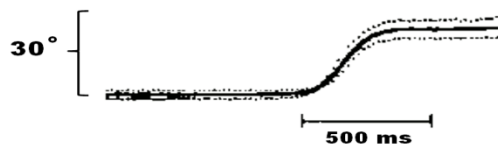
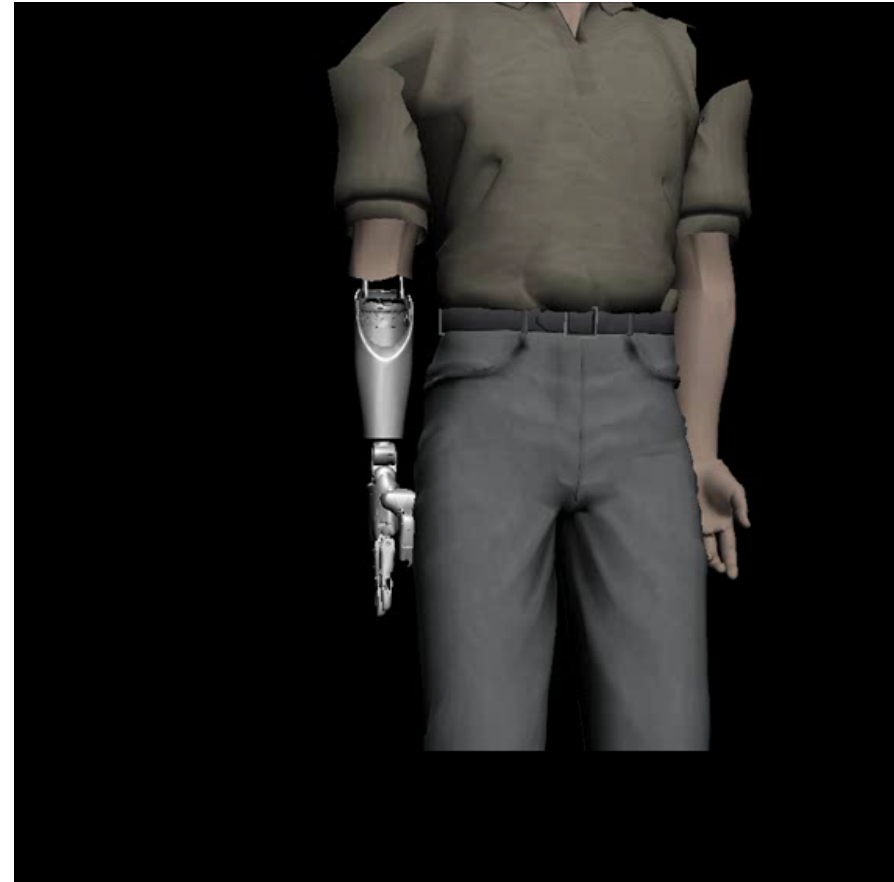
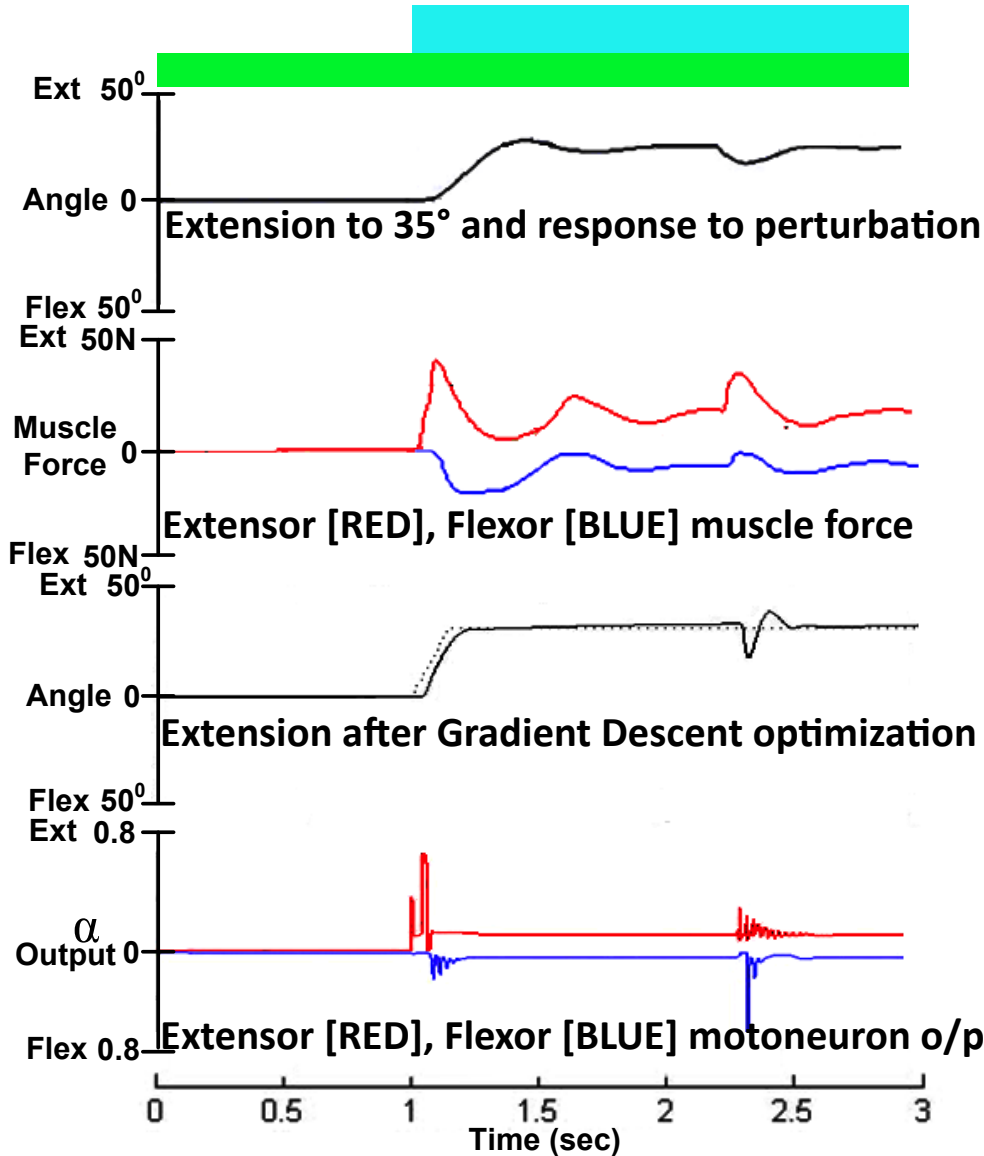


Liles S L 1985 J Neurophysiology

Activity of neurons in putamen during active and passive movements of wrist



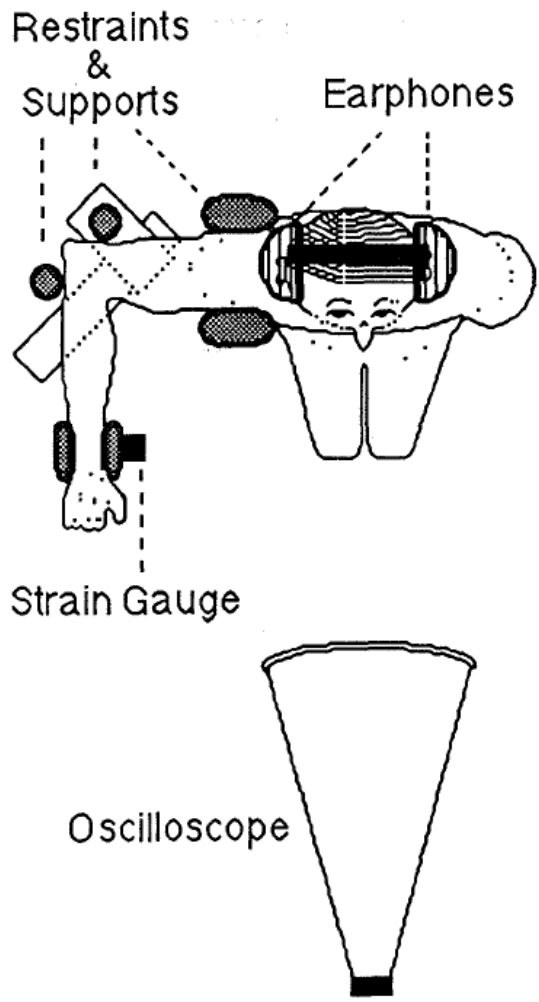
# Task 2: Rapid voluntary movement to a position target



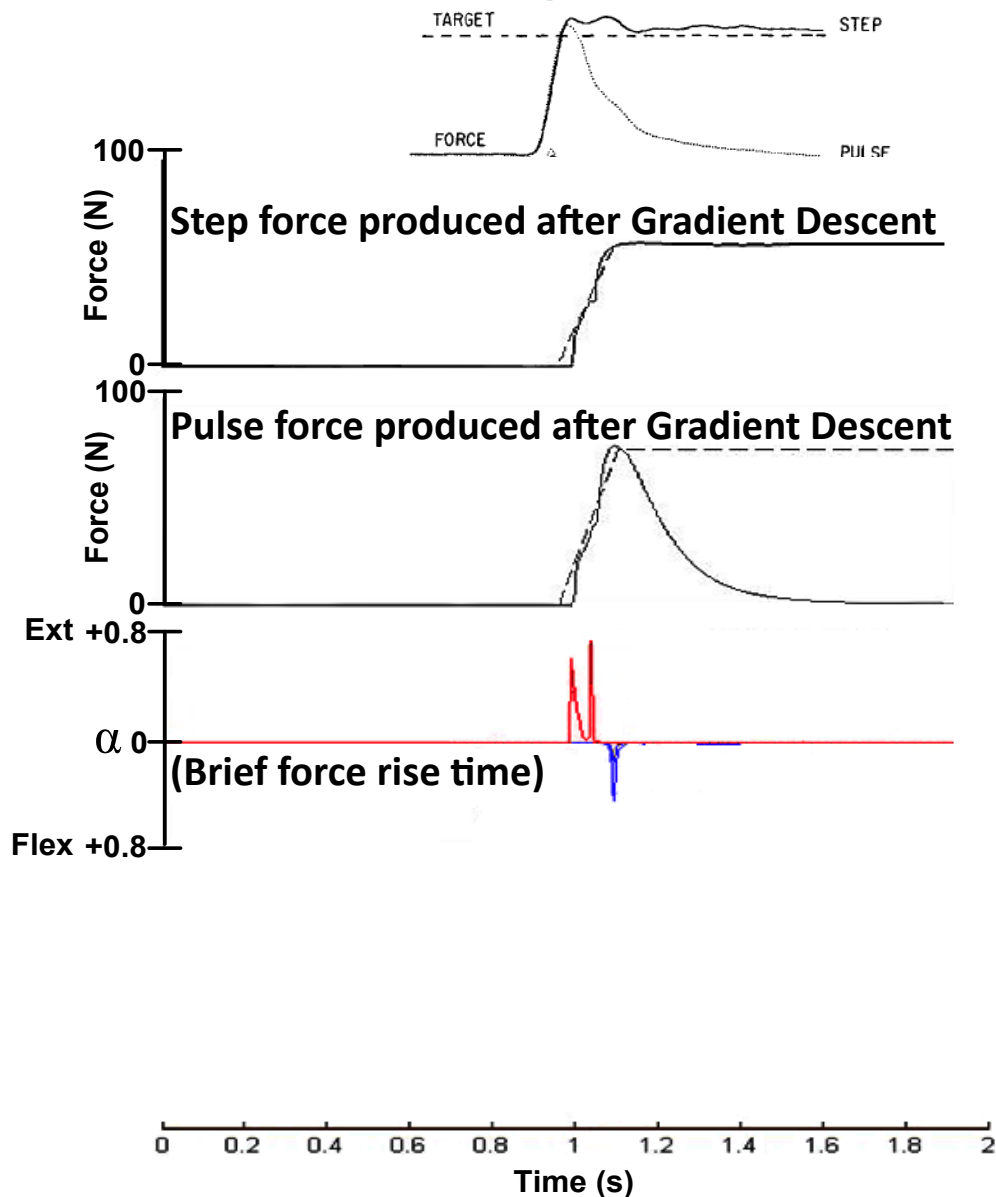
Liles S L 1985 *J Neurophysiology*

Activity of neurons in putamen during active and passive movements of wrist

# Task 3: Voluntary isometric force to a target level

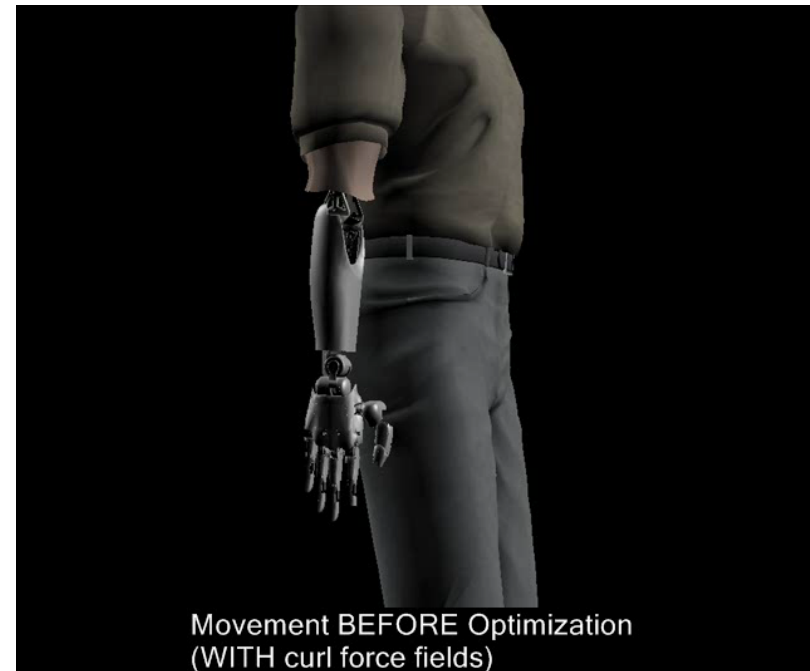
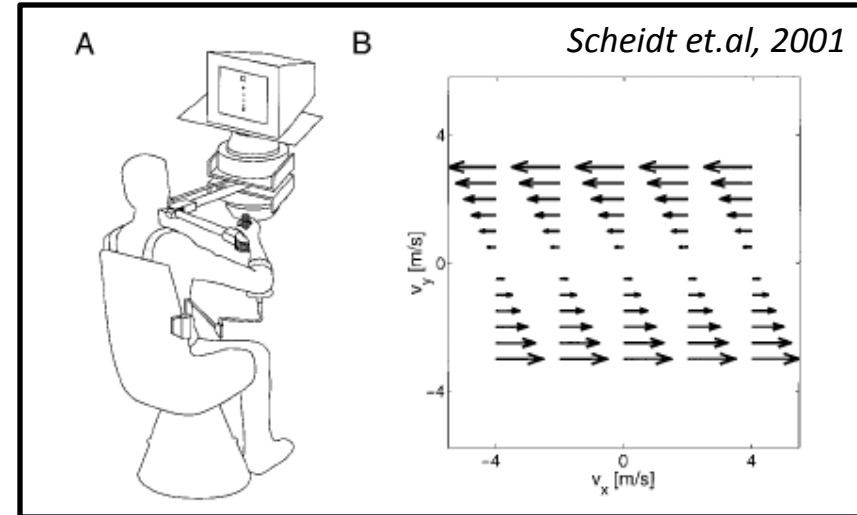
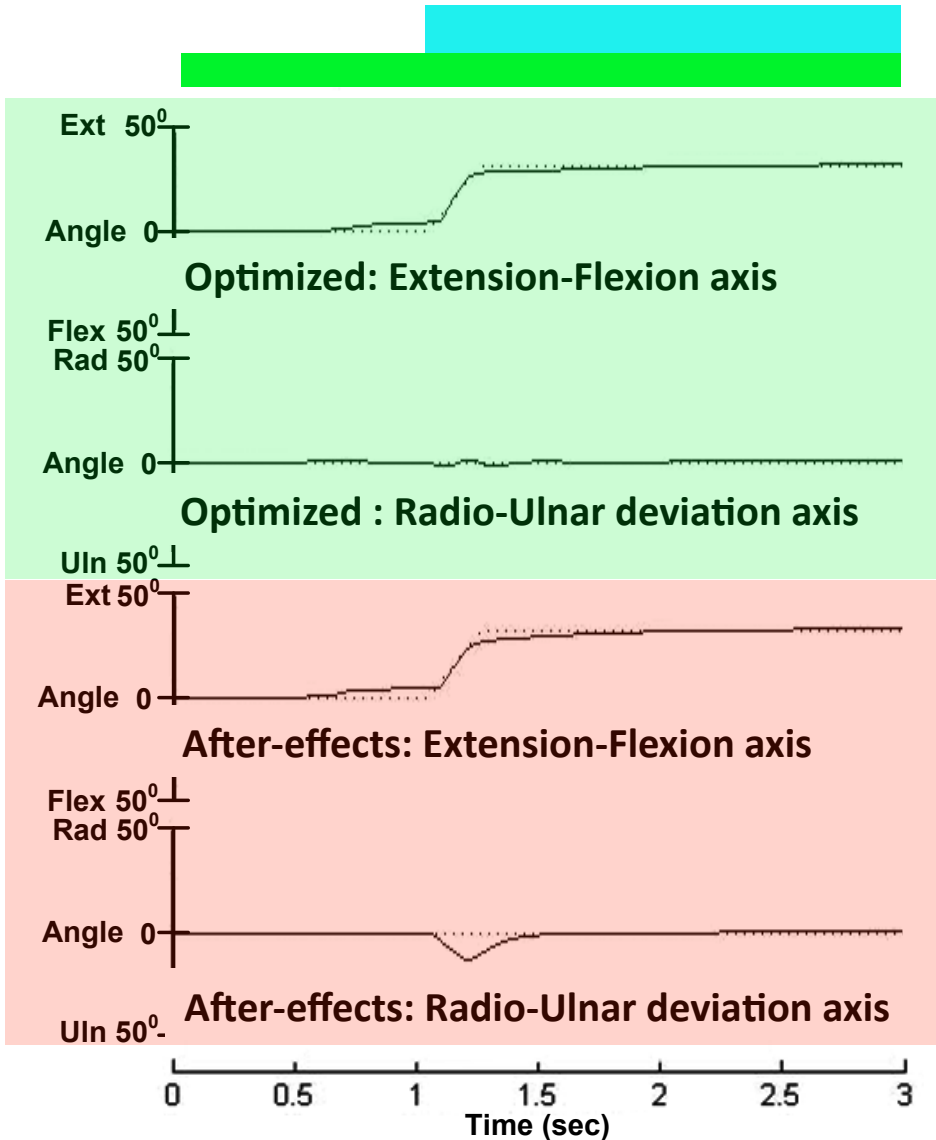


Ghez C and Gordon J 1987 Trajectory control in targeted force impulses I. Role of opposing muscles  
*Exp. Brain Res.* **67** 225-240



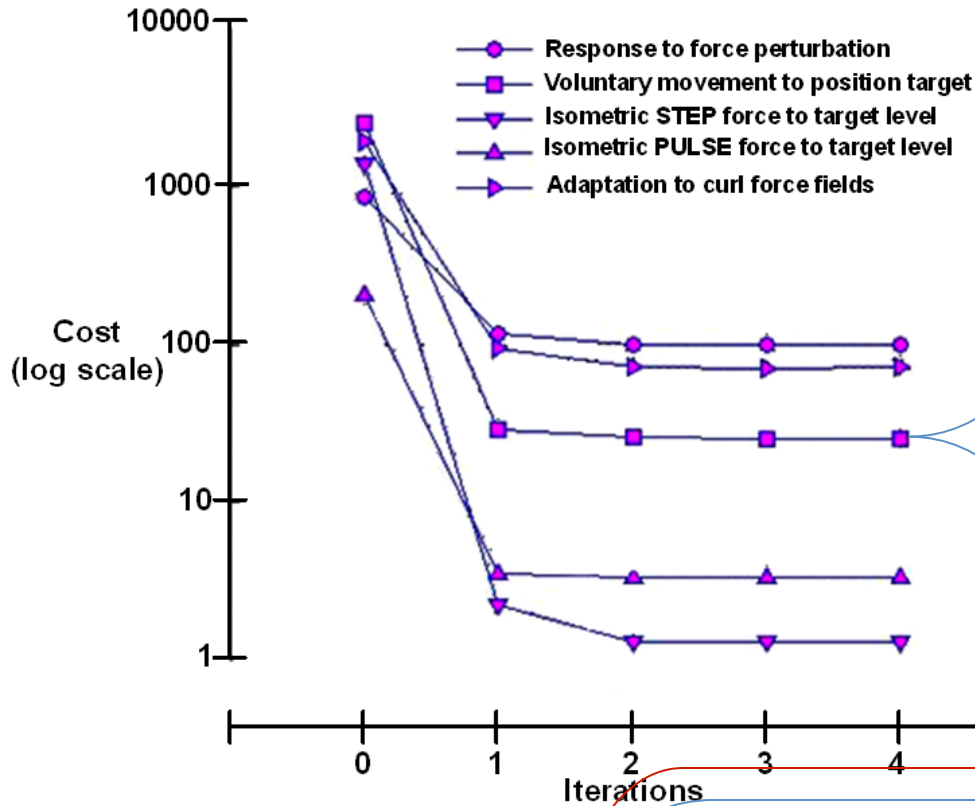
# Task 4: Adaptation to viscous curl force fields

Experiments: Kluzik 2008, Scheidt 2001; 2000; Diedrichsen 2005; Flanagan 1999; Hwang 2005; Karniel 2002, etc!

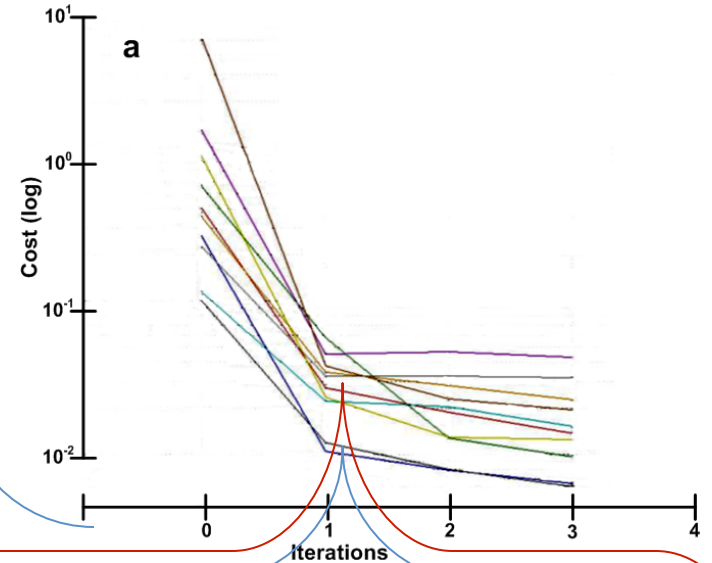


## Typical learning curves for all tasks

# Learning Curves

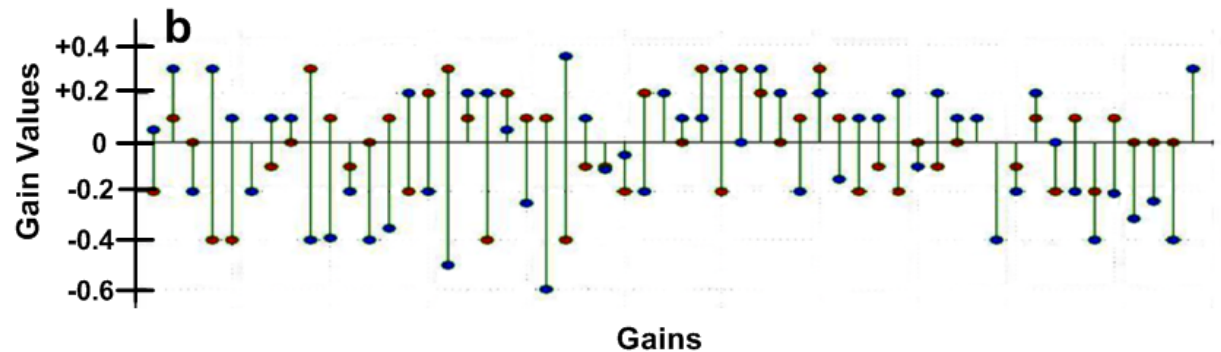


Random starting conditions for rapid movement

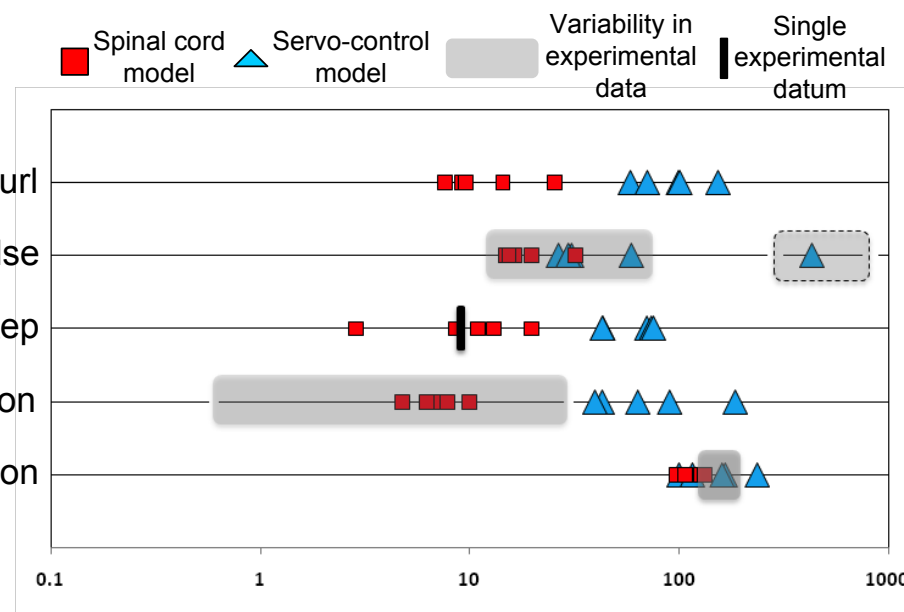
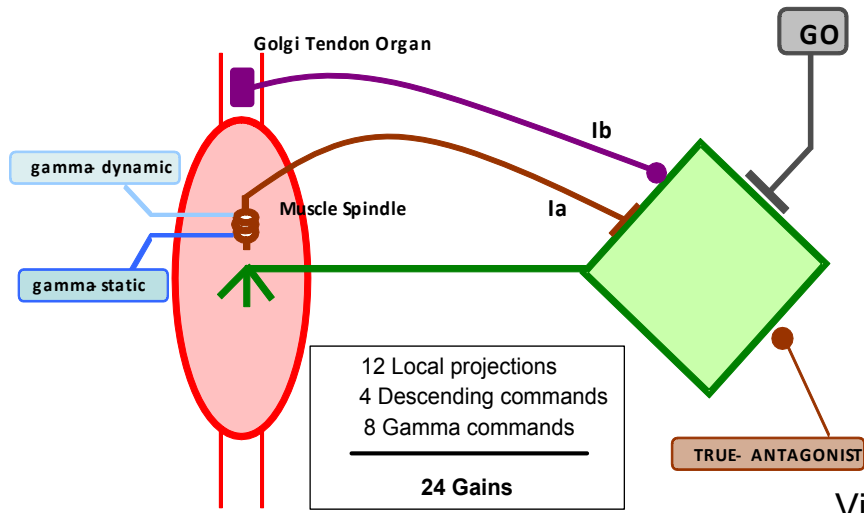


Conclusion:  
many local  
“good enough”  
minima

## Analysis of gain values

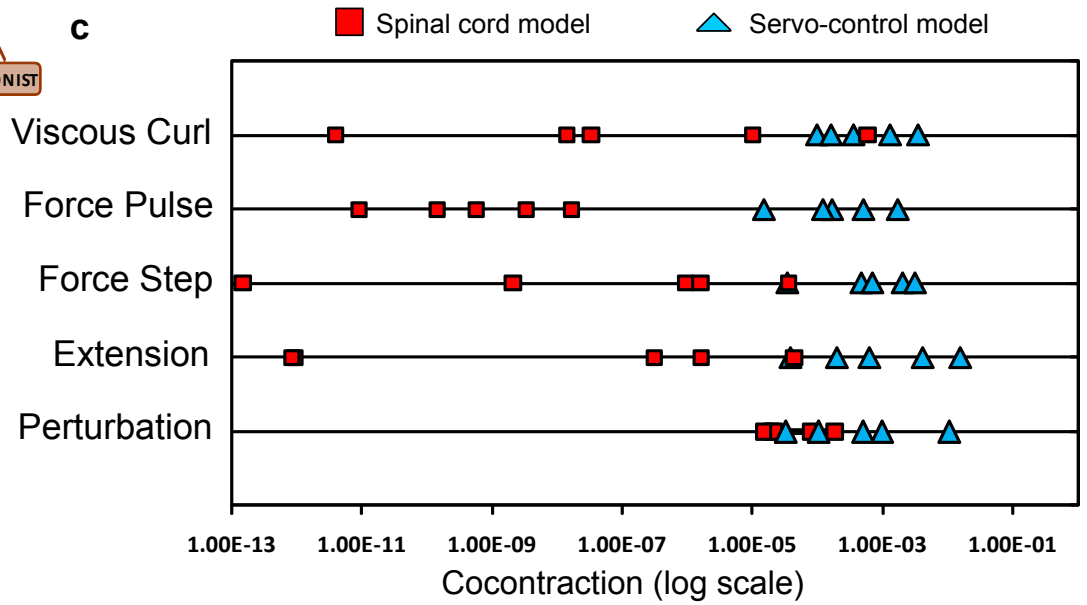


# Comparison with Servo-Control

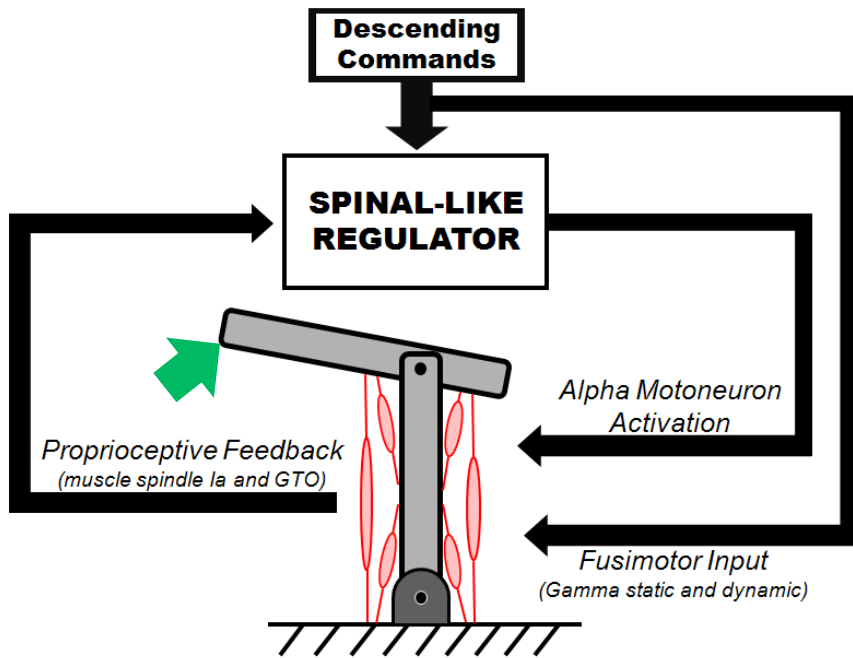


$$\int (\text{state}^* - \text{state})^2 dt$$

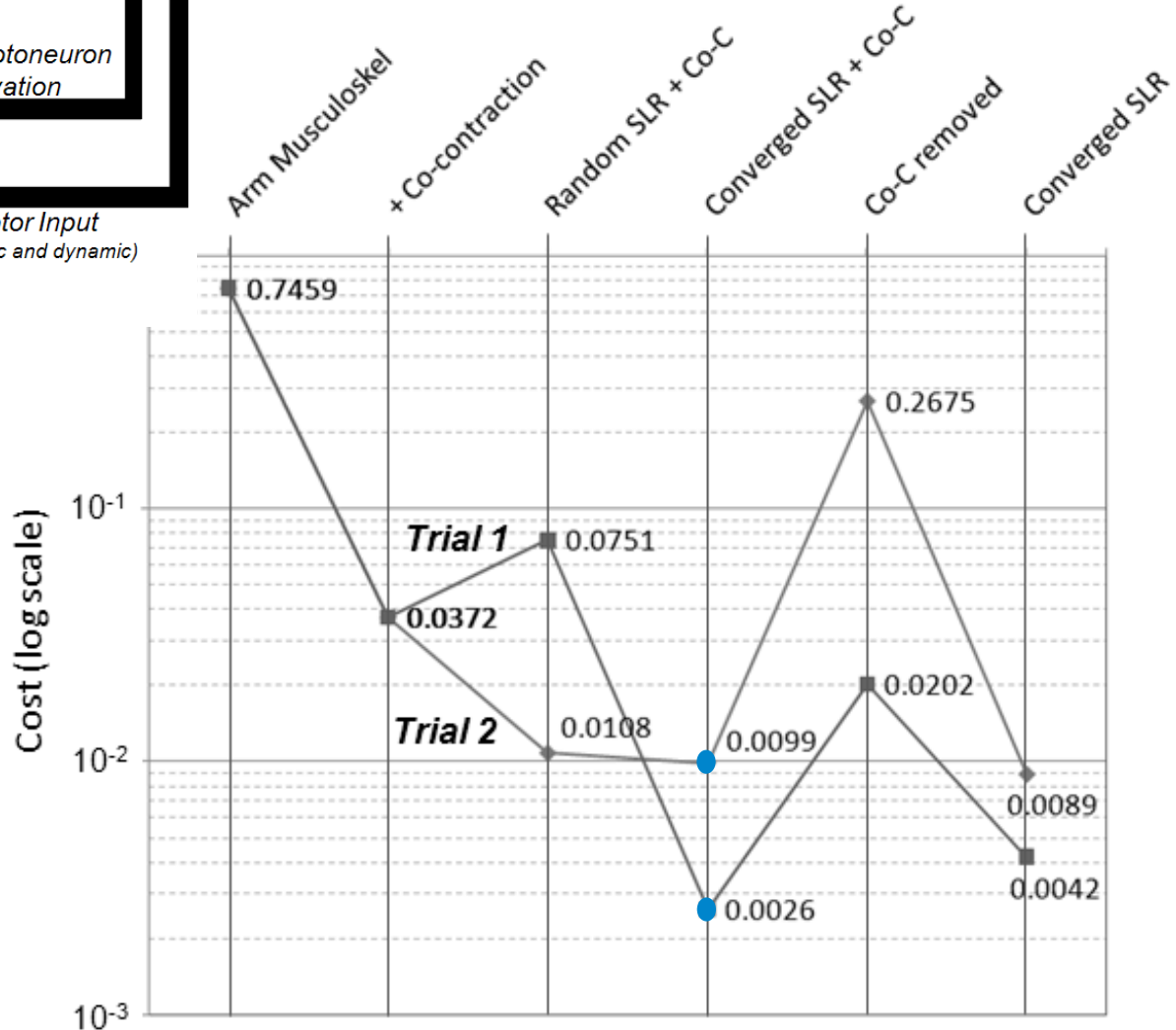
$$\int (\alpha_{EU}\alpha_{FR} + \alpha_{ER}\alpha_{FU}) dt$$



# SLR Controller for Planar Elbow-Shoulder Musculoskeletal System

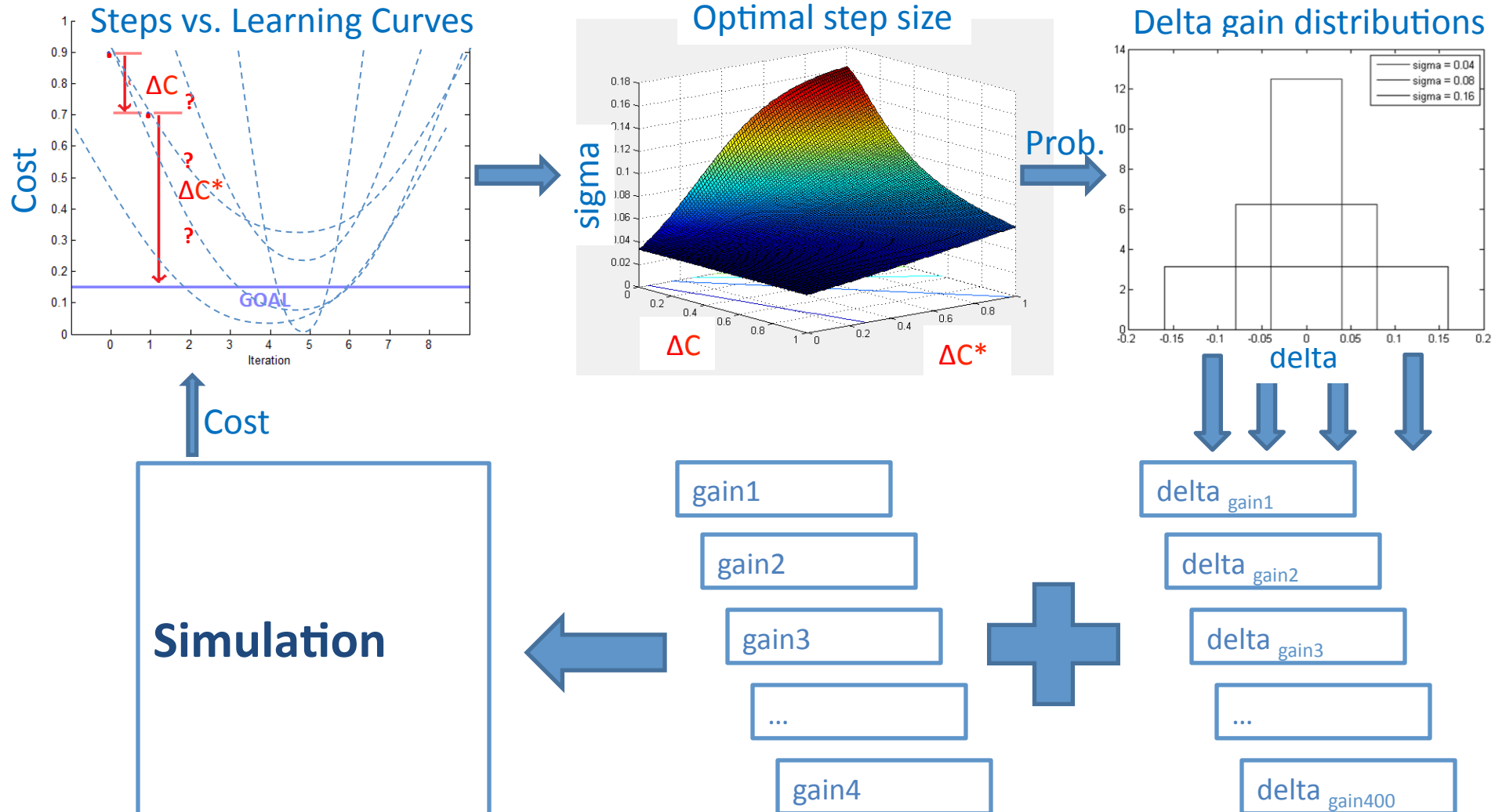


Learning to Resist  
**Sudden**  
**Perturbing**  
**Force**  
100N x 10ms

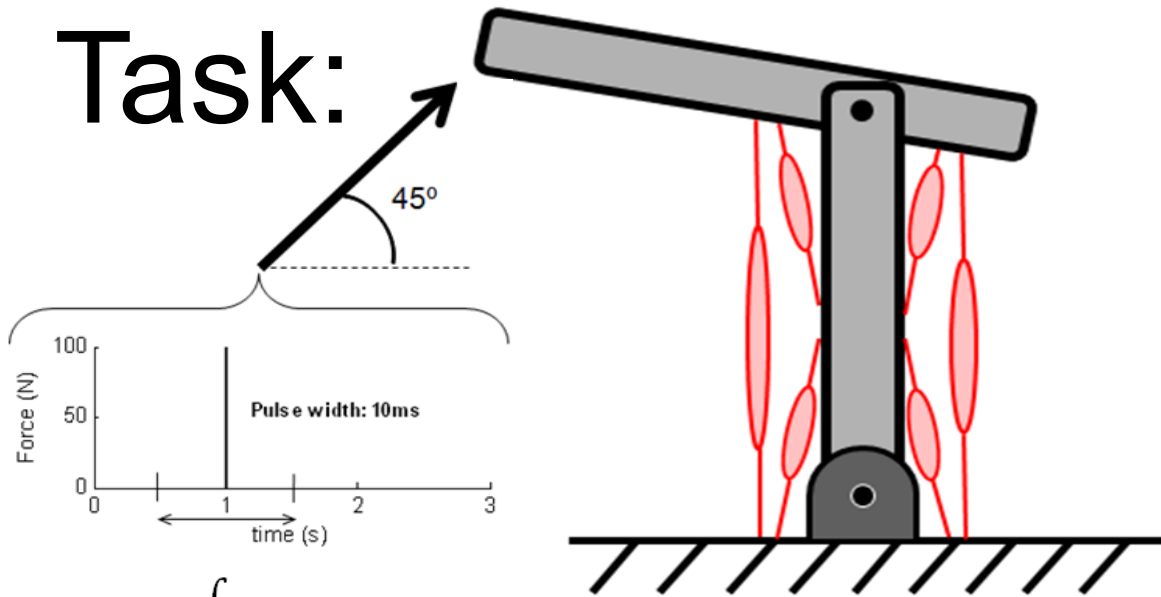


# BioSearch™ Corticospinal Learning Algorithm

Hypothesis: Landscape has so many “good enough” local minima that a Random Walk is a viable learning process



# Task:



$$Cost = \int (\text{Endpoint deviation from initial position})^2 dt$$

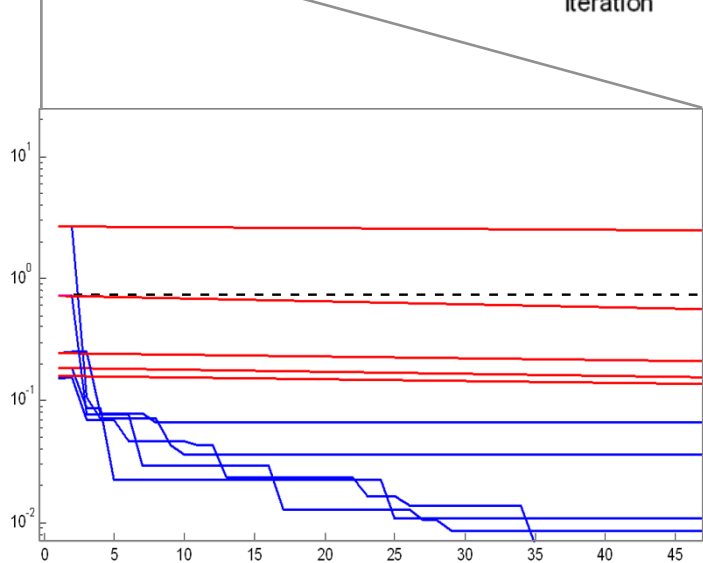
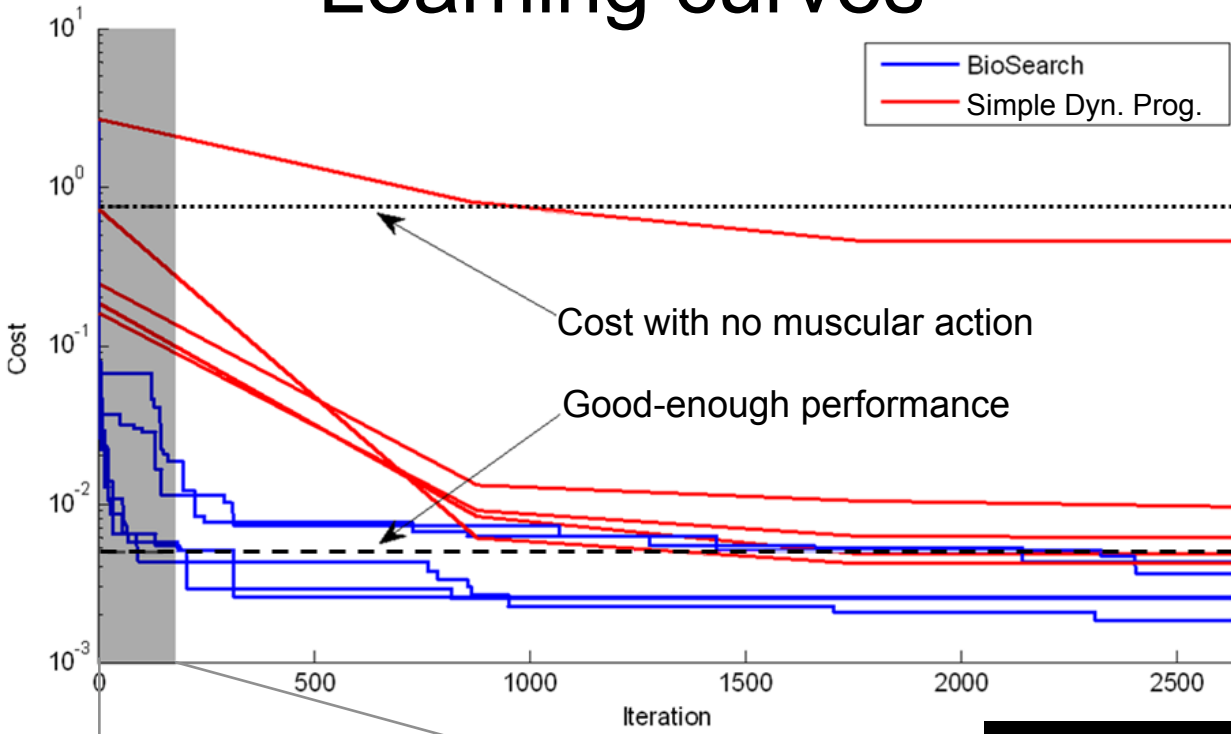
SET the gains of the SLR  
to resist an  
impulsive perturbation  
at the endpoint.



Passive Musculoskeletal System

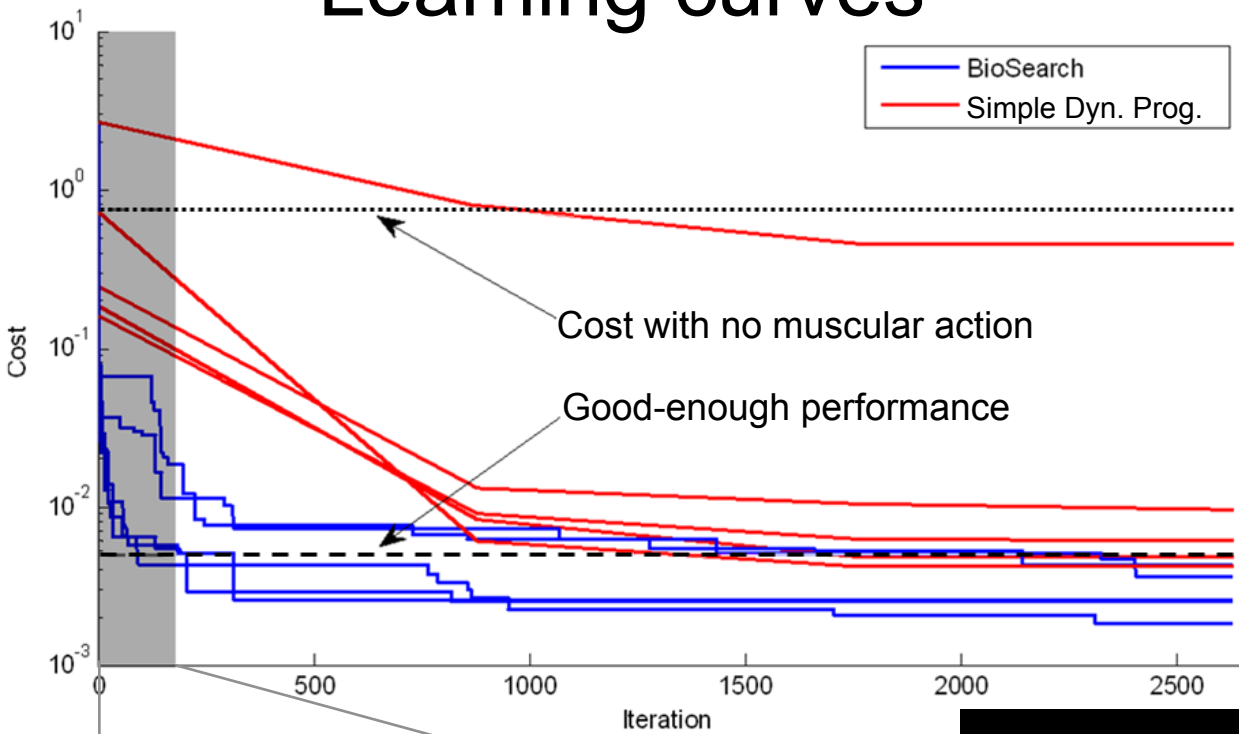


# Learning curves

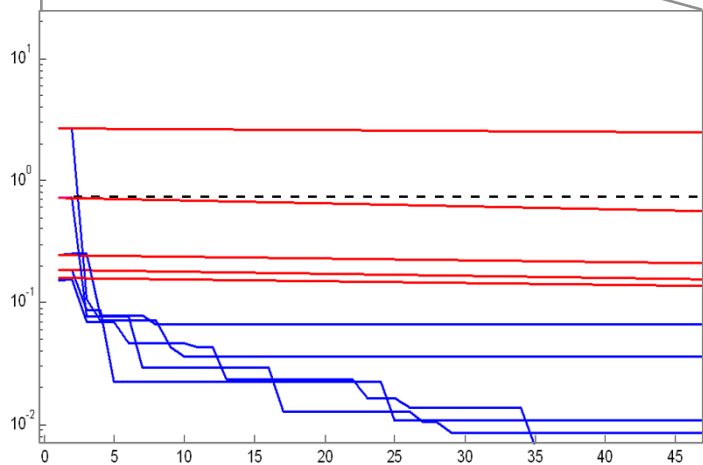
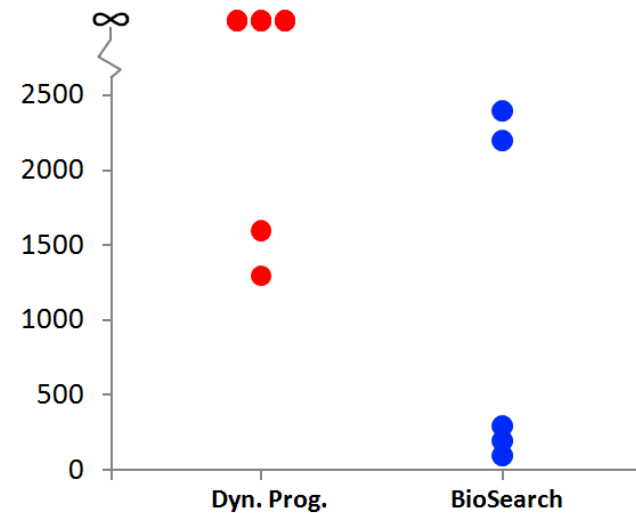


Random SLR

# Learning curves

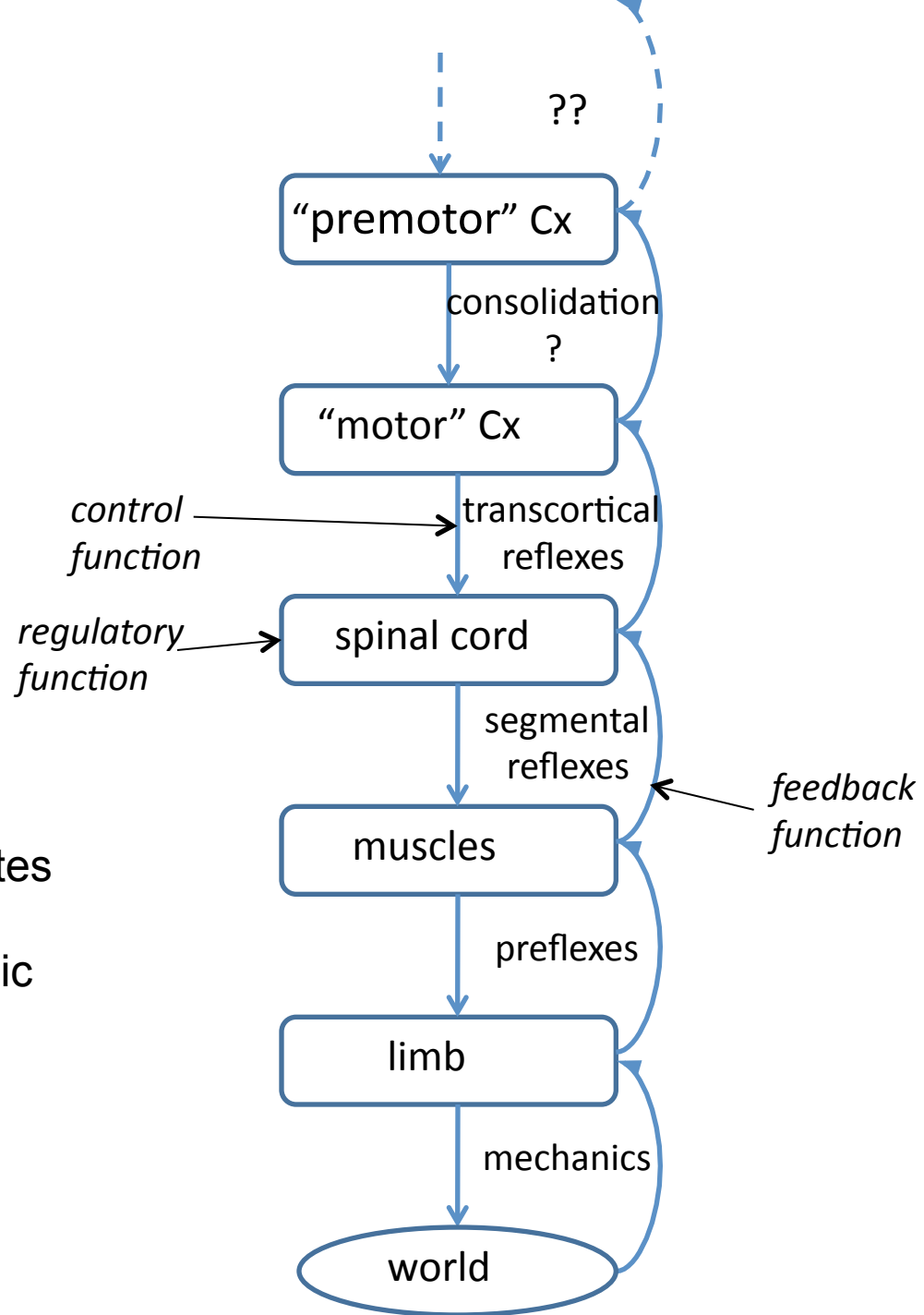


## Convergence rate



Multiple Solutions

# Hierarchical Control Updated



Each control stage operates on a lower stage whose local feedback and intrinsic properties constitute a regulator that is programmed by its controller.

# Anthropomorphic Design

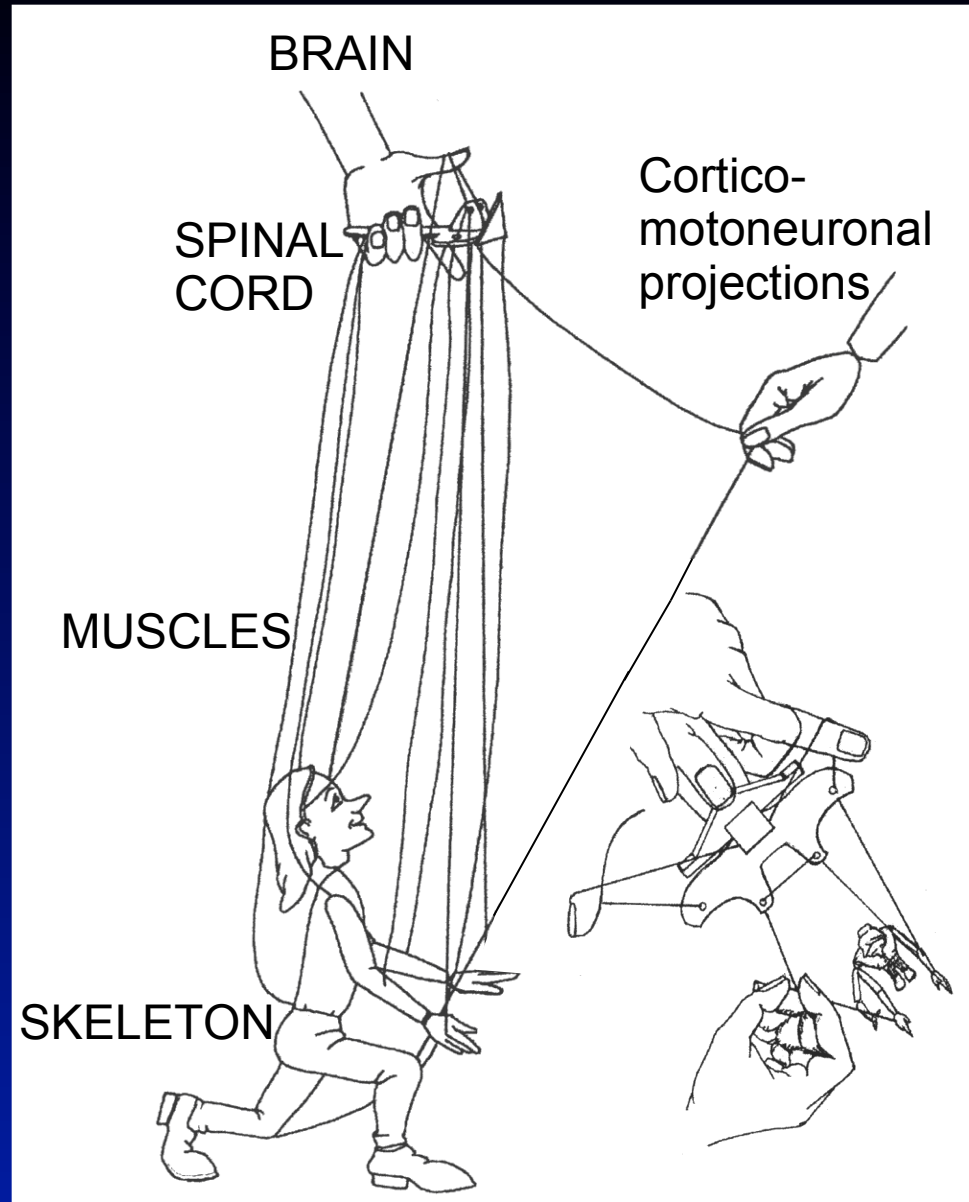
- Copy as many details of biological constructs as possible.
- Hope that the machine does something useful.

# Biomimetic Design

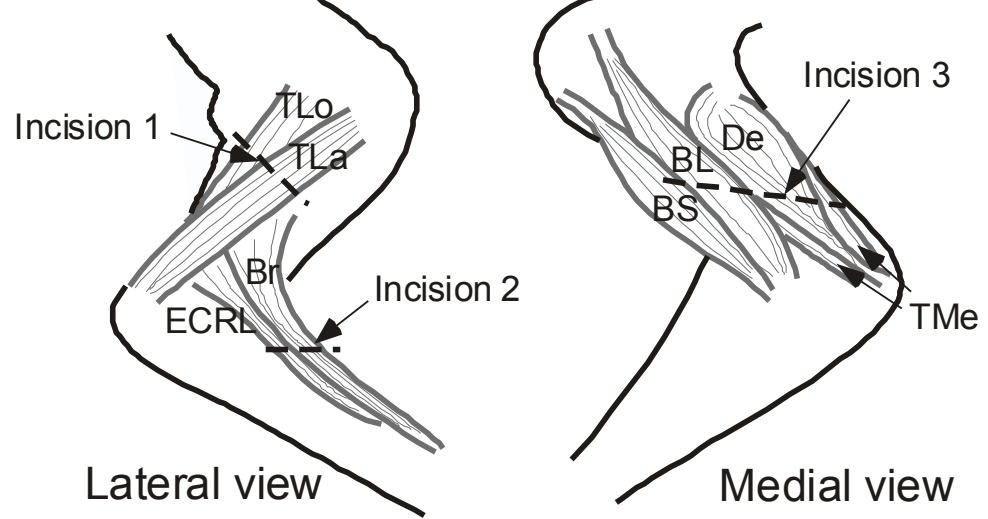
- ✓ Identify utility of each biological design feature.
- ✓ Understand principle of operation of the design feature.
- ✓ Build a machine based on that principle of operation.
- ✓ Demonstrate human-like capabilities enabled by that design feature.

# Valid Analogy?

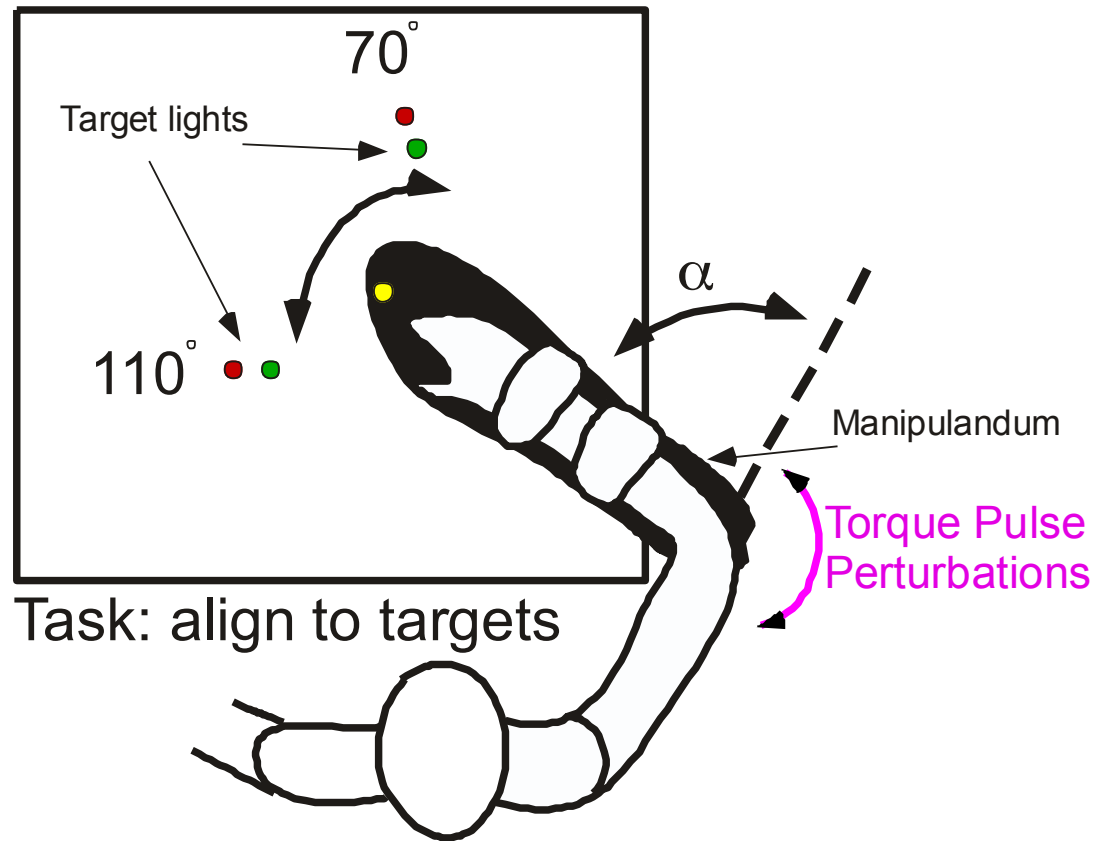
## *Theory of Computation for the Spinal Cord*



# Using a Musculoskeletal Model To Interpret Motor Control Strategies In a Forearm Pointing Task

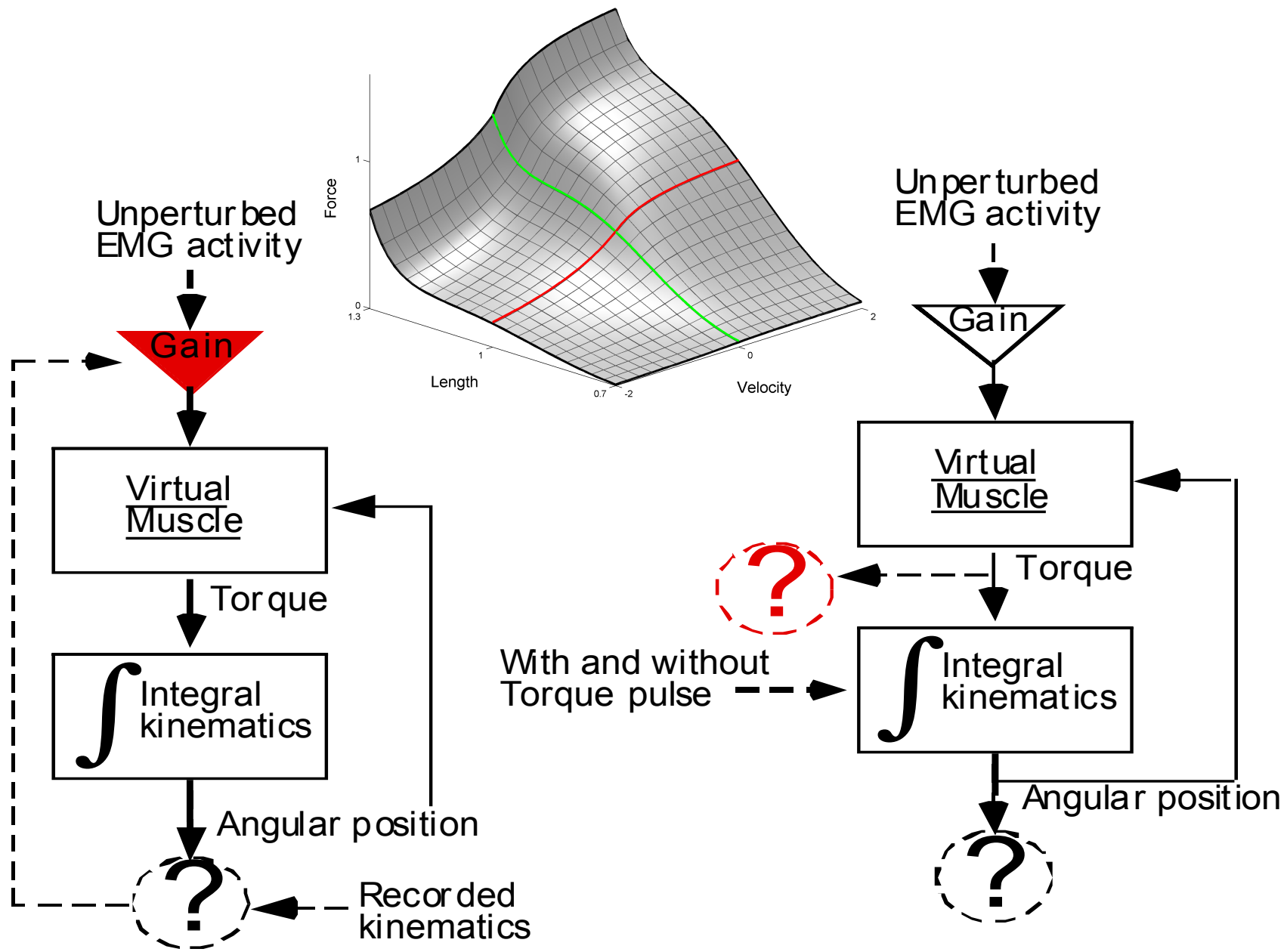


EMG recordings & muscle models

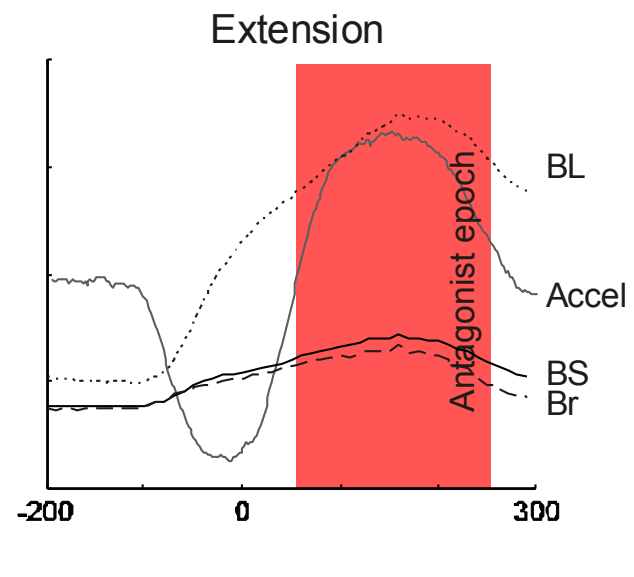
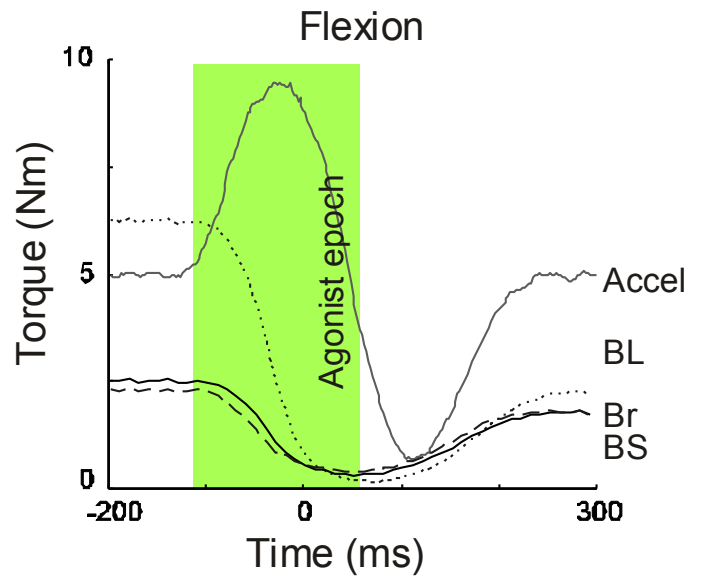
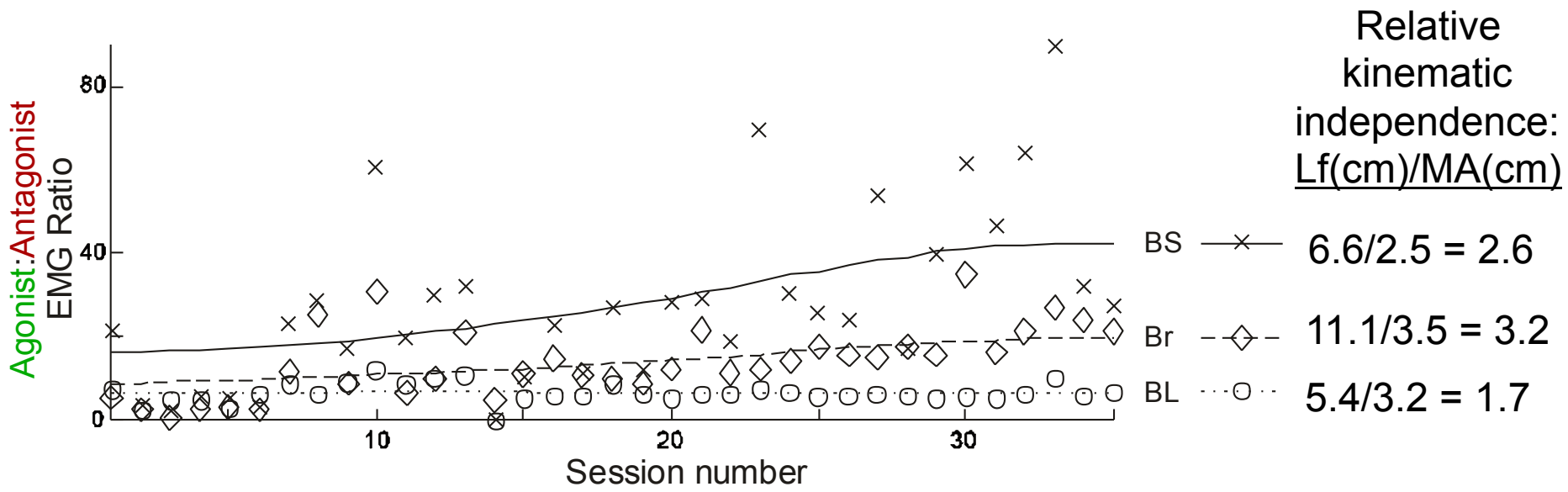


Cheng & Loeb (in prep.);

Cheng, Brown & Loeb (2000)  
Virtual Muscle,  
J. Neurosci. Meth.  
101:117-130

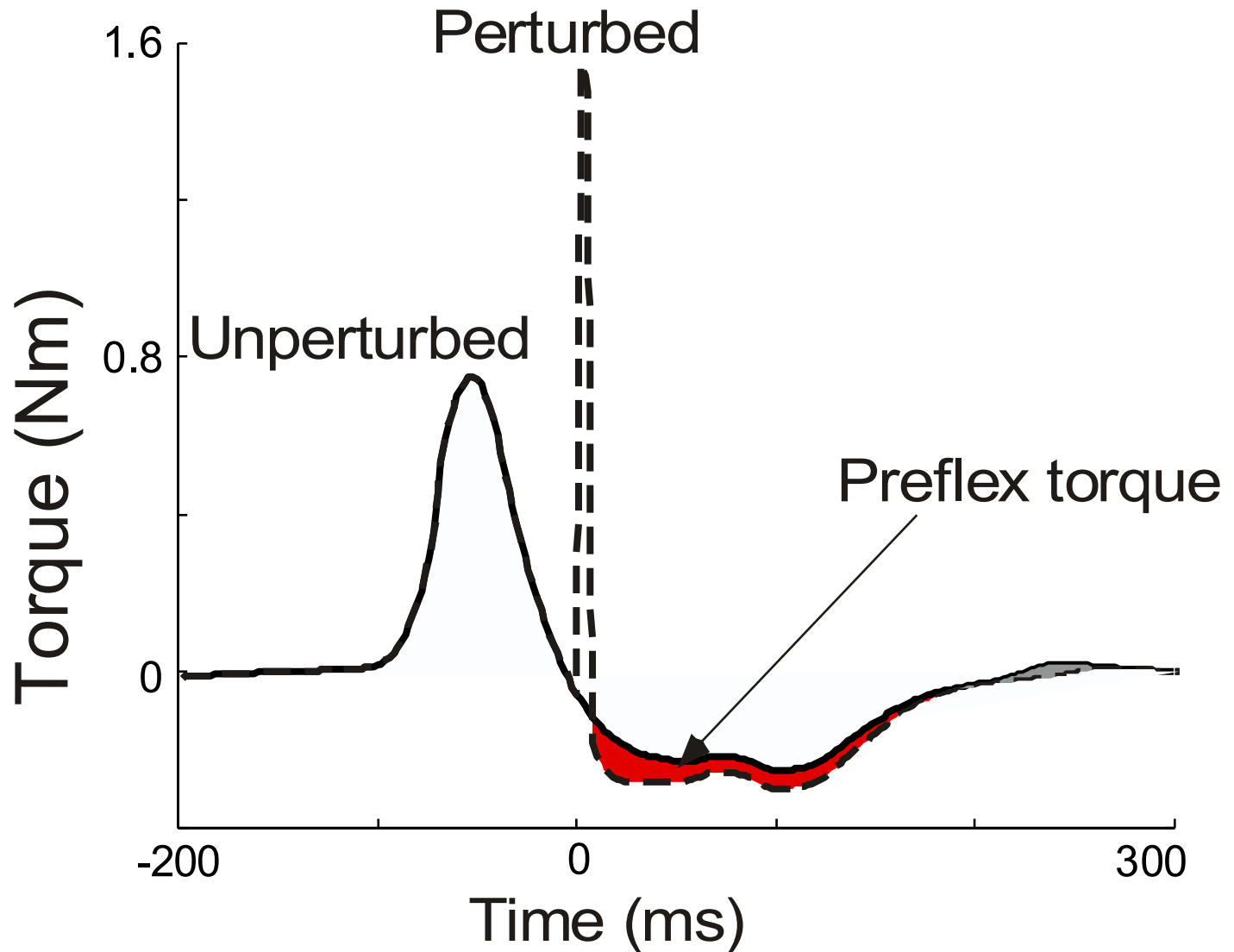


# Not all synergists are created equal.



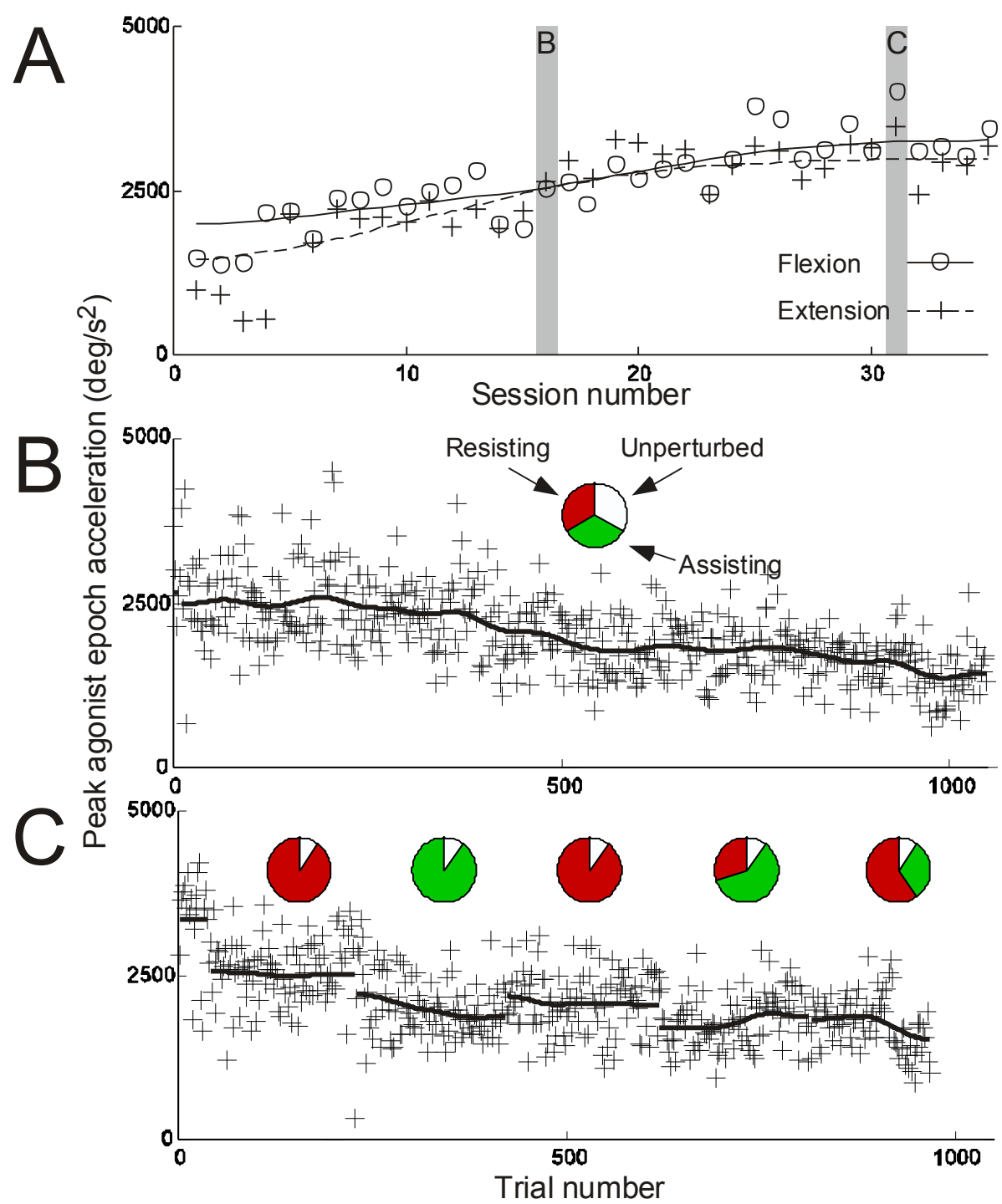


# Muscles are smart.

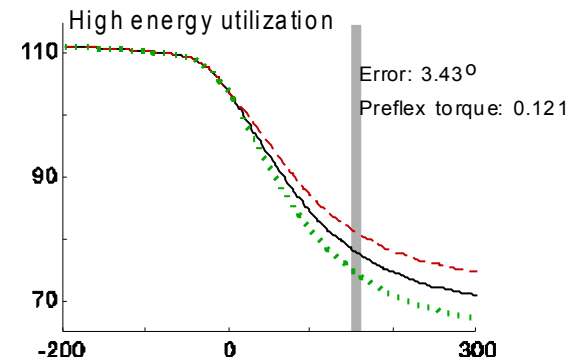
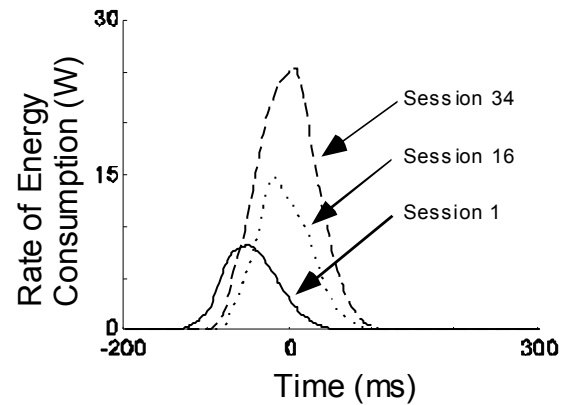
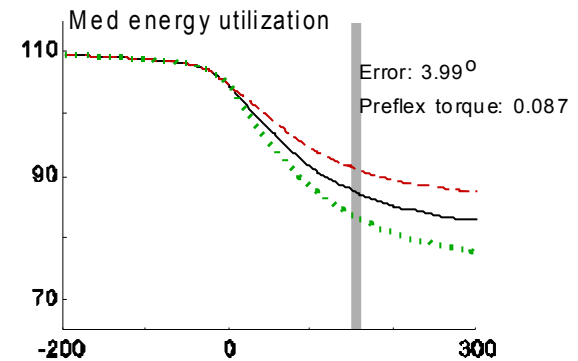
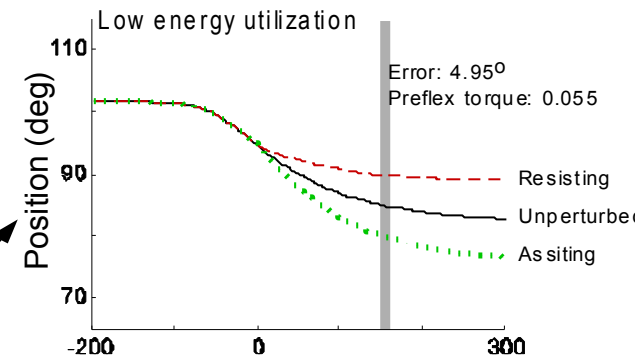
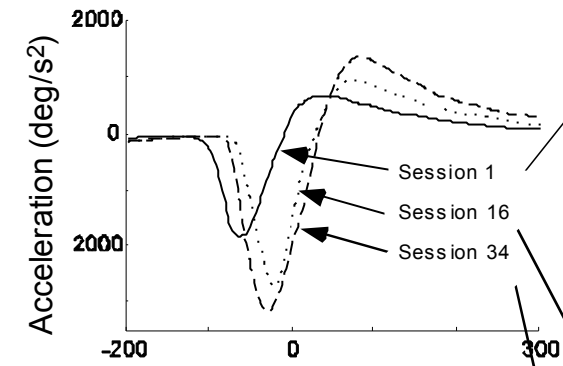


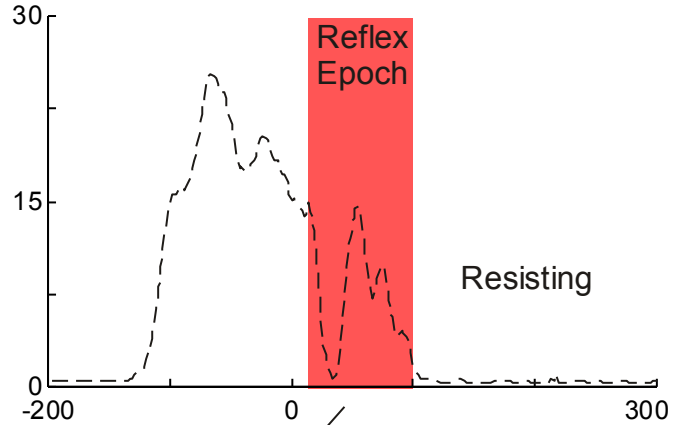
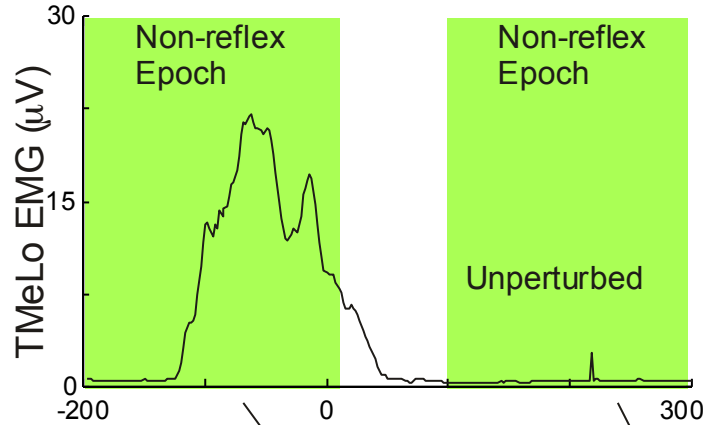
Even  
inertia  
can be  
smart

$$\frac{\text{Impulse } \Delta \Gamma \cdot t}{\text{Momentum } J \cdot \dot{\omega}}$$

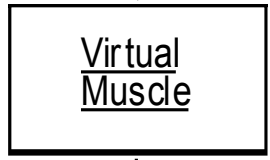


But  
momentum  
and  
preflexes  
have fixed  
costs





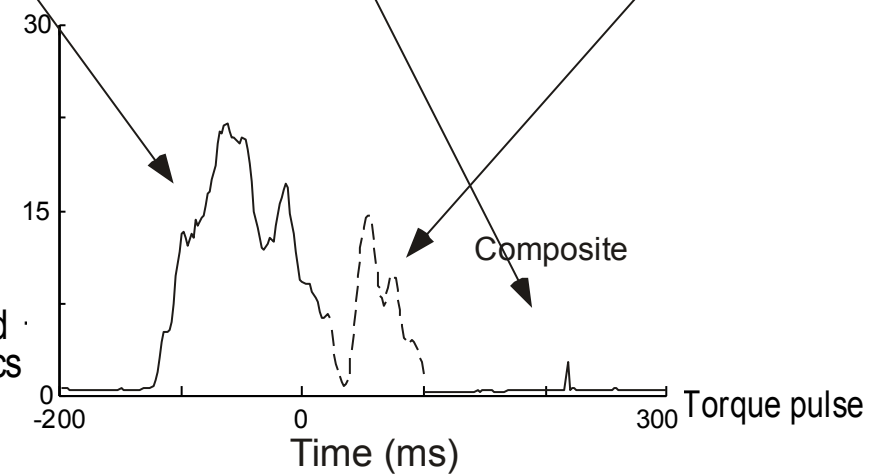
Unperturbed versus reflex EMG activity



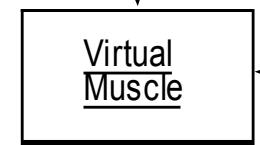
Torque



Quantifying reflex effects of individual muscles



Unperturbed versus reflex EMG activity



Torque



Angular position

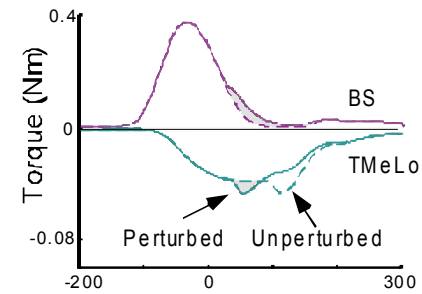
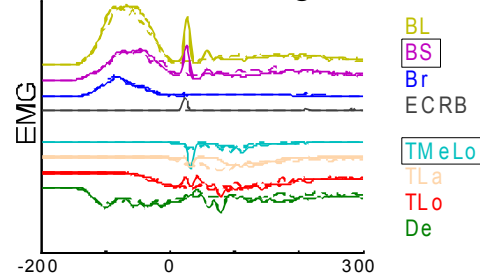


Effectiveness of reflexes in controlling perturbations

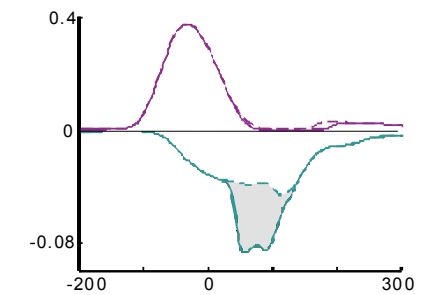
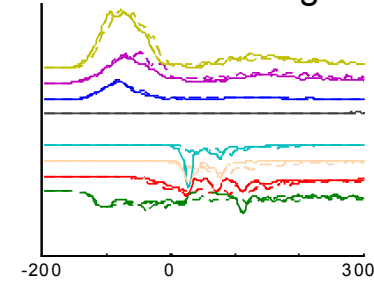
# Use Model to Understand Reflexes

They look like reflexes.  
Are they important?

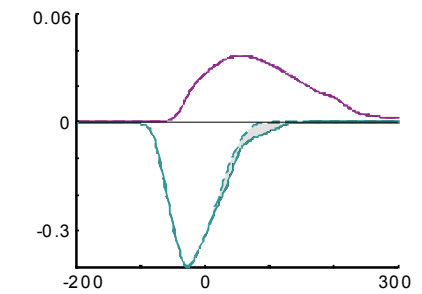
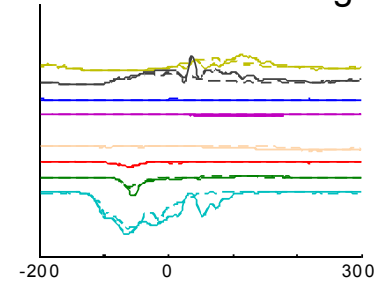
A. Flexion resisting



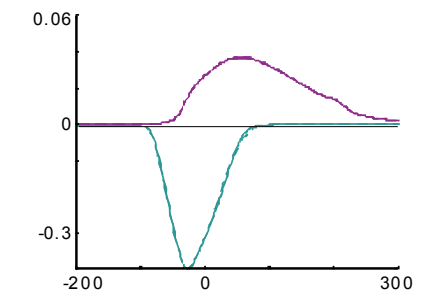
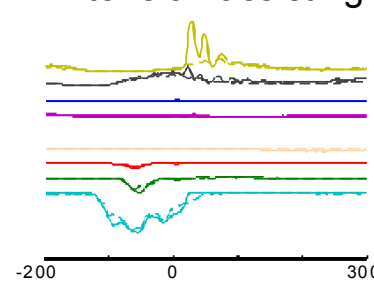
B. Flexion assisting



C. Extension resisting



D. Extension assisting

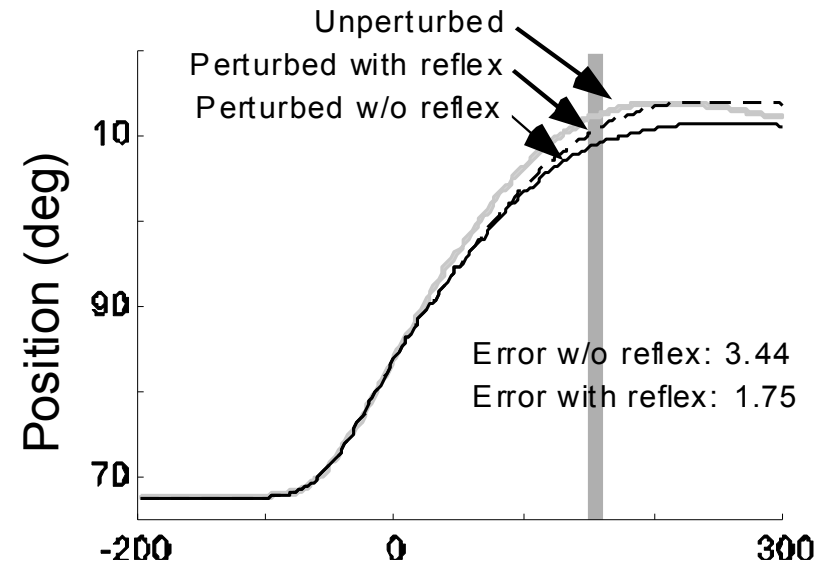
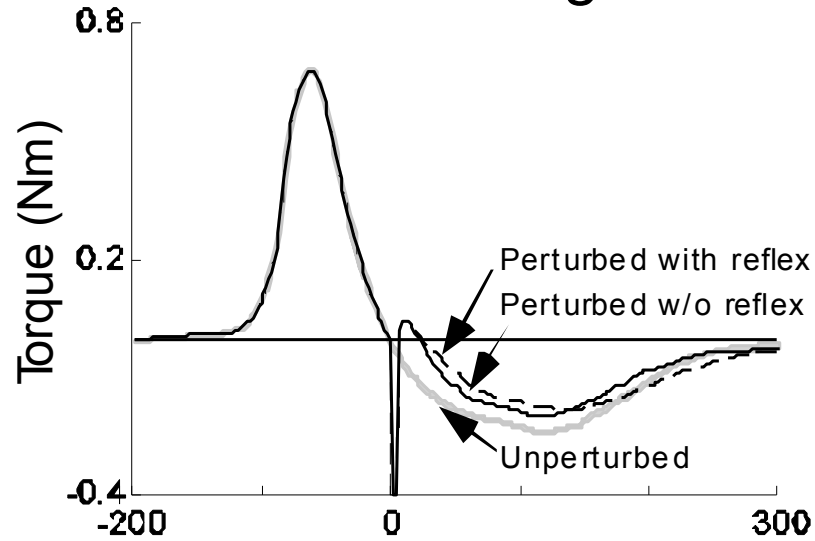


Time (ms)

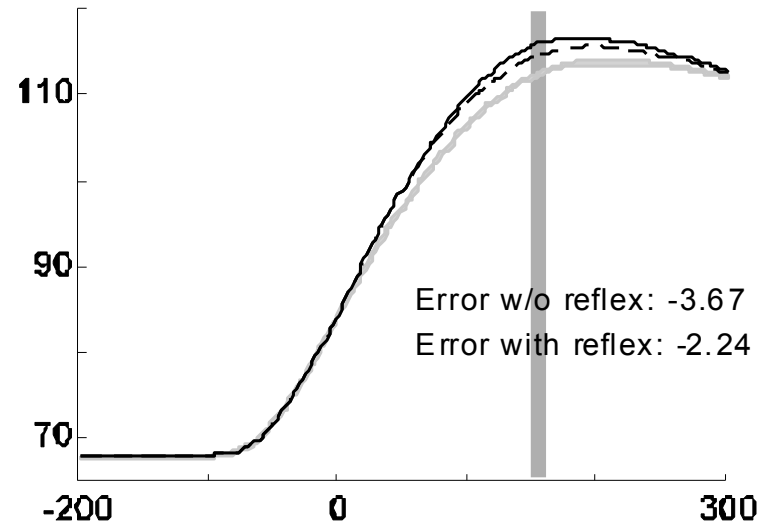
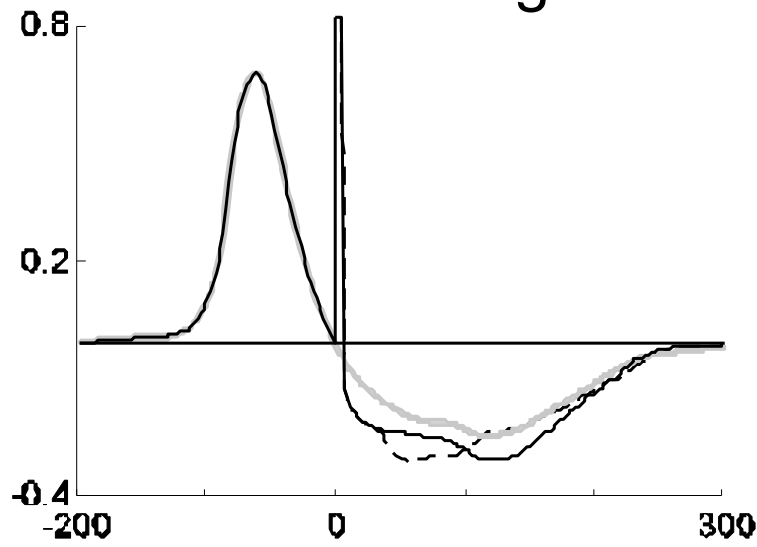
Time (ms)

# Preflexes alone don't cut it.

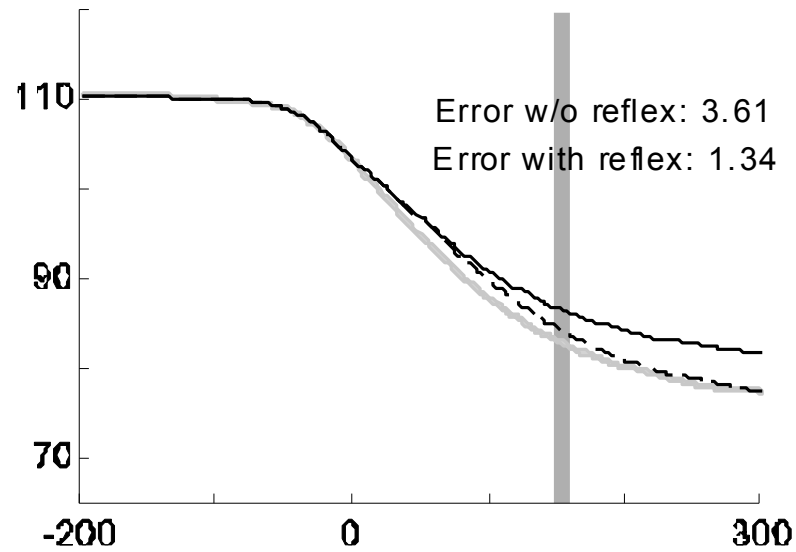
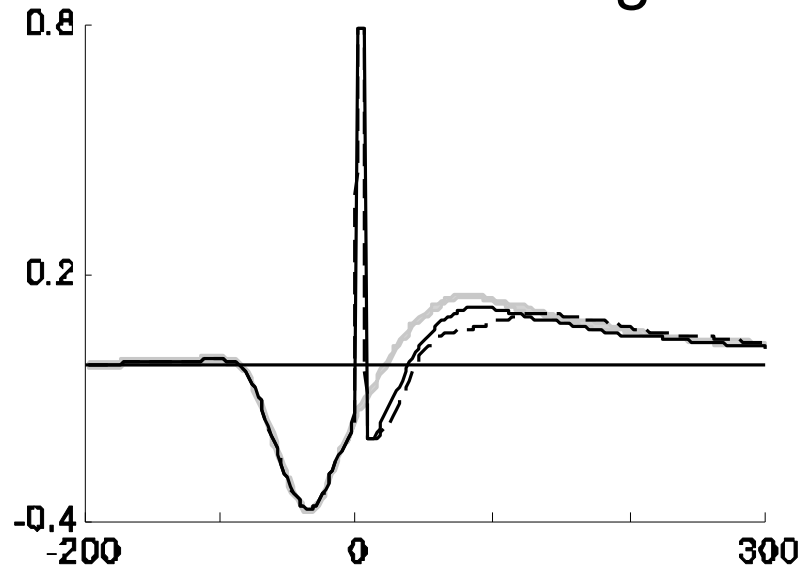
## A. Flexion resisting



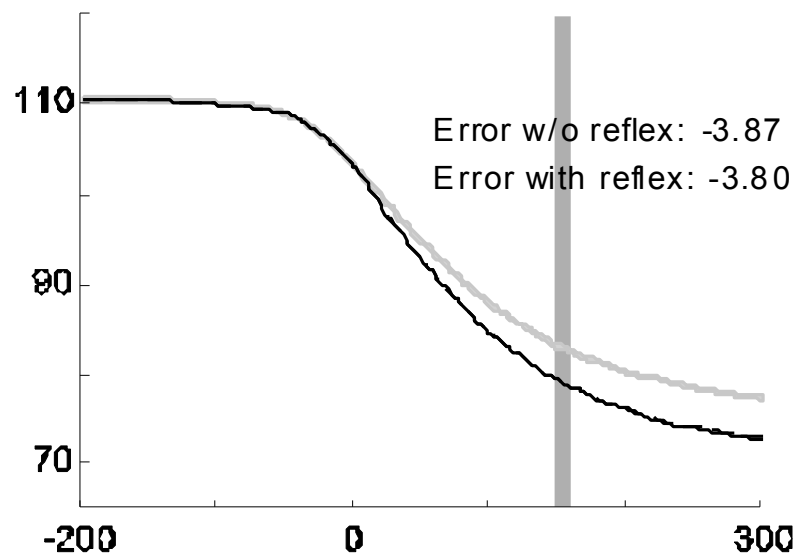
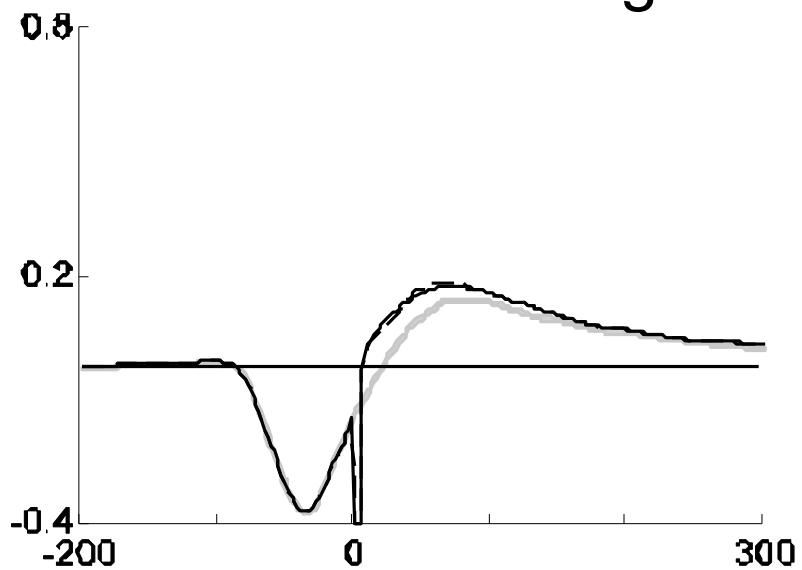
## B. Flexion assisting



### C. Extension resisting

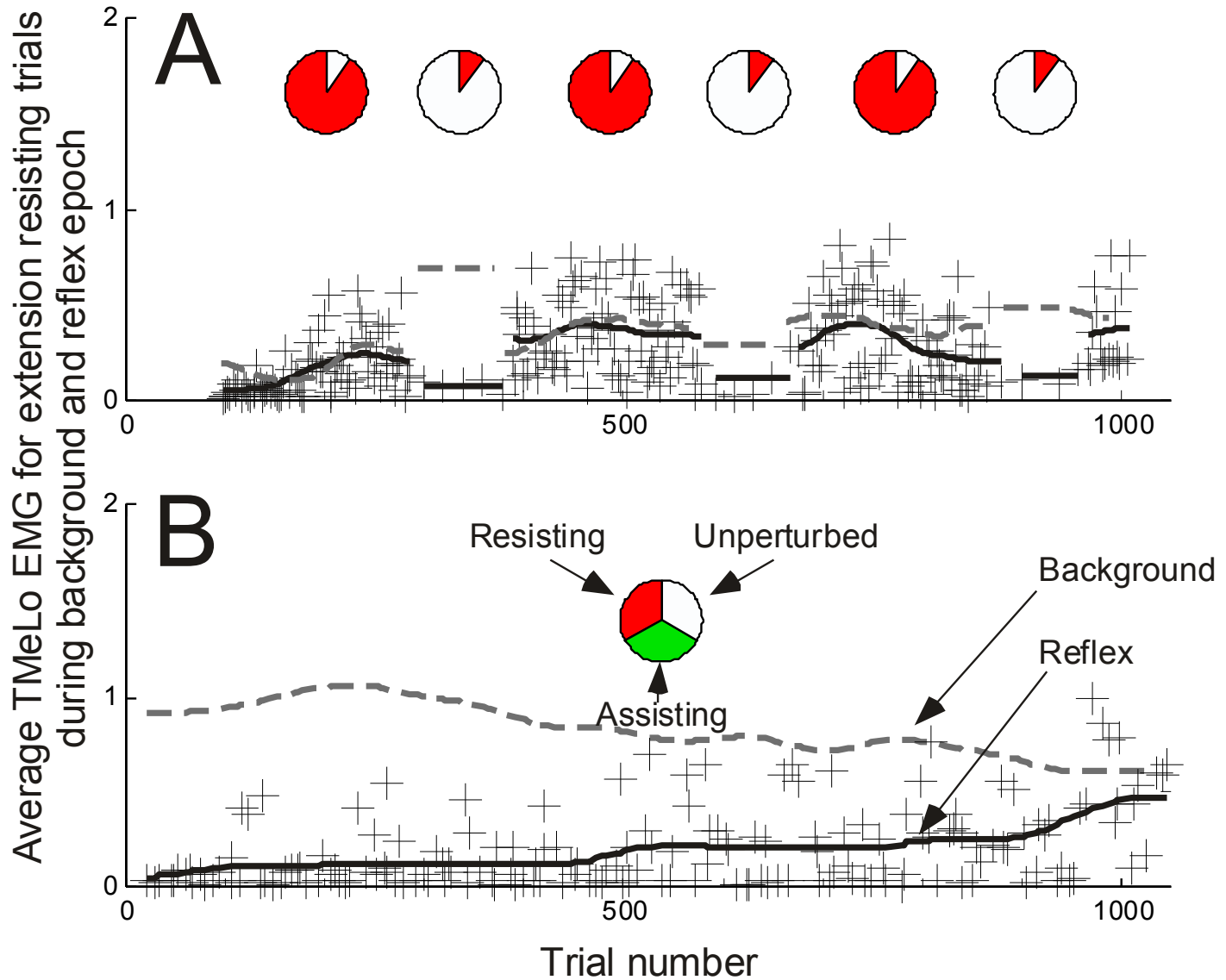


### D. Extension assisting



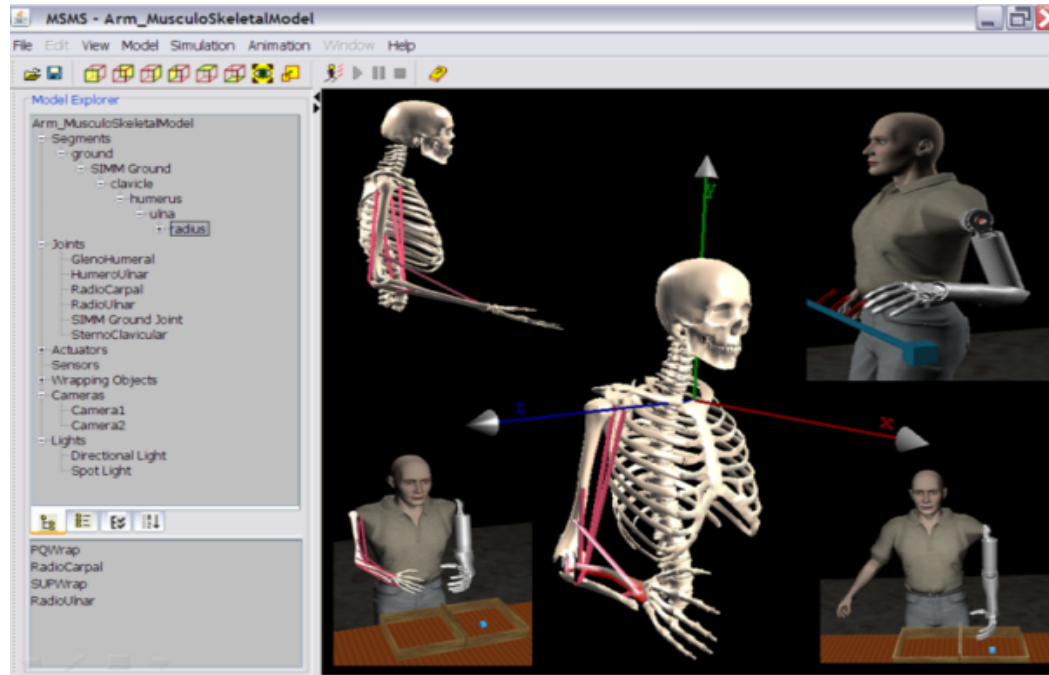
Time (ms)

# Are reflexes selectively controlled?





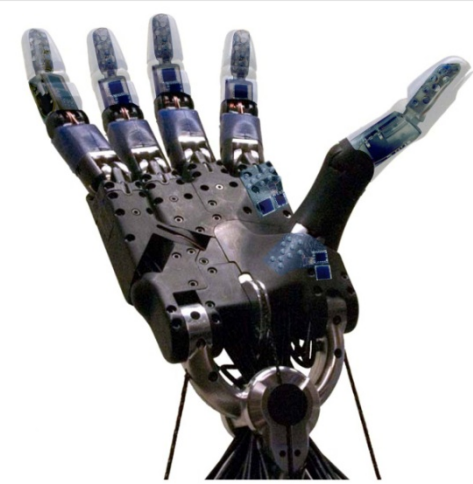
# MSMS: Main Goals and Features



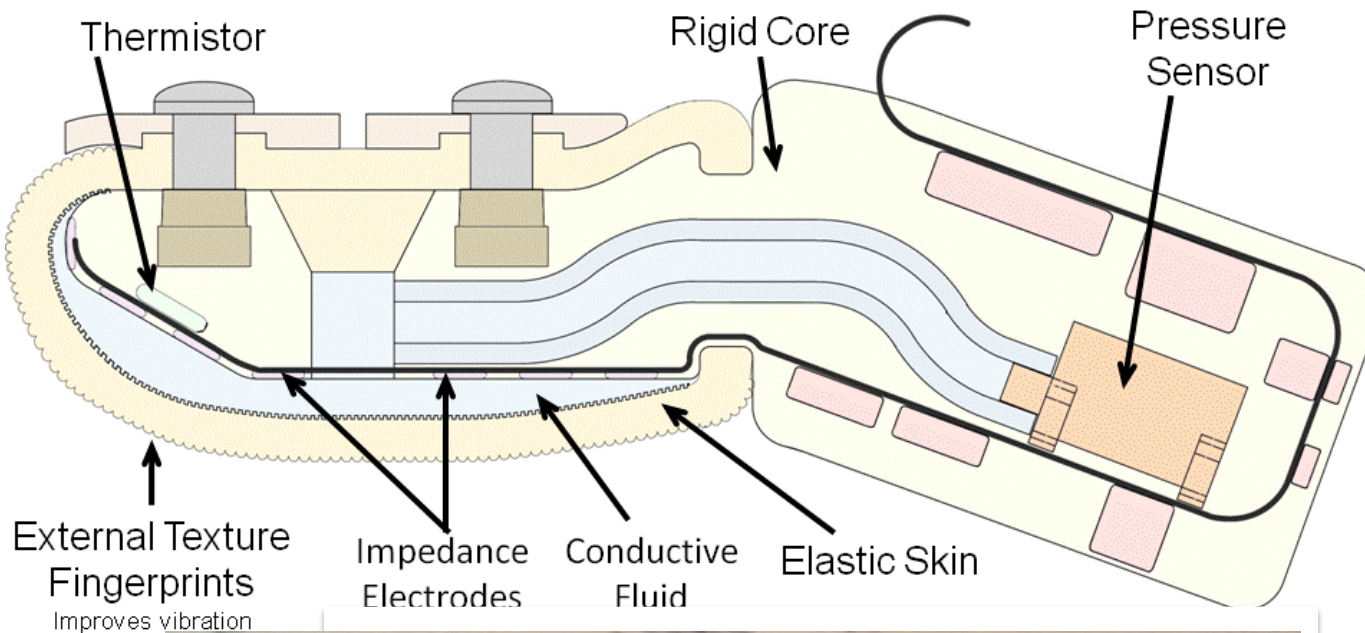
- ❑ Provides interactive tools for modeling musculoskeletal and prosthetic limbs and the task environments
- ❑ Simulates the models to predict limb's movement caused by neural controllers and external forces
- ❑ Simulates the models in real-time VR environments with the human or non-human primate subject in the loop

*Development since 1999 led by Dr. Rahman Davoodi  
Medical Device Development Facility, University of Southern California*

# Challenge: Can we endow mechatronic prosthetic & robotic hands with haptic abilities?



## BioTAC<sup>®</sup>



- Answer:**
- ### Biomimetic tactile sensors
- Contact with object deforms skin and fluid, changing electrode impedances
  - Heat flux into object identifies material properties
  - Skin sliding over textures generates vibration spectra recorded by pressure sensor